

DISSERTATION

TUMOR MICROENVIRONMENT IN SPONTANEOUSLY OCCURRING TUMORS
AND *IN VITRO* EVALUATION OF HYPOXIA ASSOCIATED
MUTAGENESIS

Submitted by

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In partial fulfillment of the requirements
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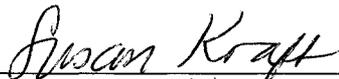
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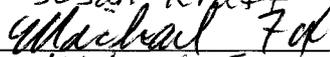
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WE HEREBY RECOMMEND THAT THE DISSERTATION PREPARED UNDER OUR SUPERVISION BY NADIRA TRNCIC ENTITLED TUMOR MICROENVIRONMENT IN SPONTANEOUSLY OCCURING TUMORS AND *IN VITRO* EVALUATION OF HYPOXIA ASSOCIATED MUTAGENESIS BE ACCEPTED AS FULFILLING IN PART REQUIREMENTS FOR THE DEGREE OF DOCTOR OF PHILOSOPHY.

Committee on Graduate Work



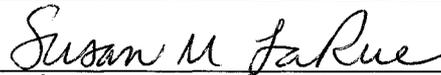
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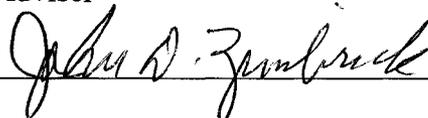


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ABSTRACT OF DISSERTATION

TUMOR MICROENVIRONMENT IN SPONTANEOUSLY OCCURRING TUMORS AND *IN VITRO* EVALUATION OF HYPOXIA ASSOCIATED MUTAGENESIS

The importance of the tumor oxygenation status in tumor progression and tumor response to radiation and other forms of treatment has been investigated in many experimental and clinical studies.

Oxygen status can impact cell killing associated with radiation treatment and, interestingly radiation can also impact subsequent oxygen levels. Part I of my dissertation is concerned with this phenomenon of reoxygenation. A multiparameter study was conducted in naturally occurring canine tumors to evaluate physiological changes in the tumor microenvironment following a 3 Gy fraction of radiation. Pre-treatment values of partial pressure of oxygen, interstitial fluid pressure, microvascular perfusion, level of apoptosis, and microvessel density were compared to the 24 hours post-radiation measurements in the same location. I analyzed changes in all parameters and evaluated the relationship between parameters and pO₂. In disagreement with my working hypothesis, I only found inverse correlation between changes in oxygen level and changes in IFP.

In Part II, I used the CHO A_L mutation assay to investigate the role of hypoxia alone in the induction of mutagenesis. After exposing cells to different hypoxic conditions I found that only severe hypoxia can cause mutations in human-hamster hybrid cells (A_L). Level of oxygen that induced mutations was less than 0.63 mm Hg. Both the complement-mediated A_L mutation assay and the flow cytometry mutation assay were done. Mutant cells were sorted from the mutant peak, and the clonal populations of cells were analyzed with the A_L flow cytometry assay to determine if cells were really mutated (negative for CD59) and not just downregulated in hypoxia. Quantitative analysis of mutations that were performed did not detect any changes in the CD59 gene.

Tumor reoxygenation, as shown here, may not be associated with improved tumor perfusion, but rather with other factors such as decreased oxygen consumption. These studies proved that severe hypoxia can cause mutations and possibly tumor genetic instability, and that those levels of oxygenation can be found in spontaneous tumors in dogs, which are a great tumor model for translating findings to human cancers.

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PART I

**THE IMPACT OF RADIATION ON TUMOR OXYGEN STATUS
IN SPONTANEOUSLY OCCURRING CANINE TUMORS**

CHAPTER 1

INTRODUCTION

Cancer is the second leading cause of death in the US, exceeded only by heart disease. In 2007 it is estimated that more than 1500 Americans a day will die of cancer (about 559,650 people) and about 1.445 million new cancer cases would be diagnosed in the US, plus more than 1 million cases of basal and squamous cell skin cancers (Cancer Facts and Figures 2007, American Cancer Society).

Cancer is a disease resulting from genetic mutations, either inherited or acquired, that allow cells to grow uncontrolled. However, there is a significant physiological contribution to the development of a tumor.

Tumor microenvironment

Microenvironment within solid tumors is different from that in normal tissues (Dewhirst et al, 1995), with characteristic chaotic vasculature and deficient lymphatic system (Rockwell et al, 2001). Unrestricted growth of tumors is dependent upon angiogenesis (Folkman et al, 1971; Folkman and Klagsbrun, 1987). The formation of new blood vessels is necessary for a tumor to grow beyond a few millimeters in diameter (Folkman, 1985). Normal angiogenesis usually occurs in the embryo as remodeling of the

primary capillary plexus, created by the process of vasculogenesis. During this process, vessels are formed from endothelial cell precursors called angioblasts. Remodeling of the primary capillary plexus is done by the sprouting and branching of new vessels from preexisting ones in the process of angiogenesis (Papetti and Herman, 2002).

Angiogenesis is also present in the adult during the ovarian cycle, in physiological repair processes such as wound healing, and in pathological non-neoplastic conditions as retrolental fibroplasia or diabetic retinopathy, arthritis, psoriasis, and duodenal ulcers (Folkman, 1995). Under non-neoplastic conditions, angiogenesis is a highly ordered process that strictly follows, and is limited, by the demand of growing tissues.

Neovascularization is essential for tumor growth and progression (Folkman et al, 1989).

Tumor-induced angiogenesis differs from that occurring in physiological situations and pathological nonmalignant conditions. Tumor-induced angiogenesis is not self-limited.

Once induced, it continues indefinitely. Tumor blood vessels may form from preexisting capillaries in a process very similar to normal angiogenesis. It has been suggested

recently that circulating endothelial precursors derived from bone marrow could be involved in tumor-derived vasculature formation. The induction of tumor

neovascularization results from the interrupted balance between pro- and anti-angiogenic factors in the tumoral microenvironment. Some of these factors are well characterized as

pro-angiogenic: vascular endothelial growth factor (VEGF), fibroblast growth factors (FGFs), heparinase, angiopoietin 2 (Ang2), and interleukin-8 (IL-8). In addition to the

stimulators of angiogenesis there are more than 40 endogenous angiogenesis inhibitors: interferons (INF- α , - β , - γ), interleukins (IL-4), tissue inhibitors of metalloproteinases

(TIMPs), photolytic fragments (angiostatin, endostatin), and others like

thrombospondin-1 (TSP-1) (Papetti and Herman, 2002). Tumor expansion after the onset of angiogenesis is dependant not only on delivery of oxygen and nutrients by new microvessels, but also on the release of anti-apoptotic and survival factors (at least 20 of them), from the endothelial cells in these new vessels, some of them being: acidic fibroblast growth factor (aFGF), basic fibroblast growth factor (bFGF), Interleukin-6 (IL-6), Insulin-like growth factor-1 (IGF-1), Platelet derived growth factor (PDGF) (Folkman, 2003).

As a tumor grows, a chaotic network of microvessels develops. Newly formed microvessels do not parallel the morphology of the host tissue vasculature as nicely shown in Fig.1.1. (Vaupel, 2004). Such microvessels are characterized by lack of smooth muscle cells and nervous components, tortuosity, dilatation, elongation, arterio-venous shunts, and blind ends (Jain, 1999). Tumor blood vessels have incomplete or even missing endothelial linings and basement membranes, resulting in increased leakiness. The extravasation of plasma and red blood cells results in an increase of the interstitial fluid space (Vaupel, 2004). The density of the tumor vascular network is expressed as intratumoral microvascular density (MVD). It is usually implied that MVD is directly related to tumor angiogenesis, but some non-specific factors, such as inflammation, can modify the vascular density within the tumor. The intratumoral vascular density was found to vary in the degree and spatial distribution between tumors, but even among tumors of the same histology (Koukourakis et al, 2000). Many studies on different tumor types have provided significant prognostic information with high vascularity associated with poor treatment outcome (Weidner et al, 1992; Alvarez et al, 1999; Guidi et al, 2000; West et al, 2001, Uzzan et al, 2004).

In addition, a functioning lymphatic system is absent in most solid tumors. Some recent findings (Stacker et al, 2001; Karkkainen et al, 2004) provide evidence that tumors can activate lymphangiogenesis, stimulated by VEGF-C and VEGF-D and the receptor, VEGFR-3.

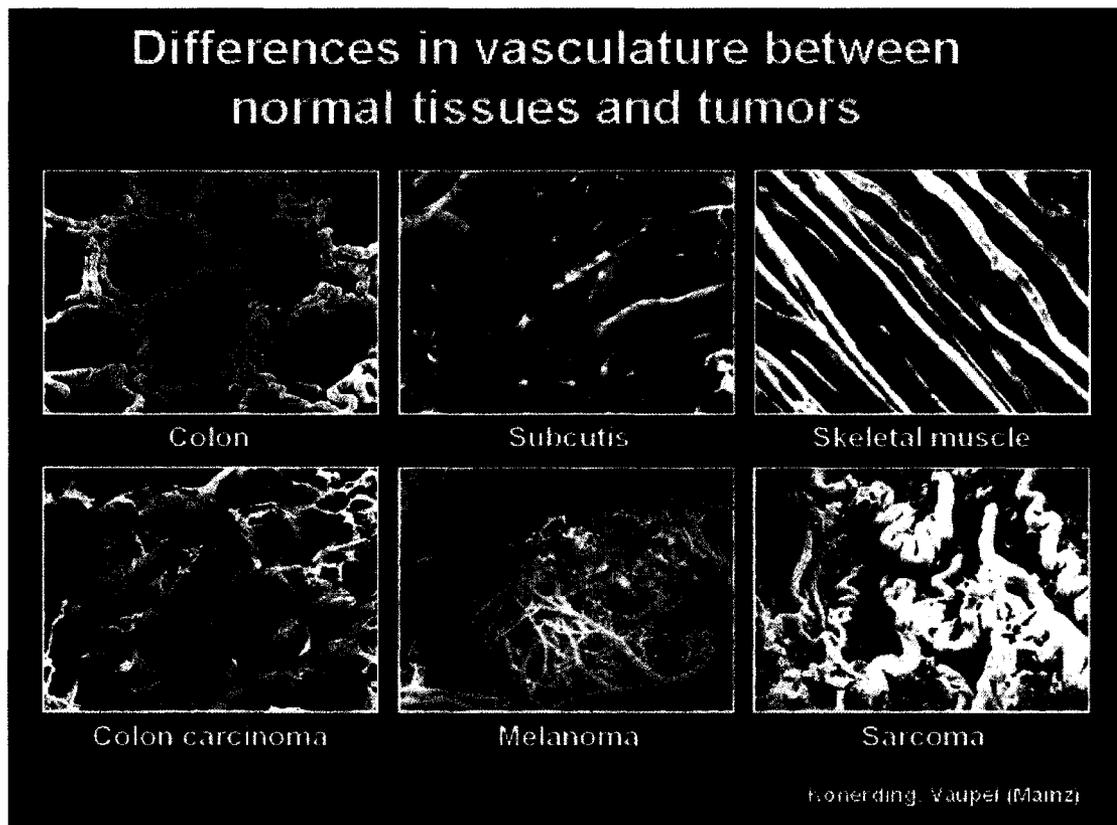


Figure 1.1 Differences in vasculature between normal tissues (upper panels) and malignant tumors (lower panels). (Vaupel from Konerding, 2004).

Tumor blood and lymphatic vessels are structurally and functionally abnormal, which results from an imbalance in molecular factors regulating growth and maturation of the

vessels, and from the compressive mechanical forces formed by proliferating tumor cells. These abnormalities can lead to hyperpermeable, tortuous vessels and compressive forces can cause vessel lumen collapse and hence influence blood flow.

The absence of properly functioning lymphatics results in decreased interstitial fluid drainage and increased values of interstitial fluid pressure (Dunn, 1997; Kuszyk et al, 2001). Elevated IFP in solid tumors was recognized as early as the 1950s (Young et al, 1950). Interstitial hypertension has been measured since then in animal and human solid tumors (Znati et al, 1996; Zachos et al, 2001; Milosevic et al, 2001). Normal IFP is close to atmospheric, but in tumors it is elevated. IFP has been measured in a variety of human tumors before treatment, and it was in a range from near zero to levels of 100mmHg (Boucher et al,1991; Gutmann et al,1992; Milosevic et al,1998; Cairns et al, 2006). Recent studies on a spontaneous carcinogenesis model (Hagendoorn et al, 2006) found that interstitial fluid pressure was already elevated in the hyperplastic/dysplastic stage (early stage of cancer development). There are two major ways that tumor IFP becomes elevated. First; the leakage of fluid and osmotic proteins from the blood into the interstitial space results in a reduction of hydrostatic pressure in the vessels and increase of colloid osmotic pressure in the interstitium. The lack of a lymphatic system enhances this problem. In addition to the influence of the architecture of the tumor vessels, there is also the role of the extracellular matrix and its contractile characteristics. The experiments have shown that normal fibroblasts grown in collagen gel will take on contractile characteristics and actively compress the gel (Steinberg et al, 1980). The process is mediated by stimulation from platelet-derived growth factor (PDGF),

transforming growth factor- β receptors and through the interactions of β 1 integrin and collagen (Clark et al, 1989; Nakamura et al, 2002).

Hemoconcentration, found due to fluid loss from the tumor vasculature (Vaupel et al, 87; Sevick and Jain, 1988), causes elevated viscosity of the blood resulting in increased resistance to flow (Vaupel, 2004; Jain, 1988). A significant increase in the aggregation and rigidity of RBC (red blood cells), fibrinogen and globulin concentrations, and plasma and blood viscosity has been reported in melanoma patients (Dintenfass, 1978). This increase in RBC aggregation has been reported in lung and bowel cancers (Dintenfass and Forbes, 1973, 1975), breast cancer (Riley, 1976) and in various carcinomas (Tietjen et al, 1977). The resistance of blood is regulated by the viscosity of plasma and the number, size, and rigidity of blood cells. The increased RBC aggregation may explain increased blood viscosity, and the associated elevated fibrinogen and globulin concentrations may explain increased plasma viscosity (Jain, 1988). Therefore blood flow through a tumor is more sluggish and inadequate. Impaired blood flow leads to reduced oxygen delivery through the tumor and contributes to regions of tumor hypoxia. Deviant vasculature and vessel density lead to an increase in geometric resistance to flow (Vaupel, 2004), consequently contributing to deficient perfusion.

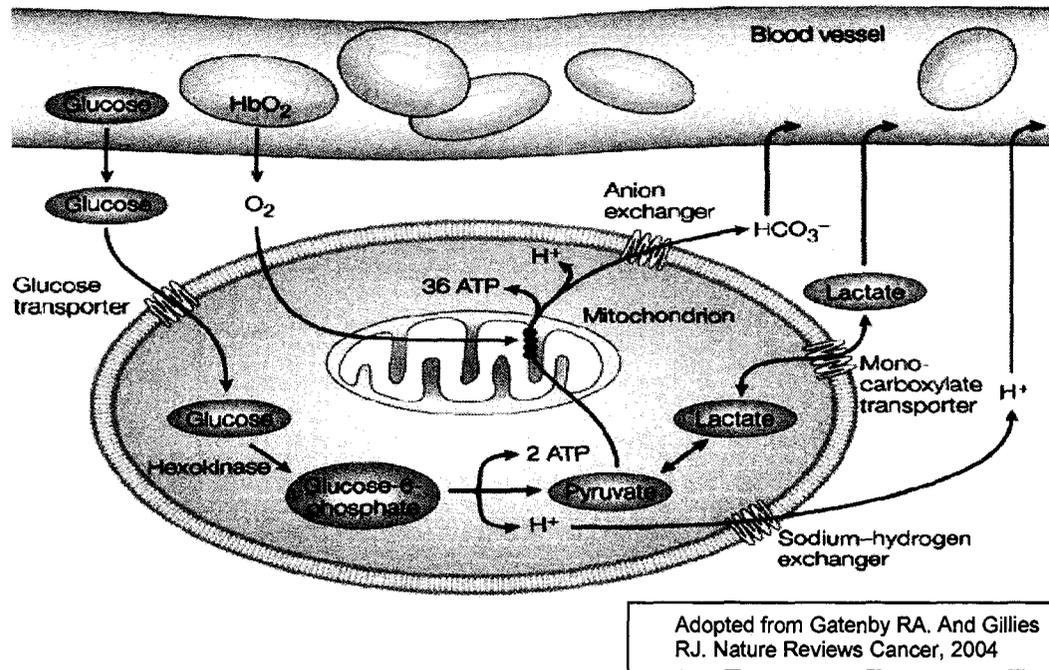
Poor perfusion and elevated metabolic rates are bases for the unique microenvironment characterized by regions of low oxygen (hypoxia) and low pH (acidosis) (Reynolds et al, 1996). The diffusion distances of glucose and other critical nutrients are similar to that of oxygen (Reynolds et al, 1996; Vaupel, 2004), and the uptake of glucose is limited by its delivery by the defective tumor blood flow (Kallinowski et al, 1988). Tumor characteristic vasculature is not only inefficient in the delivery of oxygen, but it can also

limit tumor tissue supply of energy sources and growth factors. Therefore, cells found at a distance from the nearest functional blood vessel may experience nutritional deprivation (Vaupel, 2004).

One of the properties of invasive cancers is altered glucose metabolism. Lysis of glucose, glycolysis, starts with conversion of glucose to pyruvate. In most mammalian cells, glycolysis is inhibited by the presence of oxygen, which allows mitochondria to oxidize pyruvate to CO_2 and H_2O . In cancer cells pyruvate is converted instead to a waste product, lactic acid (Figure 1.2). Conversion of glucose to lactic acid in the presence of oxygen is known as aerobic glycolysis or the Warburg effect, since this phenomenon was first observed by Warburg in the 1920s (Semenza et al, 2001). Increased aerobic glycolysis is specifically observed in cancers. Upregulation of glycolysis is likely to be an adaptation to hypoxia that develops as pre-malignant lesions grow further from the blood supply, and malignant cells in invasive cancers remain glycolytic even in the presence of oxygen (Gatenby and Gillies, 2004). Increased production of lactic acid results in acidic tumor microenvironment, with significantly lower pH of the extracellular space.

A significant amount of work has shown that tumor microenvironment enhances malignant progression and aggressiveness (Graeber et al, 1996; Kunz and Ibrahim, 2003). It has been shown that hypoxia, by selecting for mutant p53, tumor suppressor gene, may lead to more malignant phenotype of tumors (Graeber et al, 1996). Hypoxia is associated with metastasis of soft tissue sarcomas, cervix carcinomas, carcinomas of the head and neck (Brizel et al, 1997; Hockel et al, 1996, Flyes et al, 1998; Brizel et al, 1999; Nordmark et al, 1996; Rofstad, 2000a). It has been shown experimentally that hypoxia can lead to increased mutations (Reynolds et al, 1996). Clinical data support the

conclusion that hypoxia is a strong prognostic factor selecting for tumor metastatic spread.



Afferent blood delivers glucose and oxygen (on haemoglobin) to tissues, where it reaches cells by diffusion. Glucose is taken up by specific transporters, where it is converted first to glucose-6-phosphate by hexokinase and then to pyruvate, generating 2 ATP per glucose. In the presence of oxygen, pyruvate is oxidized to HCO₃, generating 36 additional ATP per glucose. In the absence of oxygen, pyruvate is reduced to lactate, which is exported from the cell. Note that both processes produce hydrogen ions (H⁺), which cause acidification of the extracellular space. HbO₂, oxygenated haemoglobin.

Figure 1.2 Glucose metabolism in mammalian cells.

Tumor hypoxia also stimulates tumor progression through hypoxia-inducible transcription factor-1 (HIF-1), which regulates most genes induced by hypoxia stimulating their transcription. More than 60 HIF-1 target genes have been identified. A large number of them are involved in angiogenesis, glycolysis, cell survival, and erythropoiesis. Some of these genes are vascular endothelial growth factor (VEGF), glucose transporters (GLUT), glycolytic enzymes and erythropoietin (EPO). (Semenza, 2002; Lu et al, 2002). Also, high tumor lactate levels predict an elevated risk of metastasis in head and neck carcinoma (Brizel et al, 2001) and cervical cancers (Walenta et al, 2000; Rofstad, 2000a; Hockel et al, 1996). The upregulation of glycolysis resulting in elevated glucose consumption, and the subsequent microenvironmental acidosis, lead to the evolution of phenotypes resistant to acid-induced cell toxicity. These cells have great growth advantage that promotes uncontrolled proliferation and invasion. It has been shown in numerous studies that the extracellular pH in tumors is acidic and can reach values of almost 6.0. It was demonstrated that H^+ ions from acidic tumors diffuse into peritumoral normal tissue (along concentration gradients). Normal cells are unable to survive in this environment, while tumor cells continue to proliferate. Acidosis can alone be mutagenic through inhibition of DNA repair (Gatenby and Gillies, 2004).

It has been shown that overexpression of IL-8 caused by hypoxia and acidosis plays an important role in tumor angiogenesis and in the aggressive biology of human pancreatic cancer (Shi et al, 1999). The expression of IL-8 by human ovarian cancer cells correlates directly with disease progression. It has been shown that acidic pH activates nuclear factor-kappaB (NF-kappaB) and activator protein-1 (AP-1) and consequently induced elevated IL-8 gene expression by human ovarian carcinoma cells (Xu and Fidler, 2000).

While tumor specific vasculature is in part responsible for regions of tumor hypoxia along with acidosis and elevated interstitial fluid pressure, the cells within the tumor contribute to the characteristic tumor physiology by responding to these changes.

The inflammatory responses in solid tumors can alter tumor microenvironment. Tumor-associated inflammatory cells and fibroblasts contribute to neoplastic progression in the early stages, by modulating synthesis and degradation of the extracellular matrix components, and allowing tumor to produce mitogenic and angiogenic factors that promote tumor growth and metastasis (van Kampen et al, 2003).

Cellular responses to tumor microenvironment

In vitro studies have shown that cells exposed to hypoxia had decreased cellular adenosine triphosphate (ATP) levels that are further decreased by exposure to low pH (Rotin et al, 1986). The concentration of ATP in human malignancies, consistent with these in vitro findings, was found to be lower than in normal tissues (Vaupel et al, 1989).

Cells exposed to conditions of tumor microenvironment and metabolic changes exhibit a reduced synthesis of the macromolecules. It has been shown that during hypoxia protein synthesis was reduced and protein degradation was increased (Pettersen et al, 1986). Hypoxia is also associated with a decrease in DNA synthesis (Graeber et al, 1994). One of the common cellular responses to environmental stress is reversible growth arrest by activation of the G1-phase check point. Probably G1/early S phase cell cycle arrest protects cells from advancing to S phase, when they are the most sensitive to killing by hypoxia (Amellem and Pettersen, 1991).

It has been demonstrated that hypoxia induces apoptosis (Graeber et al, 1996; Nelson et al, 2004). Apoptosis is a form of programmed cell death that is genetically encoded. The magnitude of apoptosis both in cell culture and in experimental tumors is promoted by the presence of functional p53. It has become apparent that the cellular inability to undergo apoptosis may have important consequences during neoplastic transformation. Damaged and possibly mutated cells that have lost the p53 tumor-suppressor gene or overexpressed the anti-apoptotic genes such as Bcl-2 are prevented from entering the apoptotic pathway. Instead, these cells survive and may go on to divide and expand the line of mutated cells, increasing carcinogenic risk. Hypoxia thus provides a physiological selective pressure in tumors for the cells that have lost apoptotic potential and particularly p53 mutants (Graeber et al, 1996).

Gene expression regulated by tumor microenvironment

To survive the extreme conditions of tumor microenvironment, tumor cells upregulate the expression of large number of genes as an adaptive mechanism. Some of these genes are, as categorized by their physiologic functions (Sutherland, 1998): glycolytic enzymes (phosphofructokinase, lactate dehydrogenase), glucose regulated proteins (GRP), glucose transporters, and growth factors that play an important role in tumor angiogenesis including vascular endothelial growth factor (VEGF), epidermal growth factor (EGF), transforming growth factor β (TGF- β), and platelet-derived endothelial growth factor (PDEGF). The gene products include proteins regulating the production of vasodilators, tumor suppressor genes and oncogenes, proteins involved in

maintaining redox homeostasis, and proteins involved in the regulation of signal transduction pathways (Dachs and Stratford, 1996).

Transcription factors are involved in expression of many cellular metabolism effectors. The most important such factor is hypoxia-inducible factor 1 (HIF-1). Many hypoxia-inducible genes are controlled by HIF-1 (Wang and Semenza, 1993) including genes involved in cell survival: insulin-like growth factor 2 (IGF2), transforming growth factor- α (TGF- α), and nitric oxide synthase 2 (NOS2). HIF-1 also increases glucose transport and anaerobic metabolism by activating glucose transporters (GLUT-1 and GLUT-3), and enzymes such as phosphoglycerate kinase-1 (PGK-1) and aldolase A (ALDA) (Wouters et al, 2004).

HIF functions also at the tissue level through up regulation of genes involved in angiogenesis and blood flow (VEGF and haem oxygenase-1) (Rofstad and Danielsen, 1999). Furthermore, HIF has an effect at the level of the whole organism by inducing erythropoietin (EPO) gene responsible for oxygen-carrying capacity of blood by involvement in the generation of hemoglobin (Wouters et al, 2004). HIF-1 is a heterodimer consisting of constitutively expressed HIF-1 β subunit and a HIF-1 α subunit, whose expression is highly regulated by hypoxia (Semenza, 2003). Even though not as well investigated as HIF-1, there are other transcription factors that play role in adaptive responses to hypoxia including early growth response protein (Egr1), nuclear factor- κ B (NF- κ B), and activator-protein 1 (AP-1) (Papandreou et al, 2005).

Potential mechanisms of microenvironment-induced tumor progression are proposed to be by DNA damage induced by hypoxia and/or reoxygenation leading to deletions, amplifications and genomic instability; selecting for metastatic cell phenotypes

and induction of specific genes involved in metastasis like HIF-1 α , VEGF, IL-8, TGF β . High lactate concentration, low extracellular pH and low glucose concentration probably induce metastasis by similar mechanisms as hypoxia (Rofstad, 1999, 2000b).

Hypoxia

One of the most investigated features of the tumor microenvironment is reduced oxygen content or hypoxia. While the oxygen tension in normal tissue is in the range of 10 to 80 mmHg, depending on the tissue type (Cairns and Hill, 2004), many tumors contain regions of decreased partial pressure of oxygen (pO_2), less than 10 mmHg. The significance of 10 mmHg pO_2 is that is when radiation resistance starts to develop (Vaupel et al, 1989; Steen, 1991) with full resistance occurring at values of less than 0.5 mmHg (Wouters and Brown, 1997; Brown, 1999). The pO_2 value at which cellular radiation sensitivity is midway between fully oxygenated and anoxic is approximately 3-4 mmHg. The hypoxic cell radioresistance is a result of lack of oxygen in the radiochemical process by which ionizing radiation is interacting with cells (Hall, 2000). In the last decade the threshold was set even lower, reporting levels of pO_2 less than 5 or 2.5 mmHg as hypoxic (Thews et al, 1999; Haider et al, 2004; Cardenas-Navia et al, 2004; Vaupel and Harrison, 2004). Precisely, we are talking about radiobiological hypoxia. These are levels of oxygen enough for tumor cells to stay viable, but they become more resistant to killing by irradiation.

The existence of hypoxia in solid tumors was first reported by Thomlinson and Gray over 50 years ago (1955). Since then, many investigators have shown that animal tumors contain radioresistant hypoxic cells, and that these cells play a significant role in

reducing the response to radiation treatment (Powers, 1963; Thomlinson and Craddock, 1967). It is believed that tumor hypoxia results from imbalance between the supply and consumption of oxygen or poor and inefficient perfusion (Vaupel and Hockel, 2003; Gillies et al, 2002). Numerous studies have clearly shown the presence of hypoxic areas in different human malignancies including cancers of the breast, prostate, uterine cervix, head and neck, rectum, pancreas, brain tumors, malignant melanomas and soft tissue sarcomas (Vaupel et al, 1987; Vaupel, 2004). Hypoxic regions are found in a wide range of tumors with evident intra- and inter-tumoral variability in the extent of hypoxia. These findings are independent of clinical size, stage, and histopathologic type (Vaupel et al, 2001). Two forms of tumor cell hypoxia were initially identified in tumors.

Diffusion-limited or chronic hypoxia develops in areas distant from functional blood vessels. This mechanism was first proposed by Thomlinson and Gray after examination of tissue sections of human lung cancers, noticing viable cells around regions of oxygen supply, and necrosis at distances consistent with the limit of oxygen diffusion in tumor tissue (~150 μm) (Thomlinson and Gray, 1955). Perfusion-limited or acute hypoxia results from transient occlusion of blood vessels producing fluctuations in blood perfusion of tumor regions (Brown, 1979; Sutherland and Franko, 1980; Chaplin et al, 1986). Vaupel and Hockel introduced the terms anemic hypoxia and hypoxemic hypoxia as separate forms (Vaupel et al, 2001). Tumor-associated or therapy-induced anemia can reduce oxygen transport capacity of the blood and contribute to the development of hypoxia. Tumor microvessels can be perfused by plasma only, and hypoxia develops around those vessels rapidly because of inadequate supply. In the mammary carcinoma model (R3230AC) it has been found that approximately 8 to 9 % of microvessels are

plasma channels, vessels that don't carry red blood cells, or very few (Dewhirst et al, 1996). Considering the broad range of the factors that influence oxygen transport, and oxygen consumption rate, it is evident that the initial classification of only two types of hypoxia in tumors is oversimplified (Dewhirst, 2003). Some of these factors are: lowered vascular density, intravascular pO_2 , blood viscosity. Dewhirst proposes a model to explain the bases for tumor hypoxia: in studies using skin-fold window chamber tissues they demonstrated a reduction in pO_2 in the longitudinal direction with respect to the arterioles that supply the tumor. Away from the arteriolar source microvascular pO_2 decreases, resulting in shorter diffusion distances and larger hypoxic zones between vessels. Tumor hypoxia has traditionally been thought to result from limitations of oxygen gradients in the radial direction from blood vessel (Thomlinson and Gray, 1955).

The rate of oxygen consumption is an important factor in tissue oxygenation since pO_2 depends on the supply of oxygen by the microvessels and on the local metabolic demand (Dewhirst et al, 1994; Thews et al, 1996). Malignant proliferation and aberrant metabolism increase the metabolic rate of tumors. Considering the demands involved in the replication of cellular organelles and chromosomes in addition to the physical division of a mother cell into two new ones, it is not surprising that the oxygen consumption rate of proliferating cells is three to five times higher than in cells not actively dividing (Vaupel et al, 1989).

Cancer cells display high rates of aerobic glycolysis known as the Warburg effect, where lactic acid is generated even in the presence of oxygen (Gatenby and Gillies, 2004). The upregulation of glycolysis and excessive production of lactate leads to an acidic environment within the tumor (Brizel et al, 2001). Across the cell membrane in

tumors there is a pH gradient with intracellular pH_i greater than extracellular pH_e (acidic outside, which is reverse of that found in normal tissue). The extracellular environment within tumor tissues has a median pH value 0.5 units below that of the surrounding normal tissues (Yuan and Glazer, 1998).

The presence of hypoxic cells in tumors is not only a major problem in radiation treatment but also leads to resistance to many anticancer drugs, and is associated with tumor progression and increased metastasis (Rofstad, 2000a), increased mutation rates (Reynolds et al, 1996), and increased expression of genes associated with angiogenesis and tumor invasion (Rofstad and Danielsen, 1999). Hypoxia-induced modification of gene expression may contribute to poor prognostic outlook, giving rise to more aggressive locoregional disease and enhanced invasive capacity. Low oxygen concentrations activate signaling pathways leading to the activation of transcription factors (Guillemin and Krasnow, 1997). As mentioned earlier, activated transcription factors are involved further in induction and control of many genes that play a role in adaptive responses to hypoxia. Even though there are numerous studies providing evidence that hypoxia is clinically associated with metastasis and poor prognosis, the underlying mechanisms remain unclear (Hockel and Vaupel, 2001). After finding that expression of extracellular matrix protein lysyl oxidase (LOX) in hypoxic human tumor cells is elevated (Denko et al, 2003), and its expression is regulated by HIF, in recent studies it has been shown that LOX correlates with metastatic disease and is essential for hypoxia-induced metastasis (Erler et al, 2006), and is good therapeutic target for the prevention of metastasis in breast cancer.

Experimental evidence suggested that hypoxia selects for tumor cells that have p53 mutations and consequently lost their apoptotic potential (Graeber et al, 1996; Kim et al, 1997). Hypoxia was found to induce apoptosis in tumor cells and further genetic alterations, such as loss of tumor suppressor gene p53 or overexpression of the apoptosis inhibitor protein Bcl-2. These observations lead to the suggestion that hypoxia provides a pressure in tumors selecting for cells with survival and growth advantage (Graeber et al, 1996). Following these findings, in human cervix carcinomas were identified tumors with a low apoptotic index that showed high probability for lymphatic spread and post-treatment recurrence (Hockel et al, 1999).

Numerous clinical studies performed in patients with soft tissue sarcomas (Brizel et al, 1996; Nordmark et al, 2001), head and neck cancers (Brizel et al, 1997, 1999; Nordmark et al, 1996, 2000), and carcinomas of the uterine cervix (Hockel et al, 1996; Fyles et al, 1998, 2002) indicated that presence of hypoxia adversely affects locoregional control and/or disease-free survival after primary radiation therapy. Therefore, hypoxia has a significant negative role in tumor prognosis. However, the low levels of oxygen are unique characteristic of tumors, which can be of therapeutic advantage. Targeting hypoxic regions of tumor, therapeutic strategies have potential to improve oxygenation or to kill tumor cells, relatively sparing normal tissues.

Correlation of tumor hypoxia to different treatment modalities:

As a Problem

The oxygen tension of tumors is an important determinant of their sensitivity to ionizing radiation. More than five decades ago Thomlinson and Gray established that

tumors contain oxygen-deprived regions, found beyond the limits of oxygen diffusion (Thomlinson and Gray, 1955). Pioneering studies of Gray and colleagues in early 50's (Gray et al, 1953) showed that hypoxic regions exhibited resistance to radiation damage. Numerous studies have confirmed that a dose of radiation kills oxygenated cells more efficiently than hypoxic cells. The difference in radiation sensitivity between aerobic and hypoxic cells expressed as the ratio of hypoxic to aerated doses needed to achieve the same biological effect, is known as the oxygen enhancement ratio and is normally 2.5-3 for sparsely ionizing radiations. The reason for this effect is that oxygen reacts with free radicals, the basic biochemical lesion produced by ionizing radiation. The consequences of radiation in the human body are mainly induction of DNA damage either by direct ionization of DNA or indirectly by the generation of free radicals. Free radicals are highly unstable and reactive due to their unpaired electron. Since 80 % of the cell is composed of water, free radicals induced by radiation are produced predominantly by the degradation of water molecules. As a consequence, reactive oxygen species (ROS) such as OH^\bullet , H_2O_2 or $\text{O}_2^{\bullet-}$ are generated. These free oxygenated radicals are strong oxidants that damage macromolecules such as DNA, but also cellular proteins and lipids. Oxygen reacts with the free electron of the free radical, "fixing" the damage, making it permanent (Hall, 2000). In hypoxic regions thus damage is not "fixed": it can be repaired.

There are different ways in which hypoxia might contribute to drug resistance.

Oxygen concentration may have direct effect on drugs, such as mephalan, bleomycin, and etoposide, which require molecular oxygen for maximum efficiency (Koch et al, 2003). Hypoxia causes cells to slow their proliferation slowing their rate of progression through the cell cycle, likely as a result of hypoxia-induced specific proteins (Sciandra et

al, 1984; Heacock and Sutherland, 1986). Since most of anticancer drugs are more effective against rapidly proliferating cells, this slowing of cell proliferation with increased distance from the vasculature will lead to decreased cell killing (Tannock, 1968; Amellem and Pettersen, 1991). Drug concentrations are higher closer to blood vessels. Many anticancer drugs are limited in their diffusion from the blood vessel that is delivering them, not only because of the greater distances needed to be diffused, but also because of their reactivity. Many of them, such as intercalators, bind to DNA (Brown, 1999). Tumor hypoxia might contribute to drug resistance through amplification of genes leading to drug resistance (Rice et al, 1986, 1987) or through the induction of various hypoxic stress proteins that are responsible for resistance to some chemotherapeutics (Murphy et al, 1994). In addition to hypoxia, other features of the tumor microenvironment can impact effectiveness of chemotherapy.

The high interstitial fluid pressure in tumors can present a barrier to efficient drug delivery by decreasing transport from the bloodstream into the tumor interstitium. This is especially important for large molecules, such as antibodies and other proteins. Several clinical studies have shown that elevated IFP was a poor prognostic factor for patient outcome (Milosevic et al, 1998, 2001; Rofstad et al, 2002; Fyles et al, 2006).

Low pHe (extracellular) and resulting tumor cell trans-membrane pH gradient can impact the effectiveness of chemotherapy. Many commonly used chemotherapeutic agents are either weak bases or weak acids. While the uncharged form of the drug equalizes in concentration across both sides of the plasma membrane, the uptake and activity of charged forms is altered. This leads to increased uptake of weak acids such as chlorambucil, while that of weak bases like vinblastine can be decreased. For some

chemotherapeutic agents, such as the anthracyclines, this pH gradient can lead to a 50% reduction in intracellular drug levels comparing to extracellular drug levels, allowing for “physiological drug resistance” (Evelhoch et al, 2000).

Hypoxia is also a problem in cancer treatment with photodynamic therapy. Photodynamic therapy (also known as a photoradiation therapy or photochemotherapy) is a treatment modality that is a combination of light and light sensitive agents, photosensitizers, in an oxygen-rich environment. The photosensitizer is administered systemically or locally and preferentially taken up by tissues having strong mitotic activity and achieving higher concentrations in tumor than in normal tissue. This drug is activated with light at a particular wavelength that has to match the absorption maximum of the drug. It does not react directly with cells. Instead, it passes its energy to oxygen to create a chemical radical “singlet oxygen”. PDT produces cytotoxic effects through photodamage to subcellular organelles and biomolecules only in the presence of oxygen (Figure 1.3).

As mentioned earlier, hypoxia is associated with the metastatic phenotype of cancers. Hypoxia may also decrease local control such as curability of tumors by surgery. This was observed in cervical cancer patients who underwent radical surgical treatment. It was found that tumors with a median $pO_2 < 10$ mmHg had larger tumor extensions, more frequent infiltrations and lymph-vascular space involvement comparing to tumors with a median $pO_2 > 10$ mmHg. Tumor oxygen status has been observed to be the most important prognostic factor for treatment outcome and metastatic free survival in cervical carcinoma after radiotherapy as well as surgery (Hockel et al, 1996).

Overall, hypoxia presents a barrier to the curability of solid tumors, regardless of treatment modality, and is an important biological consideration in cancer research.

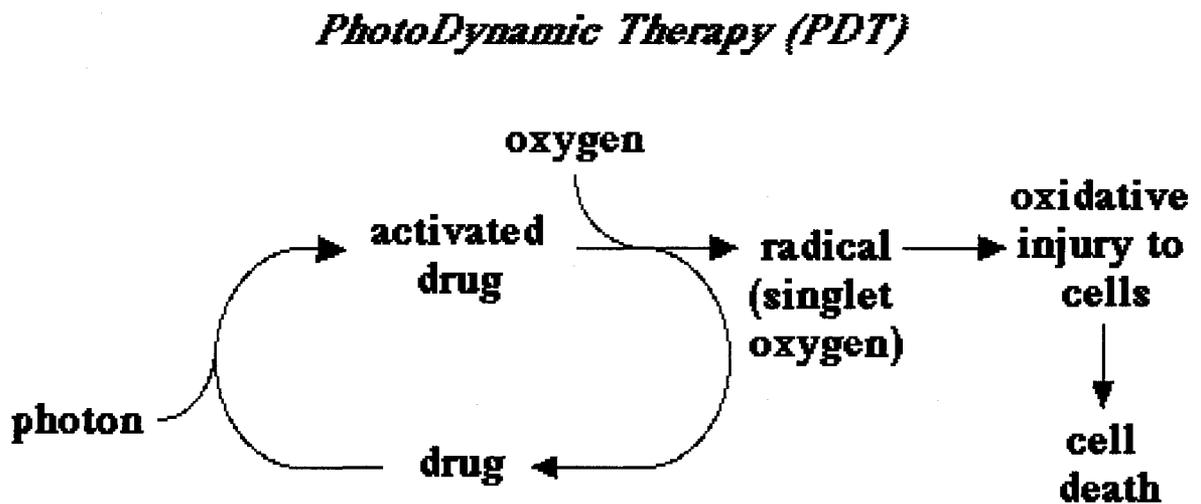


Figure 1.3. Schematics of the mechanism of action of Photodynamic Therapy.

Correlation of tumor hypoxia to different treatment modalities:

As an Advantage

Studying hypoxia in tumors has led to possibilities to use it as an advantage in a treatment of cancer. Two main strategies to overcome tumor hypoxia are to increase oxygen delivery or use oxygen-mimetic drugs, or to exploit tumor hypoxia for targeted therapy. The first strategy includes hyperbaric oxygen breathing, the administration of

carbogen and nicotinamide, and utilization of chemical radiosensitizers. The other strategy, using bioreductive drugs and hypoxia-targeted gene therapy, activates cytotoxic agents at the tumor site sparing normal tissues.

One of the first attempts to overcome the resistance of hypoxic tumor cells to radiation was to increase the oxygen level in the blood. This was performed by having patients breathe 100% oxygen at a pressure of 3 atmospheres in a hyperbaric oxygen chamber (Henk, 1986; Dische, 1991). Multicenter clinical trials showed an increase in locoregional control and survival in patients with cervix or advanced head and neck carcinoma treated with radiation and hyperbaric oxygen, compared with radiotherapy given to air breathing patients. However, these studies were discontinued mainly because of patient compliance (Greco et al, 2003).

A strategy has been devised to overcome both chronic and acute hypoxia, namely the combination of carbogen (95% O₂ and 5% CO₂), effective against chronic hypoxia and vitamin B derivative nicotinamide, which is believed to prevent transient blood flow fluctuation, has been tested in experimental models with success (Kjellen et al, 1991; Horsman et al, 1997). In clinical studies, this dual strategy was combined with radiation and has had some therapeutic efficacy, especially in treatment of bladder and head and neck malignancies. The treatment use was limited by gastro-intestinal toxicity of nicotinamide (Hoskin et al, 1997, 1999; Kaanders et al, 2002).

Hyperthermia has been shown to enhance radiation therapy (Thrall et al, 1996). It is well known that the delivery of hyperthermia therapy depends on the tumor vascularization: hyperthermia is more effective in poorly vascularized regions of the malignant tissue (Dewhirst et al, 1997). The mechanisms for the enhancement of radiation

therapy by hyperthermia varies based on the tumor temperature. Treatment with high temperatures $>42-43^{\circ}\text{C}$, may impact blood flow and actually increase tumor hypoxia. Treatment with mild hyperthermia ($41-42^{\circ}\text{C}$) has been shown to improve tumor oxygenation and has been used in number of studies (Vujaskovic and Song, 2004; Jones et al, 2004; Dewhurst et al, 2005). It has been suggested that this increase in oxygenation is due an increase in perfusion and also a decrease in oxygen consumption (Vujaskovic et al, 2000). Mild hyperthermia given before radiation may be effective in overcoming hypoxic radioresistance. There is evidence that addition of heat increased the effect of radiation therapy in many of the randomized studies (Perez et al, 1991; Overgaard et al, 1995; Vernon et al, 1996). Furthermore, the heat-induced increase in tumor oxygenation may significantly increase the effectiveness of thermoradiotherapy in combination with some chemotherapy drugs, which is also oxygen dependant. The results of phase I/II clinical trials show that trimodality treatment, consisting of hyperthermia, cisplatin, and radiation therapy is effective and feasible in different cancer types with tolerable toxicity (Bergs et al, 2007).

Radiosensitizers have been developed to sensitize hypoxic tumor cells. The first radiation sensitizer was 2-nitroimidazole. Results from studies on experimental animals with these drugs were quite striking (Sheldon et al, 1974; Brown, 1975), but human clinical trials showed severe neuropathy with multiple doses of misonidazole. This side effect restricted the dose of drug that could be used clinically with radiation treatment (Dische, 1985). Then more effective 5-nitroimidazole, known as nimorazole, was reported to improve the effect of radiation therapy in some head and neck cancers, with only mild toxicity (Overgaard et al, 1998).

Hypoxia can be used to advantage in treating tumors by selectively killing the hypoxic tumor cells. Bioreductive drugs such as mitomycin C have been utilized as hypoxia selective cytotoxins. For bioreductive drugs to be activated, the cells need to be hypoxic and to produce appropriate reductase enzymes. Bioactivation is restricted by the presence of oxygen in normal tissue. These drugs specifically kill cells resistant to radiation and chemotherapeutics, adding to their cytotoxicity. It also affects fluctuating hypoxia, and could be very effective if given with every radiation dose. However, drug mitomycin C could be given only twice during the radiation treatments. Nevertheless, clinical trials using this bioreductive drug in conjunction with radiation have shown the benefit of this combination (Weissberg et al, 1989).

The first hypoxic cytotoxin used in the clinic is from the benzotriazine di-N-oxide class of agents, known as tirapazamine or TPZ (Brown, 1999). Since TPZ is relatively ineffective in killing oxygenated cells it is not effective to be used alone in cancer treatment. TPZ in combination with fractionated radiation has been shown to potentiate cell killing by radiation (Brown and Lemmon, 1990). Combination of TPZ with cisplatin, however, had the most clinical success (Brown, 1999). Since the dose that can be administered in clinical trials during chemo or radiation treatment has been limited by toxicity like neutropenia, there is a need for improved hypoxia-induced prodrugs.

Another hypoxic cytotoxin, the anthraquinone AQ4N is promising and currently in clinical trials. AQ4N is a prodrug that gets activated in hypoxic cells to a stable cytotoxic product. Compared to TPZ, AQ4N shows an advantage since it can diffuse from hypoxic cells to kill the surrounding oxygenated cells, producing a bystander effect (Patterson and McKeown, 2000).

Besides using drugs that are toxic only to hypoxic cells, there are other ways to exploit tumor hypoxia in cancer treatment. One such approach is targeting some of the hypoxia-induced proteins such as transcription factor HIF-1 (hypoxia-inducible factor 1). The importance of the HIF pathway in tumorigenesis is very well established thanks to numerous experiments and a great amount of data in that field. Even though first discovered in 1993 (Wang and Semenza, 1993) this whole new field has become a topic of numerous investigations. Its role in angiogenesis, glucose metabolism, tumor cell survival and invasion, make it a potential tumor-specific target. Many of the enzymes involved in this pathway are potential therapeutic targets such as HIF-prolyl hydroxylases. Some of the proposed approaches to target high levels of HIF-1 α are: inhibition of transactivation of HIF-1 target genes, like vascular endothelial growth factor VEGF; suppression of HIF-1 protein levels by its destabilization or inhibiting its production; or find agents potentially toxic to cells expressing HIF-1 α (Brown and Wilson, 2004).

Another promising strategy is hypoxia-targeted gene therapy. Gene therapy can be explained as the transfer of genetic material (DNA or RNA) to modify the genetic repertoire of target cells for therapeutic purposes. Initially designed to treat inherited disorders caused by single gene defects (genetic diseases), the first clinical protocol was approved in 1989 (Rosenberg et al, 1990). Since cancer develops as the result of gene mutations, it might be effectively treated with gene therapy. Interest in research in cancer gene therapy has grown so that more than half of clinical trials now are cancer related. As an antitumor approach, gene therapy has the possibility to target tumor cells selectively by combining highly specific gene delivery and highly specific gene expression (Greco et

al, 2002). The successful gene therapy is dependent on the development of vectors with maximum efficiency and minimum toxicity. Its major limitation is the lack of specificity of the gene-delivery system. Instead of delivering vectors directly into the tumor by needle injection, it is better to have the therapeutic gene transcribed or translated by a tumor-specific property. HIF-1 is expressed in high levels in tumors but not in normal tissues, and stimulates the transcription of a number of genes via the binding of HIF-1 to sequences known as hypoxia-responsive elements (HREs) in the promoter regions of target genes. This fact is used to get hypoxia-specific transcription of a therapeutic gene by developing a promoter highly responsive to HIF-1. This way the expression of the therapeutic gene would be specifically obtained in tumors (Brown, 2002). The major approaches in the design of therapeutic genes for cancer gene therapy are genetic immunopotential, mutation compensation and molecular chemotherapy. In the first case, the insertion of genes that encode cytokines enhances tumor immunogenicity; mutation compensation is targeted towards inactivation of oncogenes or induces the expression of tumor suppressor genes. In molecular chemotherapy a “suicide” gene is delivered to the tumor cells (Dachs et al, 1997). The enzyme expressed by the therapeutic gene is not toxic, but is able to convert prodrug (non-toxic compound) into a cytotoxin. The latter system is known as gene-directed enzyme/prodrug therapy, GDEPT. This has advantages in both the amplification effect (each enzyme activates many prodrug molecules) and the bystander effect. The bystander effect can extend killing effects of the active drug to untransfected neighboring cells (Greco et al, 2000). The combination of hypoxia gene therapy and ionizing radiation is a promising approach in exploiting resistant hypoxic tumor cells.

Reoxygenation

Low oxygen level regions within tumors play an important role in tumor progression and tumor spread, and determine tumor susceptibility to killing by various anti-cancer agents. Since about half of all US cancer patients are treated with radiation therapy (Moeller et al, 2004), the possibility that tumor hypoxia may limit the response of fractionated radiotherapy has been very closely evaluated. Tumor hypoxia has been the subject of interest in many experimental and clinical studies and its role in resistance to radiation therapy, as well as the other treatment modalities, has been well documented. Hypoxic cells require up to three times more radiation than normoxic cells to reach the same level of cell killing (Gray et al, 1953). Clinically it has been reported that pretreatment oxygenation of different tumors predicts the tumor response to radiotherapy (Kolstad, 1968; Getenby et al, 88; Hockel et al, 1993; Nordmark et al, 1996; Brizel et al, 1997).

Tumor oxygen status has been proven to be very important for the outcome of patients treated with radiation. However, radiation itself also changes tumor oxygenation status. The phenomenon of hypoxic cells becoming oxygenated after a dose of radiation, known as reoxygenation, was first demonstrated in the late 1960's by work of van Putten and Kallman (1968). Since then it has been shown to occur in many experimental murine tumors (Olive, 1994; Horsman et al, 1995; Goda et al, 1995; Milas et al, 1995; Speke and Hill, 1995; Murata et al, 1996; Olsen and Rofstad, 1999; Bussink et al, 2000). Clinically it has been monitored by several authors in various human tumor types. Reoxygenation has been shown to occur in breast cancers (Pappova et al, 1982), carcinoma of the cervix (Sheridan et al, 2000; Cooper et al, 1999), and head and neck cancers (Brizel et al, 1999;

Lyng et al, 1999). The magnitude and time course of reoxygenation after radiation have been investigated in many experimental tumor models, revealing that the reoxygenation pattern could vary widely with the tumor type (Speke and Hill, 1995; Goda et al, 1995; Hockel et al, 1993), tumor size (Rofstad, 1989), irradiation conditions (Shibamoto et al, 1987), and dose of radiation (Hockel et al, 1996).

In many solid tumors reoxygenation appears within hours following radiation (Olive, 1994). Mechanisms governing tumor reoxygenation still remain unknown. Proposed explanations include extensive cell loss by apoptosis and tumor shrinkage (Milas et al, 1995; Kocher and Treuer, 1995), and consequently increased availability of oxygen to the surviving cells, decreased metabolic rate, decrease in oxygen consumption rates by radiation damaged cells (Kallman, 1972; Olive, 1994), reduced interstitial fluid pressure (Milosevic et al, 1998) as the tumor shrinks and improved microcirculation (Brown, 1979). It is also not known whether reoxygenation takes place primarily in chronic or acutely hypoxic tumor regions. It has been proposed that rapid reoxygenation may be present as a result of the resumed blood flow in acutely hypoxic areas of tumor (Brown, 1979), but that slow or inadequate reoxygenation is most likely the product of the slow process of removal of dead cells and tumor shrinkage (Horsman et al, 1995; Kocher and Treuer, 1995; Speke and Hill, 1995) with improvements in nutrient and oxygen status for chronically hypoxic areas. In the experimental tumors (SCC-VII tumors, Kitakabu et al, 1991) reoxygenation has been found to be biphasic after a single dose of 13 Gy, with rapid phase occurring within 1 hour, and a slow phase lasting 12-72 hours. With smaller doses, if applied in a number of 4 Gy fractions, more rapid reoxygenation was seen in 24 hour intervals between fractions. The work from the other

investigators, using different schedules of dose fractionation in experimental tumors, indicated that reoxygenation may not be rapid after an initial dose, but may improve over the course of fractionated radiation (Kallman et al, 1970; Rofstad, 1989).

Based on results obtained in numerous studies that measured the oxygen status of solid tumors before and post-radiation, it can be concluded that the radiocurability of tumors is probably influenced by the pretreatment hypoxic fraction as well as the reoxygenation pattern. Therefore, there is interest in knowing the extent to which reoxygenation occurs in radiation treated tumors. A better understanding of the changes in tumor oxygenation after radiation would allow for better planning of fractionated radiotherapy and its combination with modifiers of tumor microenvironmental parameters (blood flow, oxygenation, angiogenesis).

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CHAPTER 2

MULTIPARAMETER ANALYSIS OF TUMOR REOXYGENATION

INTRODUCTION

Ionizing radiation used as a therapy (radiation therapy) is one of the three major cancer treatment modalities, besides surgery and conventional chemotherapy. About half of all cancer patients are treated with radiation therapy, either alone or in combination with other types of cancer treatment. The therapeutic effect of radiation depends in part on the oxygenation status of the tumor. Hypoxic regions within tumors play an important role in tumor progression and tumor susceptibility to killing by various anticancer agents. Tumor hypoxia and its role in resistance to radiation therapy have been evaluated in many experimental (Gray et al, 1953; Kallman and Dorie, 1986; Rofstad, 1989; Murata et al, 1996; Goda et al, 1995; Fenton et al, 2001) and clinical studies (Getenby et al, 1988; Hockel et al, 1993; Nordmark et al, 1996; Brizel et al, 1997).

Interestingly, radiation itself may change the tumor oxygenation status. The phenomenon of reoxygenation has been investigated since its first demonstration in the late 1960's (van Putten and Kallman, 1968). Reoxygenation has been shown to occur in experimental murine tumors (Olive, 1994; Horsman et al, 1995; Milas et al, 1995; Murata et al, 1996; Bussink et al, 2000), and in various human tumor types (Pappova et al, 1982; Sheridan et al, 2000; Cooper et al, 1999; Lyng et al, 1999; Brizel et al, 1999).

Mechanisms responsible for reoxygenation have not been clearly established. We evaluated multiple physiological parameters in spontaneously developing canine tumors before and 24 hours after 3 Gy fractions.

In many solid tumors the increase in pO_2 begins within hours following irradiation (Olive, 1994; Crockart et al, 2005). Some experiments found reoxygenation in murine tumors to be biphasic following a single large dose of 13 Gy. The rapid phase of reoxygenation appeared within one hour of radiation, with a slower phase that lasted up to 72 hours (Kitakabu et al, 1991). With smaller doses applied in a number of daily fractions, more rapid reoxygenation was seen in between fractions. Clearly, the pattern of reoxygenation differs between different tumor types and among tumors of the same type. Even though extensively investigated, mechanisms underlying tumor reoxygenation remain unknown. Figure 2.1 is a diagram of suggested biological parameters that could impact tumor oxygen status following irradiation. We hypothesized that tumor reoxygenation was due to reperfusion of collapsed vessels after apoptotic cell death decreased interstitial fluid pressure.

To test this hypothesis, partial pressure of oxygen (pO_2), microvascular perfusion, apoptosis, interstitial fluid pressure (IFP), and microvessel density (MVD) were evaluated in the same tumor, before and 24 hours following the first fraction of radiation in 14 canine tumors. The aim was to investigate the relationship among tumor microenvironmental biological parameters and the oxygen level of tumors, looking at the changes of each of these parameters following a clinically relevant radiation dose (3 Gy). Understanding of the underlying physiological changes after radiation helps us develop strategies to exploit these changes to gain a therapeutic advantage.

MATERIALS AND METHODS

Research model

The Animal Cancer Center (ACC) at CSU is a great resource for cancer related research. Spontaneously occurring tumors in dogs are an excellent model for cancer research. Unlike experimental tumor models, canine tumors are heterogeneous. Most canine tumors have a histological counterpart in human cancer. The biological behavior and progression are often similar. The tumors also have similar tumor size to body mass ratios as found in human beings. Dogs are large enough to undergo sophisticated monitoring and the tumors are large enough for sequential biopsying.

In this study canine patients with solid tumors accessible for probe placement were eligible for the study. We entered 14 dogs into a study, 8 had soft tissue sarcoma (STS), 3 osteosarcoma (OSA), 2 carcinoma, and 1 mast cell tumor. Client consent was obtained for patient's entry into the study. Approval for the study was obtained from CSU Animal Care and Use Committee and the Hospital Clinical Review Board.

All of the measurements were made with dogs under general anesthesia. Dogs were premedicated with subcutaneously injected fentanyl at 0.006-0.008 mg/kg +/- atropine at 0.02mg/kg. Anesthesia was induced with a combination of midazolam or diazepam at 0.2 mg/kg and propofol 3 mg/kg to effect. Dogs were intubated and anesthesia was maintained with an admixture of Isoflurane and oxygen. Normosol-R solution was administered at 5-10 ml/kg/h during anesthesia. Irradiation was administered with a 6 MV photon beam from a clinical linear accelerator (Siemens, New York, NY).

The dose delivered was 3 Gy and all measurements were performed immediately before and 24 hours after irradiation.

Oxygen measurements

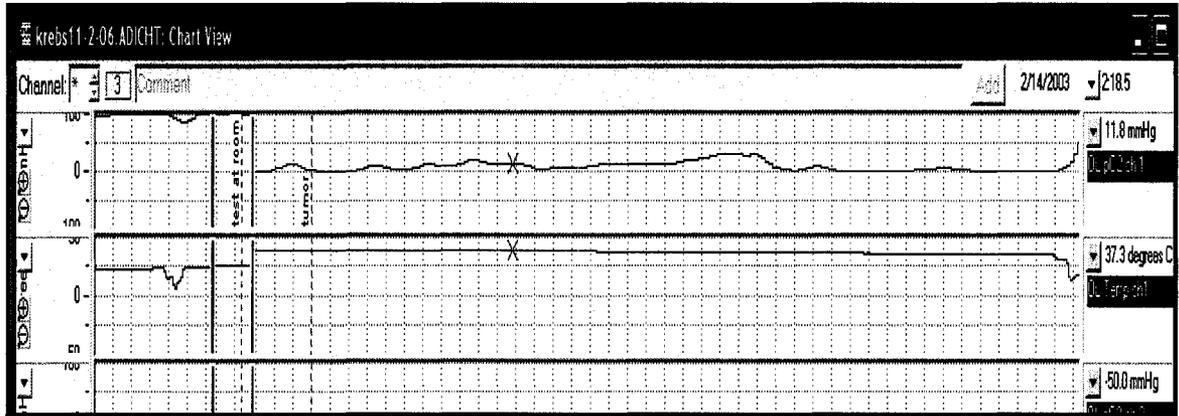
Simultaneous measurements of pO_2 , temperature and microvascular perfusion were obtained with Oxford Optronix system (Oxford Optronix Ltd, Oxford, UK) OxyLite and OxyFlow.

Tumor oxygenation measurements were obtained using OxyLite. This is a time-resolved luminescence-based optical sensory system. This system uses a fiber-optic probe that contains a fluorescent dye (a platinum-based fluorophore) immobilized at the tip. Light is emitted along the probe to excite a fluorophore at the tip. The resulting emission of fluorescent light, quenched by the presence of oxygen molecules, travels back along the fiber and is detected by the instrument. The lifetime of the fluorescent dye is inversely proportional to the concentration of dissolved oxygen in tissue, providing the value for pO_2 in mmHg. The fluorescent lifetime is longest at low pO_2 , making probes most sensitive under conditions of tumor tissue hypoxia. Because these sensors do not show significant consumption of oxygen, they are a better choice for measuring tissue oxygenation than paleographic electrodes. Not only conventional paleographic techniques consume oxygen that is most evident under conditions of tissue hypoxia, but require complex and time consuming calibration procedure which is avoided with OxyLite sensors by providing pre-calibrated probes. Another advantage of this system is the possibility to combine it with laser Doppler blood perfusion monitors for

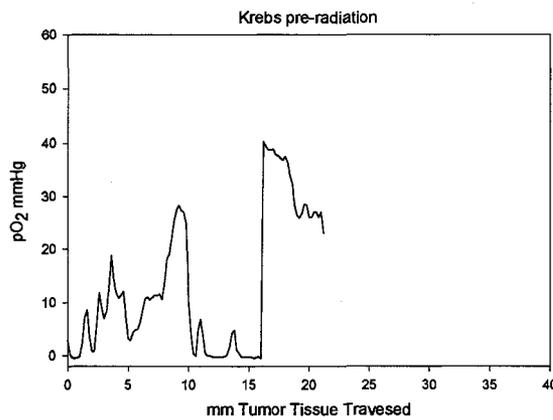
simultaneous multi-parameter monitoring. We used combined probes for pO₂, microvessel perfusion and temperature measurements from the same tumor microregion. To perform measurements at multiple locations across the tumor a digitalized caliper was adopted to pull back the probes. The probes were introduced through microdialysis split tubing (CMA/Microdialysis AB, North Chelmsford, MA), placed in the tumor with a 20-gauge catheter. After initial stabilization of recording measurements, the probe was withdrawn 0.2mm each 5sec and measurements were displayed using a data-acquisition system Chart v.4.2.4 (AD Instruments, Inc., Colorado Springs, CO). Histograms were created using SigmaPlot v.7.101 software (Systat Software Inc., San Jose, CA) (Figure 2.2).

Interstitial fluid pressure measurements

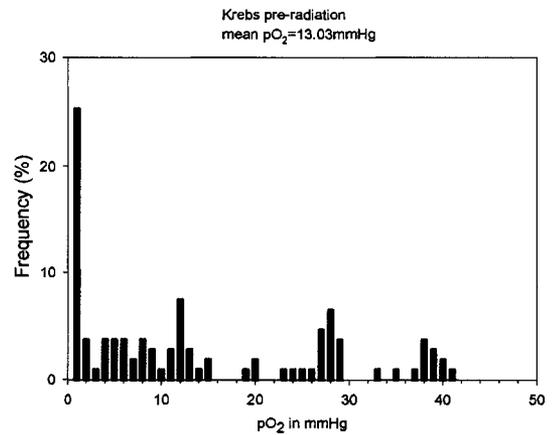
The interstitial fluid pressure (IFP) was measured using a modified “wick-in-needle” technique (Fadnes et al, 1977). Wick-in-needle probes were custom made from 22-gauge spinal needle with a 3 mm side hole located 5mm from the tip. Standard cotton thread was threaded into each needle before sterilization. The needle was connected to a pressure transducer by polyethylene tubing filled with heparinized saline solution (100 IU/ml) to prevent clotting. Instrumentation was calibrated to zero at room air before each measurement. A zero reference was obtained by placing the needle at tumor height and by resetting the system. Measurements were recorded at 0.5 cm intervals across the tumor starting at the periphery of tumor under the skin.



A.



B.



C.

Figure 2.2. Data obtained with Chart (A), and processed in SigmaPlot to present pO_2 track of measurement (B) and pO_2 histogram (C). Histogram represents percent frequency of pO_2 values measured at 0.2 mm intervals.

Microvascular perfusion measurements

Tumor perfusion was assessed by two complementary techniques: laser Doppler flowmetry (LDF) and dynamic contrast-enhanced (DCE) imaging. In the first five tumors, DCE was done using computed tomography (DCE-CT) and upon availability of

magnetic resonance imaging at the Animal Cancer Center we used dynamic contrast-enhanced MRI (DCE-MRI).

Laser Doppler Flowmetry

OxyFlow is part of the Oxford Optronix system that measures microvascular perfusion with laser Doppler flowmetry (LDF). It contains the laser source, sensitive photo detection and signal processor. Probes contain optical fibers that direct stable low power laser light to the tissue and collect scattered light to a photo detector. The presence of moving red blood cells in capillaries, arterioles, and venules in the tissue cause a Doppler shift in the fraction of returned light and it is this shift which constitutes the output signal. The signal is more correctly described as related to tissue perfusion rather than blood flow, as it cannot be directly calibrated in units such as ml/min.

Perfusion is indicated on a display in relative blood perfusion units (BPU) defined using a carefully controlled motility standard. Microvascular perfusion is proportional to the number of red blood cells moving in the tissue sampling volume under illumination from the probe, and mean velocity of these cells. The mean tumor blood flow was presented as a graph using SigmaPlot v.7.101 software (as an example given in Figure 2.3).

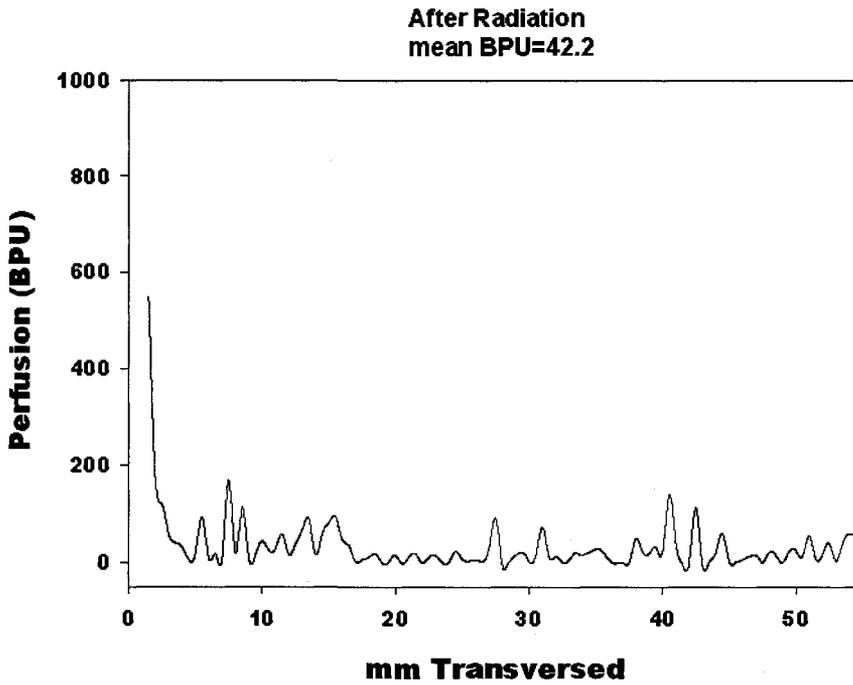
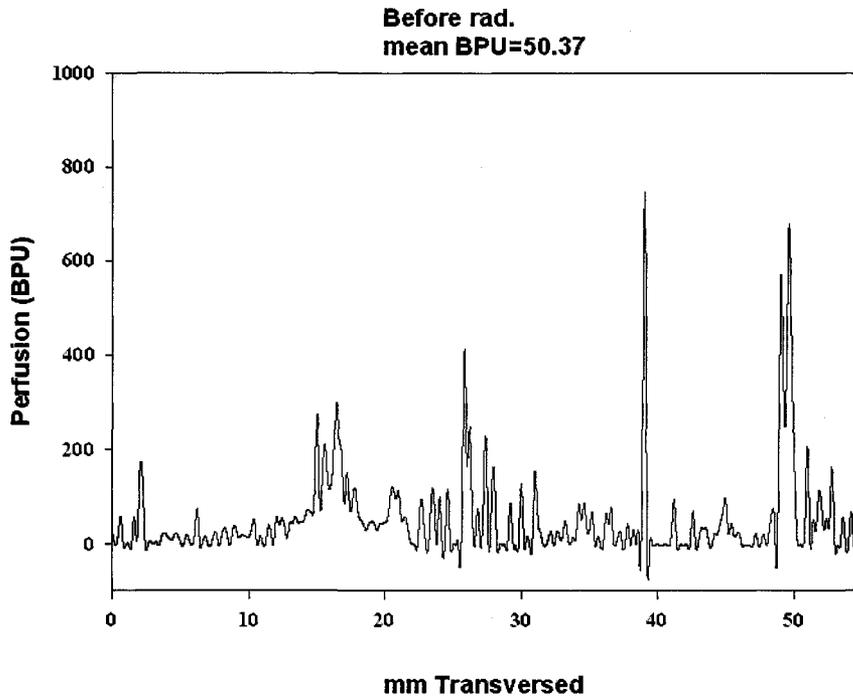


Figure 2.3. The changes in microvascular perfusion (measured via laser Doppler) along the probe track both before (left graph) and 24 h after radiation (right graph) in a canine tumor.

Dynamic contrast-enhanced CT

We also evaluated perfusion using quantitative dynamic contrast-enhanced computed tomography (DCE-CT). The use of wash-in kinetics of contrast medium was utilized to estimate perfusion. Images were acquired using a Picker PQ 2000 CT (Picker International, Highland Heights, OH).

An initial non-contrast CT scan was performed to evaluate the extent of tumor involvement. The imaging plane was repositioned at the central location of tumor (this slice was also the location of oxygen and interstitial fluid pressure measurements that were performed after CT).

Contrast agent was injected in the cephalic vein using a pressure injector at the rate of 3 ml/sec, 100 psi maximum, using a dose of 1 ml/lb body weight of sodium diatrizoate (370 mg/ml iodine) with a maximum dose of 60 ml. Tissue and vessel attenuation (“density”) changes were observed during the first pass of the agent by rapid image acquisition. Image acquisition started just prior to contrast injection. Dynamic acquisition was performed using one image per 2 seconds for total of 40 images. Slice thickness was 5 mm (Figure 2.4).

Perfusion was estimated by assessing the uptake of contrast medium into the tumor compared to the concentration in the arterial supply as an input factor. Time-density (Hounsfield units) curves were constructed for regions of interest (ROI) drawn over the nearest major artery and the tumor (Figure 2.5). Tumor ROIs were drawn at the locations of tumor oxygen measurements. Arterial ROIs were chosen for an artery within the scan plane during the dynamic acquisition.

Tumor perfusion estimation was calculated as described in Van Camp et al. 2000.

Tumor perfusion was expressed as rate of rise of attenuation (Hounsfield units) in the tumor over the arterial attenuation (Hounsfield units) value over the same time points (Figure 2.6). Values obtained for perfusion are in units of ml/sec/ml.

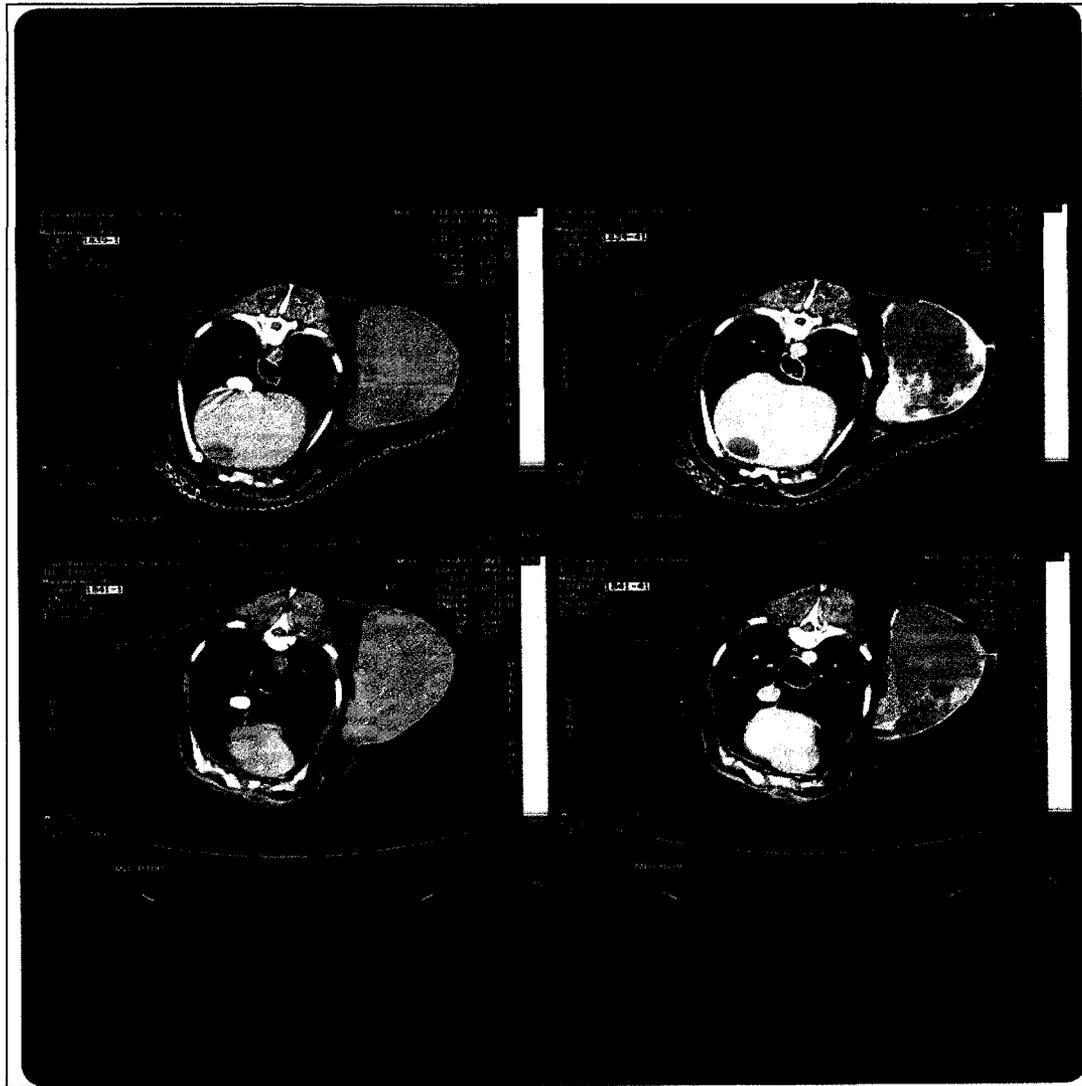


Figure 2.4. Tumor CT images of a large canine extrathoracic tumor show at the location of perfusion measurements. The tumor is the large grey area along the left side of the thorax (patients left is on the images on the right side). The heart and diaphragm are visible centrally in the chest on each image. Iodinated contrast medium was administered intravenously using pressure injector. Images are taken before (upper images), and 24h after irradiation (lower images). Images on the left were obtained at the beginning of the contrast injection, while images on the right were later in the series. Note the needle positioned to assist probe placement for subsequent measurements.

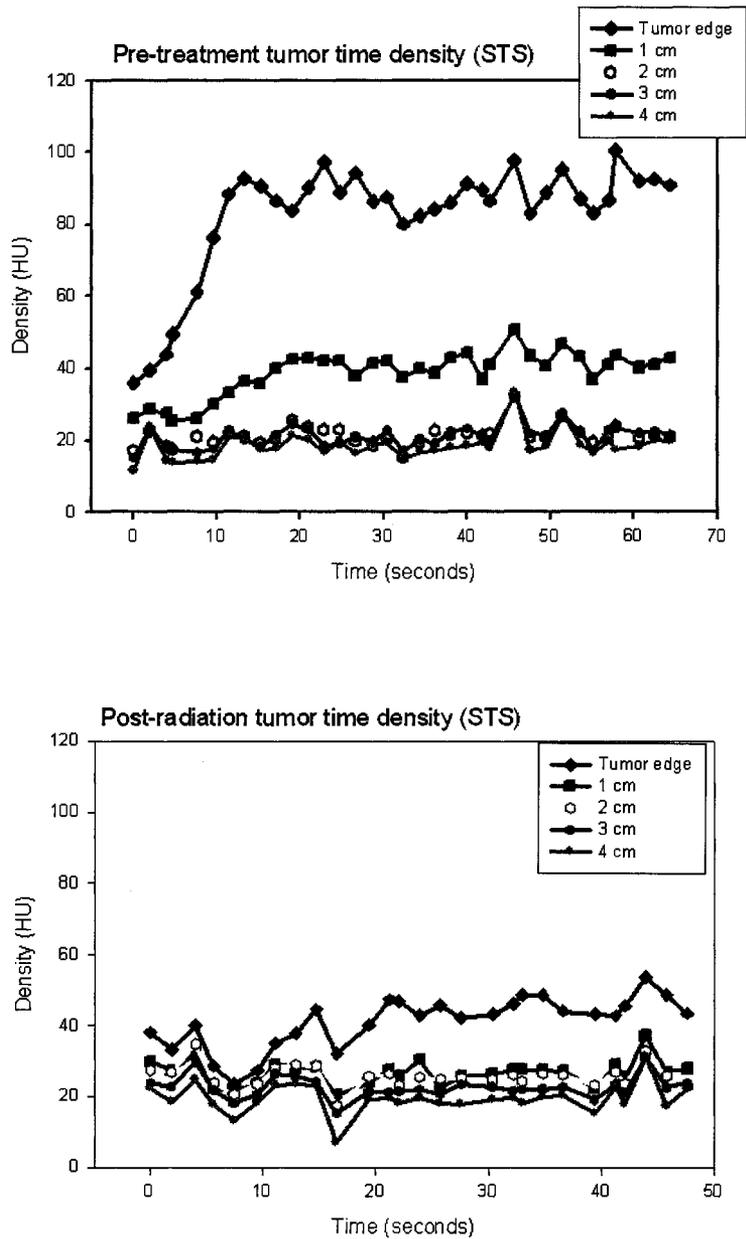


Figure 2.5. Time-density curves of tumor Hounsfield units (HU) plotted as a function of time after contrast injection are constructed for various regions of interest (ROI). ROIs are drawn at different depths along the needle position seen in figure 2.3.

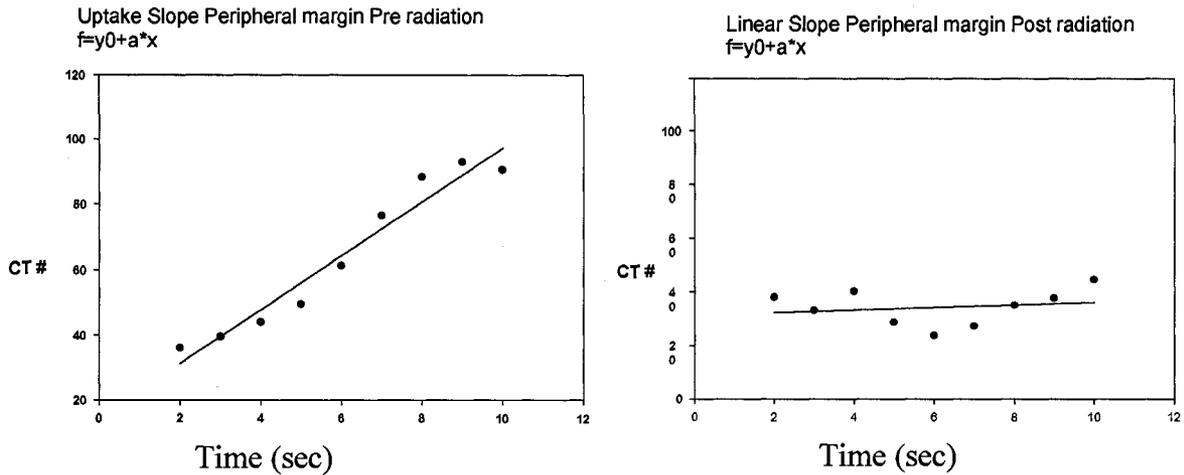


Figure 2.6. DCE-CT data was calculated as Δ tumor HU / Δ arterial HU derived from CT time density curves. Time-density curves were generated for the tumor ROIs and the largest artery in the imaging field. The slope of increasing tumor density was divided by the peak arterial density to obtain an estimate of perfusion.

Dynamic contrast-enhanced MRI

After the first five tumors entered our study we continue to measure tumor perfusion with dynamic contrast enhanced magnetic resonance imaging DCE-MRI instead of DCE-CT, still followed by LDF measurement. Tumors were imaged with dogs under general anesthesia, with a 1.5T GE Signa LX 9.0 MRI instrument (Signa, GE Medical Systems, Milwaukee, WI) using a coil appropriate for the body region. Anatomic T2 and T1 weighted pulse sequences were obtained to first evaluate tumor morphology. The dynamic contrast-enhanced scan was acquired as a T1 fast spin echo sequence (TR 400 ms, TE 15 ms, matrix 256X128, NEX 0.5) and the entire tumor volume was imaged repeatedly in 30-35 second phases for a total of 15 transverse slices, with thickness of slice from 5-10 mm. The field of view (FOV) was as small as possible. Gadolinium DTPA (Magnevist, Berlex Laboratories, Trenton NJ) contrast medium was administered

intravenously as a bolus using a pressure injector at 0.1 mmol/kg at a rate of 2.5ml/sec.

The dynamic acquisition was done after contrast injection for a total of 30 minutes.

Afterwards the skin on the tumor was marked for the probe placement for the subsequent physiological measurements and biopsy.

Analysis of the DCE-MRI was done using an “intensity based” method (Belfi et al. 1994). Time-intensity curves were generated for regions of interest (ROIs) that were drawn at the location of subsequent probe placement, for interstitial fluid pressure and partial pressure of oxygen measurements. Similar ROIs and slices were analyzed before and after radiation (Figure 2.7).

The ROI signal intensities were first converted into percent intensity values (%IE) by subtracting out baseline intensity (from pre-injection) and dividing by that pre-contrast intensity value:

$$\%IE = (\text{new intensity} - \text{background intensity}) / \text{background} \times 100$$

This signal intensity data was then fitted to a two compartmental analysis (done by Dr. Susan Kraft) to derive α , β , and A using the formula:

$$\%IE = A (1 - e^{-\alpha t}) e^{-\beta t}$$

with a standard commercial software package SigmaPlot 8.0.

A Relative Perfusion Index (RPI) was then calculated as: $RPI = \alpha A$, to characterize the uptake portion of the contrast dynamic curve. RPI was compared for each ROI before and after radiation (Figure 2.9).

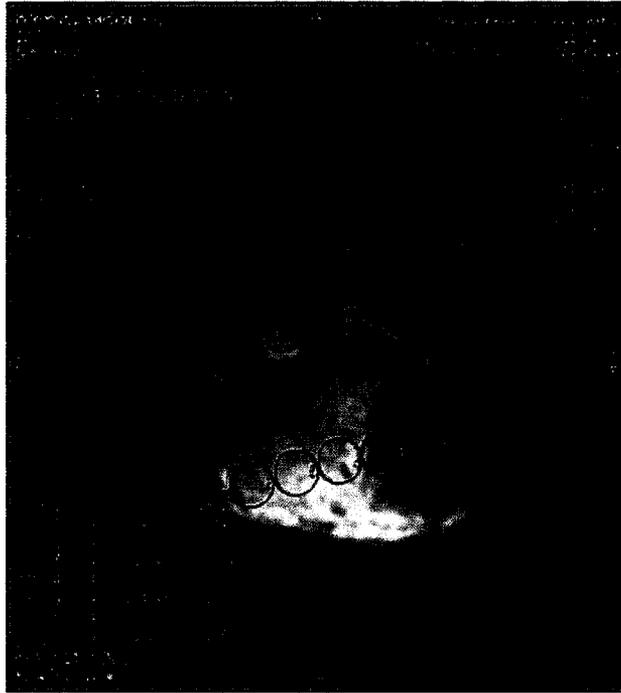


Figure 2.7. MRI image of a soft tissue sarcoma of the forelimb of a dog at the location of perfusion measurement, correlating to other parameters of interest. Regions of interest (ROI's) (numbered circles on the image) were drawn at the LDF probe placement location. Corresponding ROIs were drawn on post-radiation image and graphs obtained for the uptake of the contrast at different depths of tumor, as in figure 2.7. The contrast-enhancing tumor is hyperintense (white). The circular darker area is a necrotic center to the tumor. Normal musculature (dark grey in upper left) and cross sections of the normal radius and ulna are included in this image.

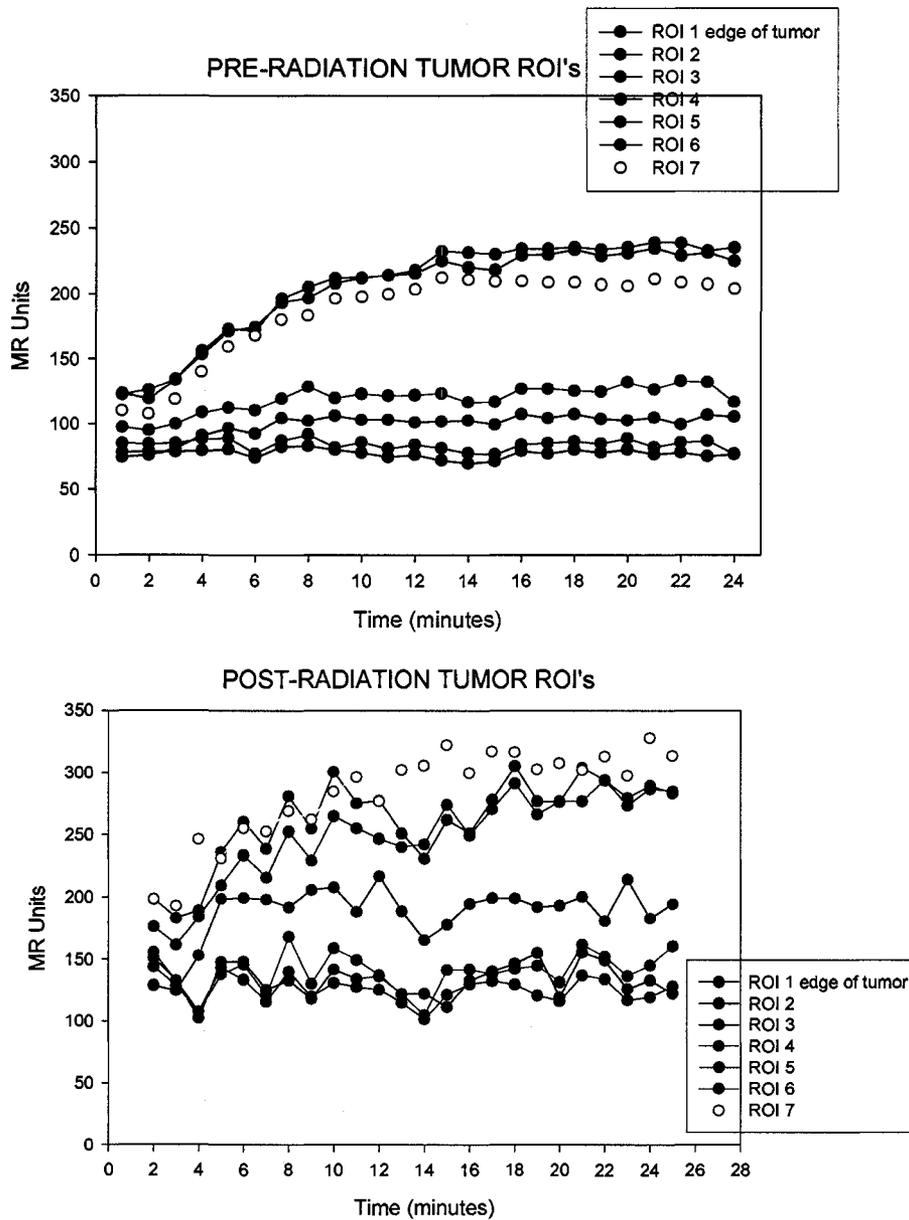


Figure 2.8. The ROI signal intensities: Curves of tumor MR units plotted as a function of time after contrast injection, were constructed for various regions of interest (ROI). ROIs are drawn at different depths, along OxyFlow probe placement, before and after radiation.

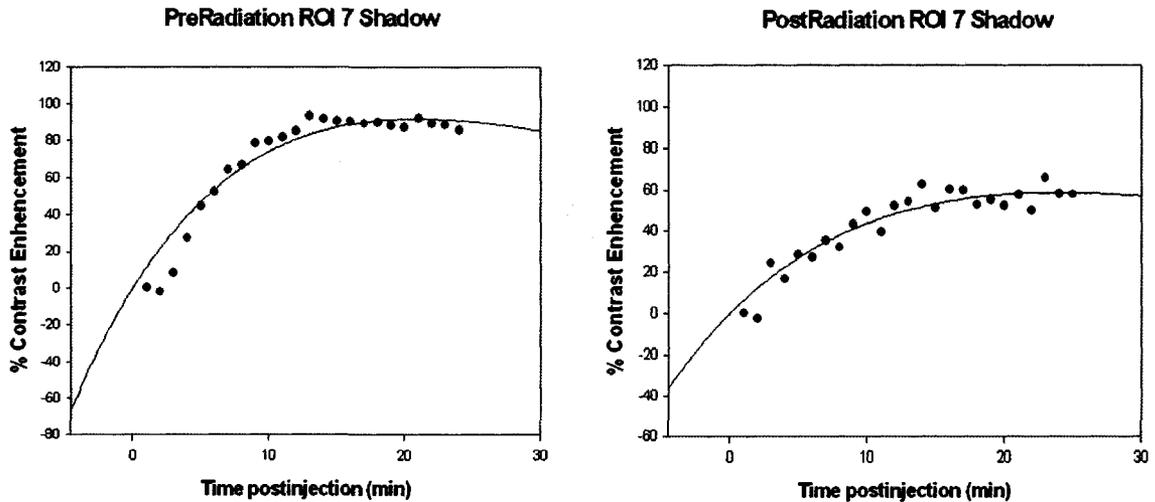


Figure 2.9. DCE-MRI data was calculated as a Relative Perfusion Index and compared for each ROI before and after radiation. The ROI signal intensities were first converted into % intensity values (Belfi et al. 1994): $\%IE = [(I_{post} - I_{pre}) / I_{pre}] \times 100\%$. This is the same tumor shown in MRI image in figure 2.7 and in ROI signal intensity curves in figure 2.8.

Apoptosis quantification

Needle biopsies were performed after each probe measurement to obtain tumor samples for quantification of apoptosis and microvessel density. In the first 4 dogs the biopsies were taken before, and 24 hours after radiation. Starting with dog 5 an additional time point at 6 hours after radiation was included. Paraffin embedded slides for immunohistochemistry, and hematoxylin and eosin stained slides were obtained from the tumor biopsies.

Apoptosis was measured in paraffin embedded histological sections of the tumor.

Sections were stained by use of the In Situ cell death detection kit, Fluorescein (Roshe Molecular Biochemicals, Indianapolis, IN). The staining was based on the terminal

deoxynucleotidyl transferase (TdT)-mediated deoxyuridine triphosphate (dUTP)-biotin nick end labeling (TUNEL) method.

Using the TUNEL assay, the apoptotic fraction was expressed as percentage of TUNEL positive cells. Analysis was performed using KS 400 system software (Carl Zeiss MicroImaging, Inc., Thornwood, NY). For each tissue section images were taken using a Carl Zeiss Axioplan 2 imaging microscope coupled with an AxioCam HRc Carl Zeiss camera. Nine to ten areas of the tumor specimen were identified, counting was performed at X 200 magnification and the percentage of the apoptotic cells was calculated. It was expressed as an apoptotic index (AI):

$$\text{AI} = \frac{\text{\# of Fluorescein labeled cells} \times 100}{\text{\# Fluorescein labeled} + \text{DAPI labeled cells}} \%$$

For standardization, the measured fields were size 150X100 microns.

TUNEL Protocol

This protocol is used for detection and quantification of apoptosis at single cell level, based on labeling of DNA strand breaks. One of the characteristics of the apoptosis is the fragmentation of nuclear chromatin which results in a multitude of 3'-OH (hydroxyl) termini of DNA ends. These DNA strand breaks can be identified by labeling free 3'-OH terminal with modified nucleotides in an enzymatic reaction. This is the modified protocol used in this study:

1. Deparaffinize slides in HemoDe, 2 times for 5 min.
2. Rehydrate in a series of EtOH (100, 95, 90, 80 70%) for 5 min each.
3. Wash in PBS for 2 min.

4. Incubate slides in Proteinase K (PK) in a water bath for 30 min @ 37°C. To prepare PK: 66.5 µl/50ml 10mM Tris HCl. Tris HCl 10mM= 0.1576 g/100ml diH₂O.
5. Wash in PBS 2 times for 2 min each.
6. Centrifuge PN buffer and milk (to take off background noise), 5-7 min.
Dry around the tissue and circle with PapPen. Add 30 µl of supernatant on slide, place a cover slip and keep 5 min at room temperature.
7. Prepare TnT in dark: take out 100 µl from vial 2 (Label solution) and add all 50 µl of vial 1 (Enzyme) from the TUNEL kit. Add 100 µl to each slide.
8. Incubate in a humidified chamber (box with wet paper and covered with foil), at 37°C for 60 min.
9. Wash in PBS, 3 times for 2 min. each.
10. Prapere 10 µl RNase + 90 µl PBS (100 µl). Apply 100 µl on each slide and leave for 60 min in humidified box at room temperature.
11. Dry around the sample and apply AntiFade and DAPI (counterstain). (SlowFade light AntiFade kit, Molecular Probes, Inc., Eugene, OR and Sigma-Aldrich, St. Louis, MO, respectively). DAPI stock solution: 10 mg/ml in dH₂O. Use 1 µg/ml stock solution in SlowFade. Place cover slip.
12. Dry in dark overnight. Then keep slides at -20°C.

Microvessel Density

Quantification of microvessel density (MVD) was performed using immunohistochemical staining of endothelial cells for factor VIII-related antigen (von Willebrand factor). Immunohistochemical staining was performed in the Diagnostic lab of The Veterinary Teaching Hospital, using standard immunoperoxidase technique on an automated stainer (Discovery System, Ventanna Medical Systems, Tucson, AZ). All reagents were purchased from Ventanna Medical Systems, and incubated at 37° C. Briefly, 4 micron sections were cut and mounted on positively charged slides. The sections were deparaffinized then rehydrated with descending alcohol concentrations to buffer. Antigen retrieval was with protease 1 incubation for 8 minutes. The sections were then incubated in the primary antibody anti factor VIIR, polyclonal, 32 min at 37°C. A pre-diluted, universal biotinylated secondary antibody, an alkaline phosphatase red basic kit detection system, and fast red as chromogen were utilized to detect the immunoreactive complexes. The slides were counterstained with hematoxylin and bluing for 4 min each. Image analysis was performed using KS 400 system software (Carl Zeiss MicroImaging, Inc., Thornwood, NY). Microvessel density was assessed in areas of highest neovascularisation found by scanning the tumor sections, “hot spot” technique (Weidner N.’91). Microvessel counts of these areas were performed at high-power field (X 200). Any brown stained endothelial cell or endothelial cell cluster that was clearly separated from adjacent microvessels, tumor cells, and connective elements was counted as one microvessel, irrespective of the presence of a vessel lumen. For the consistency in the MVD analysis the grid containing 100X150 micrometer squares was placed over the

images while counting. The vessels were counted in five to seven squares, depending on the tissue slice size, and the mean count was taken as the MVD (Figure 2.10).

Statistical analysis

Five pO₂ parameters were calculated for each tumor from pre and post radiation measurements: mean pO₂, median pO₂, fractions of pO₂ readings < 2.5 mmHg, 5 mmHg, and 10 mmHg. Two microvascular perfusion methods were performed for each tumor for pre and post radiation measurements: LDF and DCE CT/MRI. All tumors were divided in two groups regarding pO₂ measurements before treatment: hypoxic tumors with median pO₂ values < 10mmHg, and non-hypoxic tumors with median pO₂ before radiation ≥ 10mmHg.

Statistical analyses were performed to explore whether there was an association between changes in tumor oxygen levels and changes in other microenvironmental parameters obtained in all pre- and post-radiation measurements in all tumors. For normality p-value, paired t-test p-value, signed rank test p-value, and mean and standard deviation of the difference between measurements after and before radiation, Shapiro-Wilk tests were performed. Pearson and Spearman correlation coefficients and p-values for the association between changes in pO₂ and changes in microvascular perfusion, MVD, IFP, and apoptotic index were calculated. Pearson and Spearman correlation coefficients and p-values were used to compare pre and post radiation perfusion measurements performed by LDF and measurements by CT/MRI.

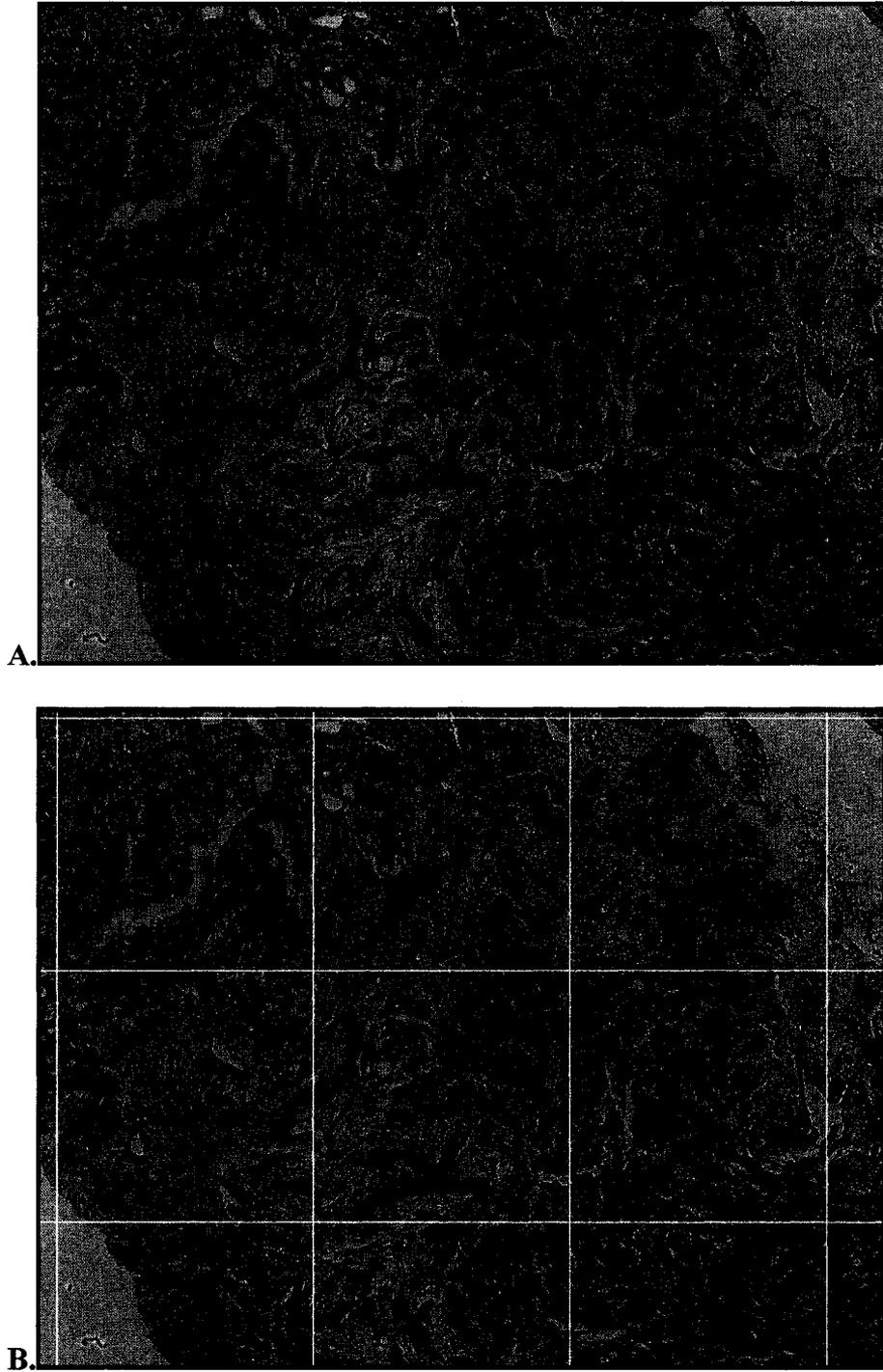


Figure 2.10. Immunohistochemical visualization of microvessels (arrows) in a dog mammary carcinoma. The section of tumor was stained for factor VIII-related antigen. Selected field (A) is a “hot spot” where counting was performed using a known size grid overlapping the field (B).

Chi Square test and Fisher's exact test were used for the changes in median pO_2 vs. other parameters, and for the changes in mean pO_2 vs. other parameters (microvascular perfusion, MVD, IFP, AI) to complete the statistical analysis.

RESULTS

Oxygen measurements

Oxygen measurements were analyzed along the track of a probe that was placed into a tumor and withdrawn toward the edge. All pO_2 values were expressed as mean and median pO_2 in mmHg. Tumors with mean/median O_2 levels above 10 mmHg were defined as normoxic. The fraction of measurements along the track with pO_2 values < 10 mmHg, < 5 mmHg, and < 2.5 mmHg was calculated (Table 2.2). The pO_2 changed after radiation; in 9 tumors it increased, and in 5 tumors it decreased (both mean and median pO_2). Tumors that were pre-radiation hypoxic mostly reoxygenated: 6 out of 7 hypoxic tumors showed increased level of oxygen measured after radiation (3Gy) compared to measurements before treatment. In the same 6 initially hypoxic tumors the percent of the measurements less than 10, 5, and 2.5 mmHg decreased after radiation. The magnitude of the change differed among the tumors. For the 7 initially well oxygenated tumors: 3 of them had increased pO_2 after radiation, while 4 of them had decreased pO_2 but still in the range of oxygenated regions (not becoming hypoxic). For the best comparison each tumor pO_2 measurements are presented in histograms, before and after radiation, set next to each other on the same scale and analyzing the same track of the measurements length

in Figure 2.14, Figure 2.15, Figure 2.16, Figure 2.17, Figure 2.18, Figure 2.19, Figure 2.20, Figure 2.21, Figure 2.22, Figure 2.23, Figure 2.24, Figure 2.25, Figure 2.26.

Table 2.2. Partial pressure of oxygen measurements in 14 tumors.

DOG #	OX Y G E N				pO ₂					
	Before Mean	After Mean	Before Median	After Median	%<10 mmHg Before	%<10 mmHg After	%<5 mmHg Before	%<5 mmHg After	%<2.5 Before	%<2.5 After
1	2.2	12.3	-0.5	-0.1			88.1	62.1	86.2	61.1
2	7.2	2.8	-0.8	-2.4			63.8	66.4	63.4	84.5
3	8.7	38.9	-0.6	37.6			77	0	76.5	0
4	21.9	28.1	22.3	26.9			0	0	0	0
5	19.4	10.9	21.3	11			5	18.3	0	16.7
6	30.5	21	32.1	14.8			8	39.1	2.5	35.9
7	19.5	13.3	17.6	15.4			0	19.6	0	15.8
8	9.2	23.2	0.4	14.2			52.6	0	51.5	0
9	22.2	25	23.2	25.6			0	0	0	0
10	3.6	22.2	2.9	19.5			60.4	27.5	47.2	25.7
11	18.6	27.7	20.9	28.1			30.1	6.4	26	4.5
12	17.1	13.1	18	12.7			0	18.9	0	17.2
13	10.8	29.6	8.1	34.3			46.5	8	36.6	4.5
14	7.2	31.2	1.8	31			63.6	0	55.3	0

Table 2.2 Data were collected before and 24 hours after dose of 3Gy radiation. Results are expressed as mean and median values for the respective tracks of probe placement and recording. Percentages of measurements in hypoxic regions which are less than 10, 5, and 2.5 mmHg are also calculated for tracks of measurement before and after radiation for each tumor. Red numbers in mean and median columns represent increased pO₂ values, while red in % columns mean decrease in hypoxic fractions (i.e. increased oxygenation).

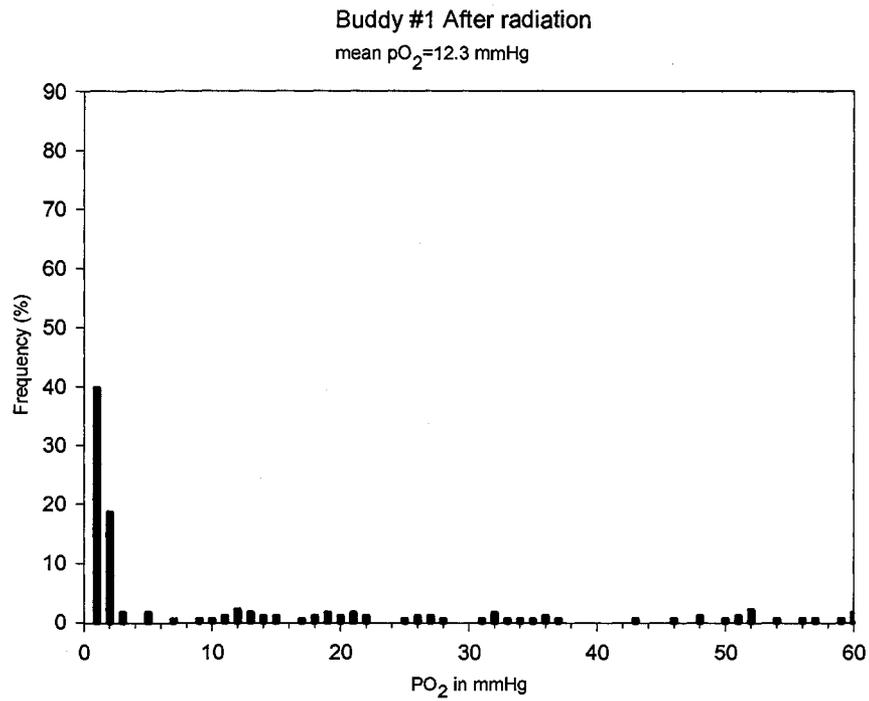
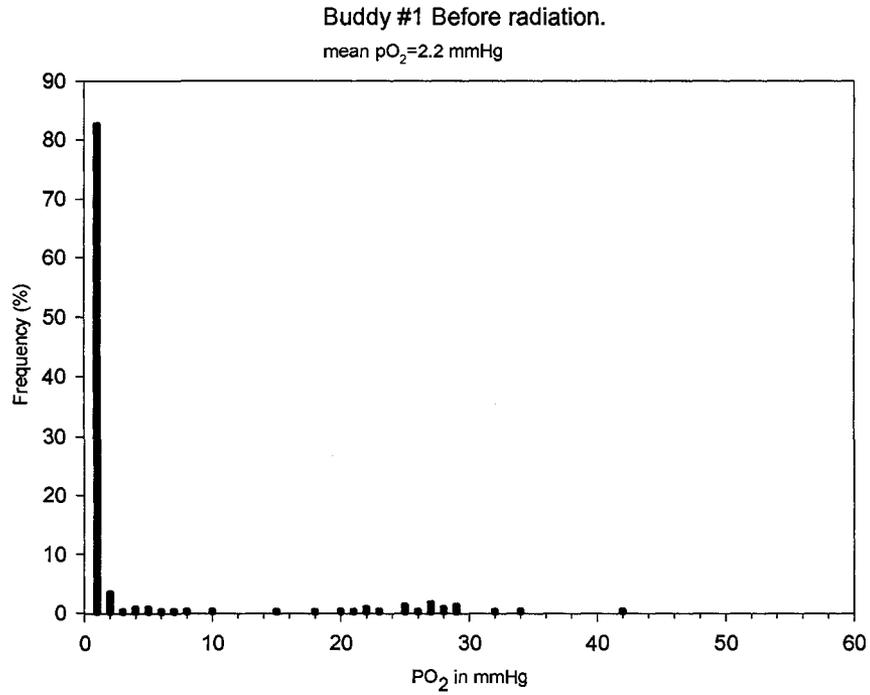


Figure 2.13. Oxygen measurements in tumor #1, soft tissue sarcoma, at the same location before and after radiation

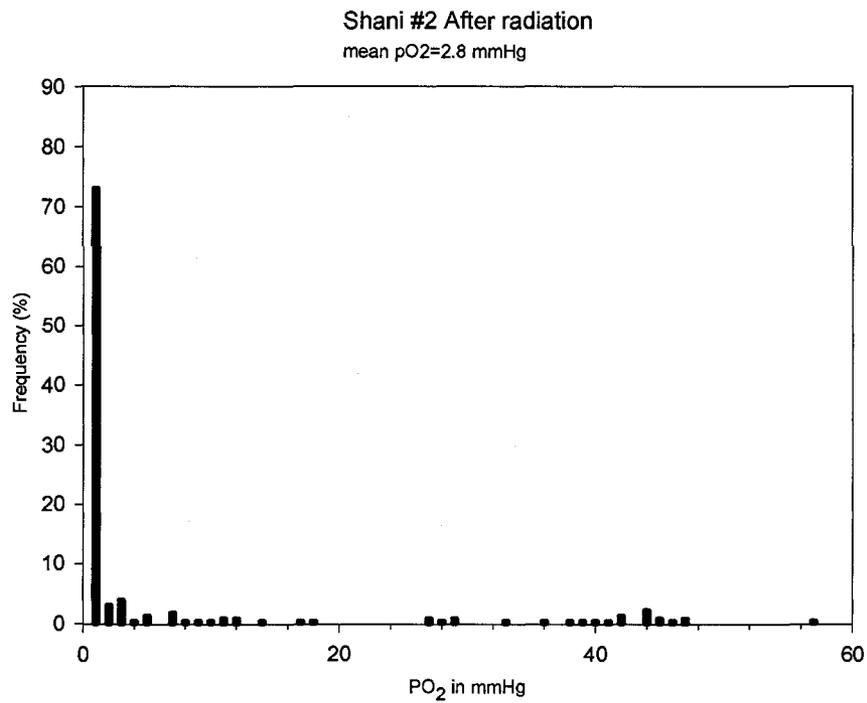
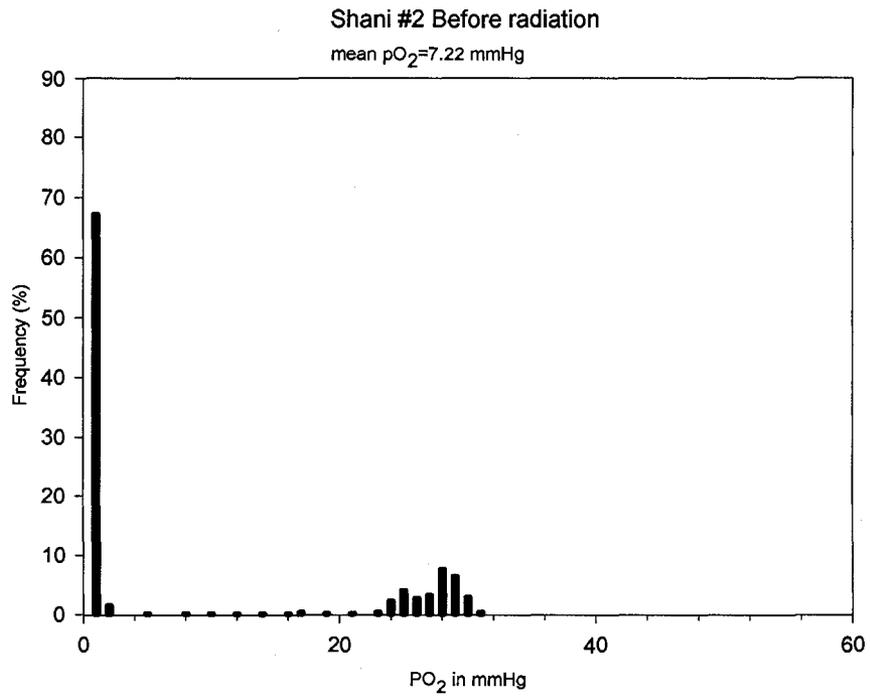


Figure 2.14. Oxygen measurements in tumor #2, soft tissue sarcoma, at the same location before and after radiation

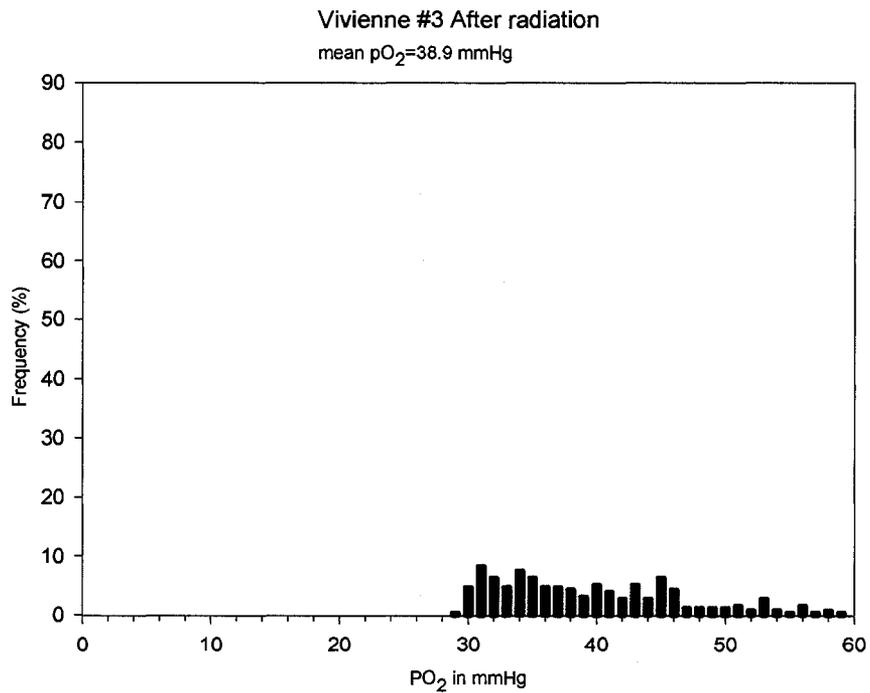
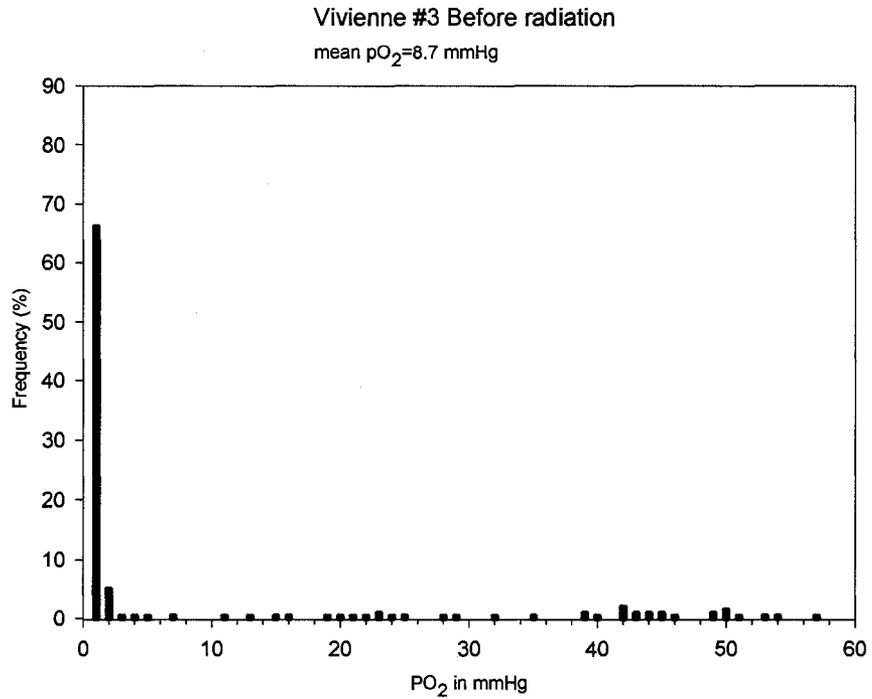


Figure 2.15. Oxygen measurements in tumor #3, osteosarcoma, at the same location before and after radiation

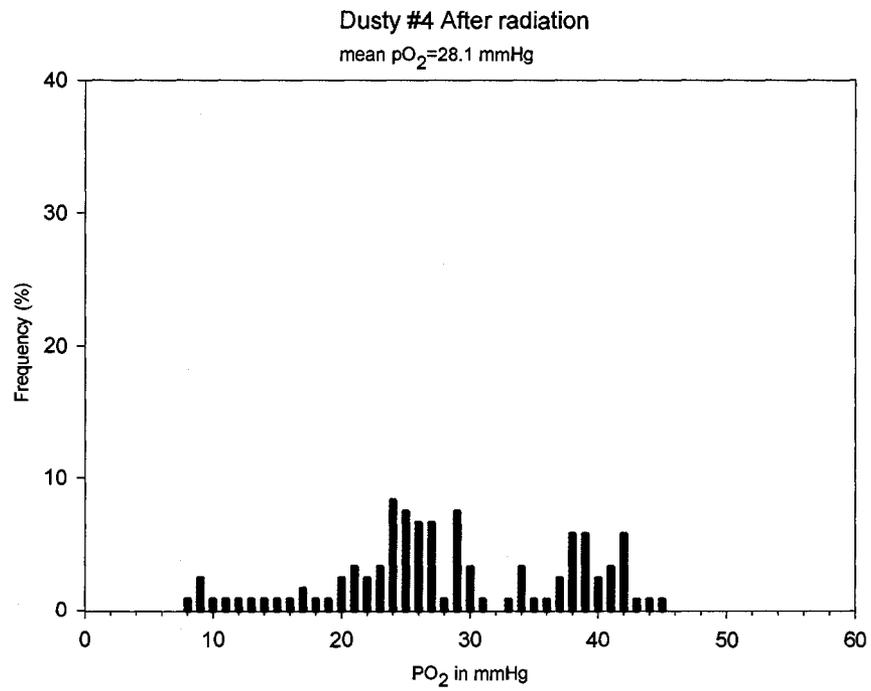
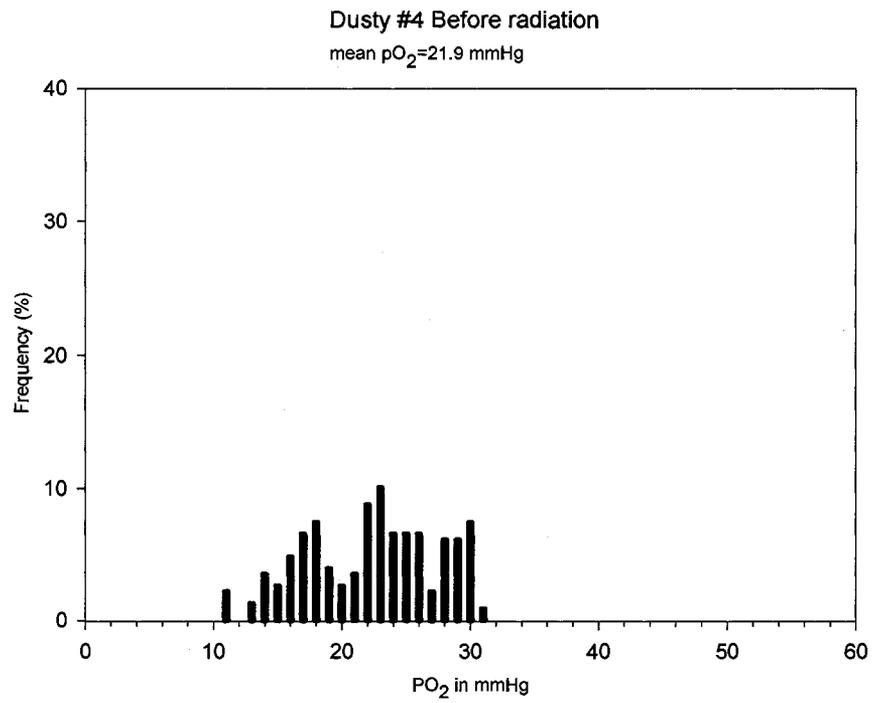


Figure 2.16. Oxygen measurements in tumor #4, osteosarcoma, at the same location before and after radiation

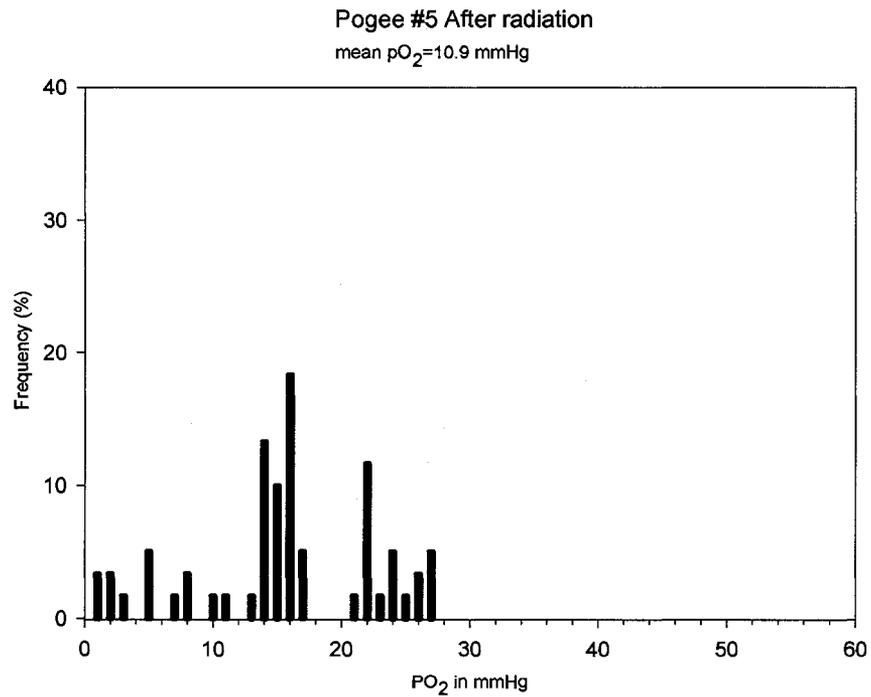
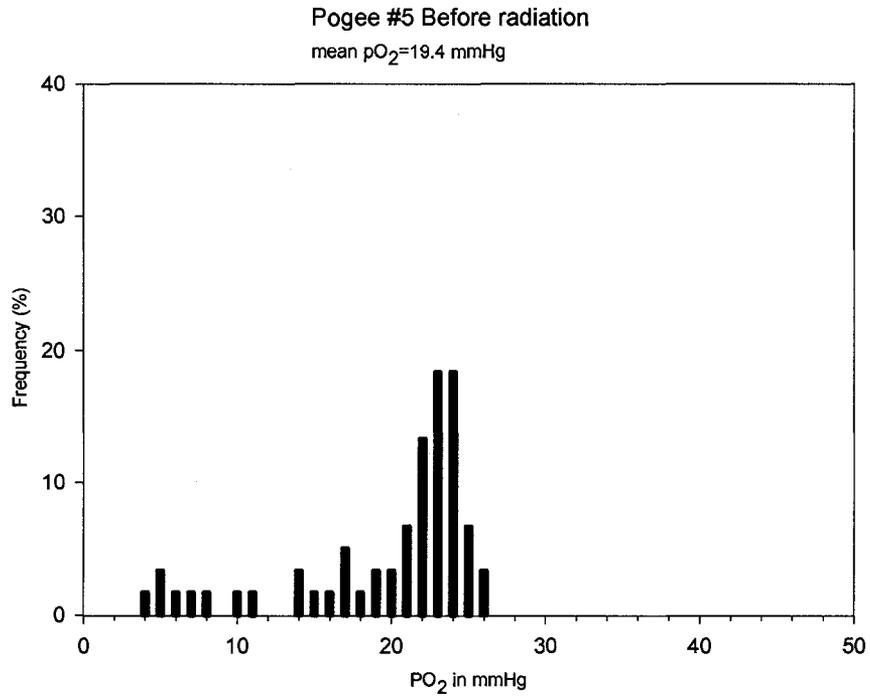


Figure 2.17. Oxygen measurements in tumor #5, soft tissue sarcoma, at the same location before and after radiation

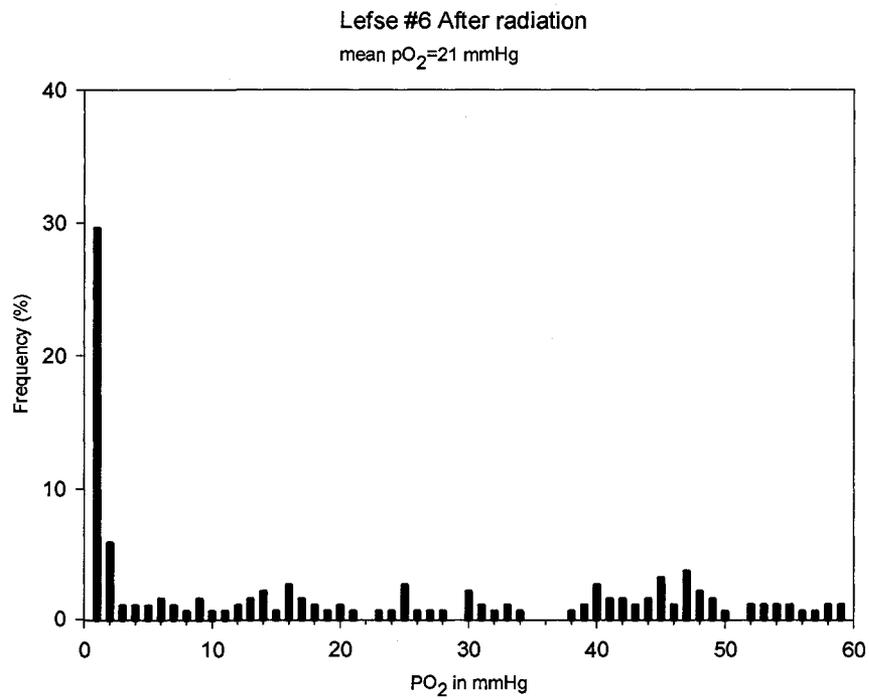
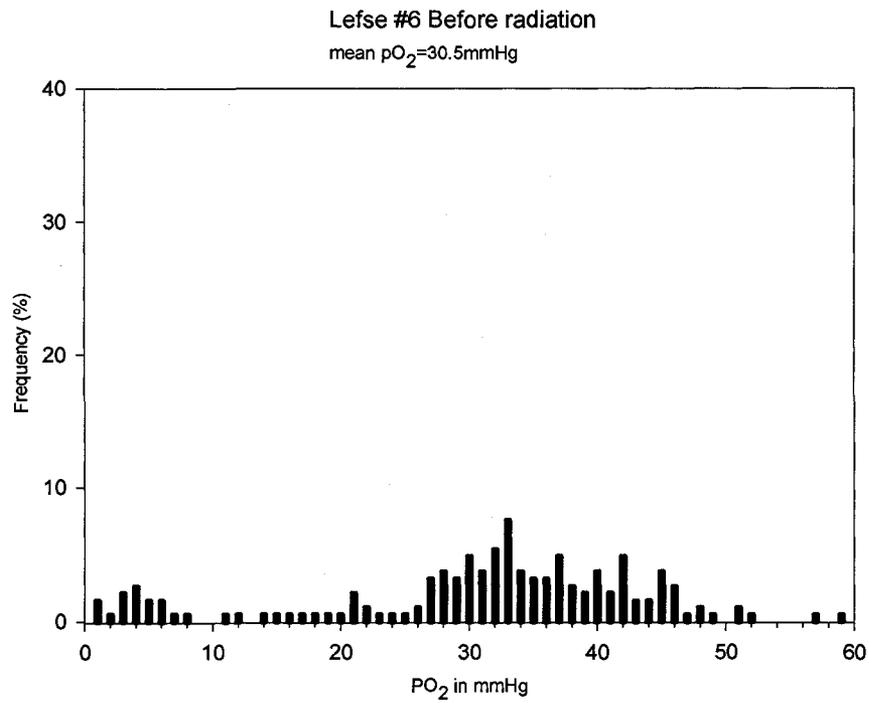


Figure 2.18. Oxygen measurements in tumor #6, mast cell tumor, at the same location before and after radiation.

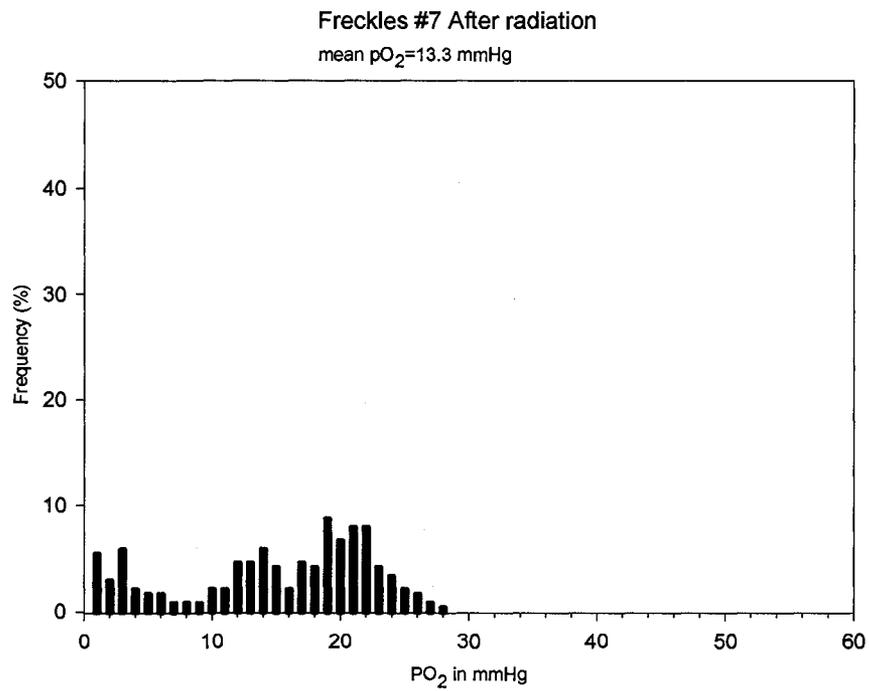
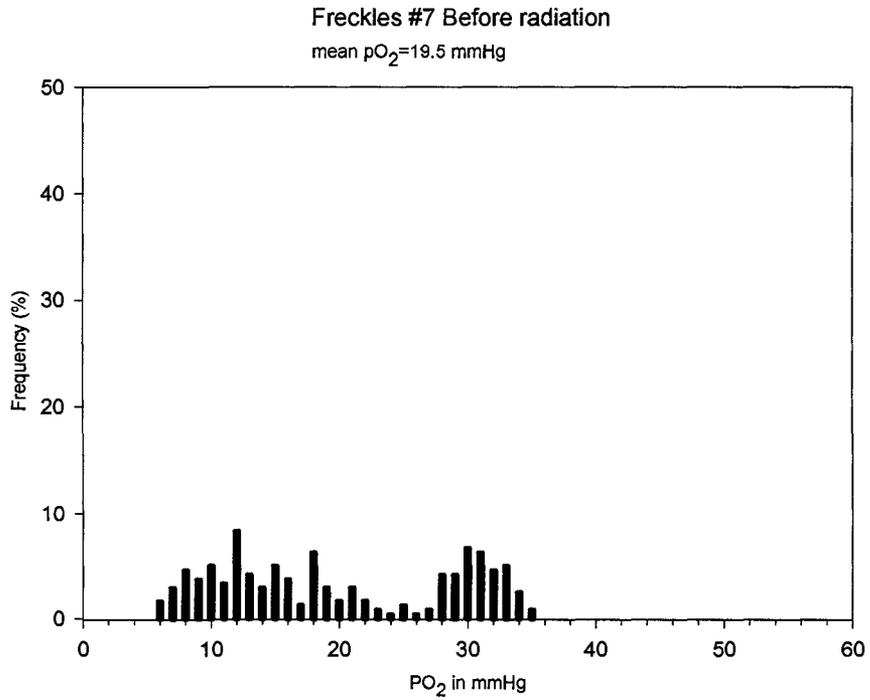


Figure 2.19. Oxygen measurements in tumor #7, adenocarcinoma, at the same location before and after radiation.

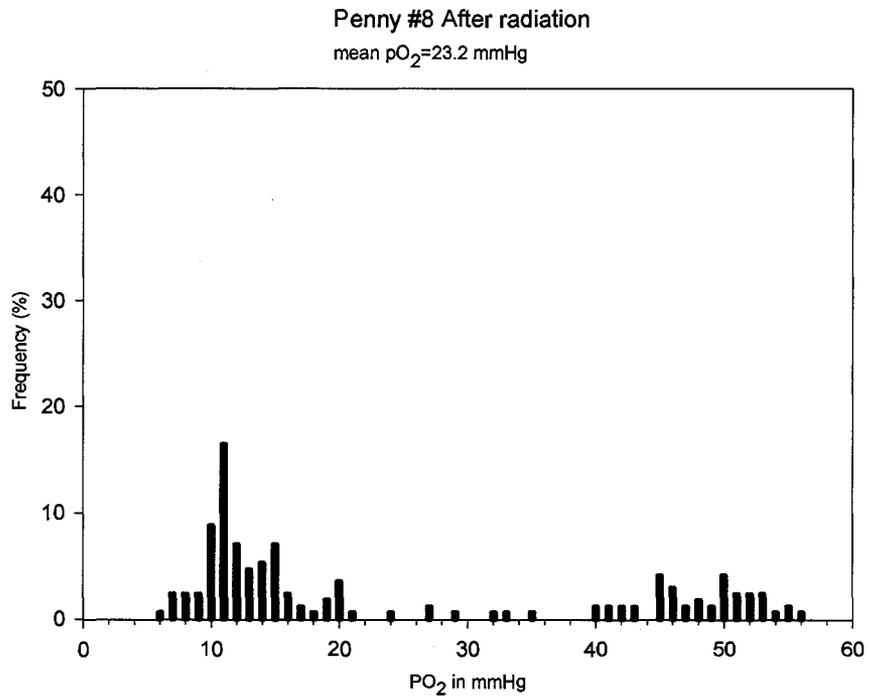
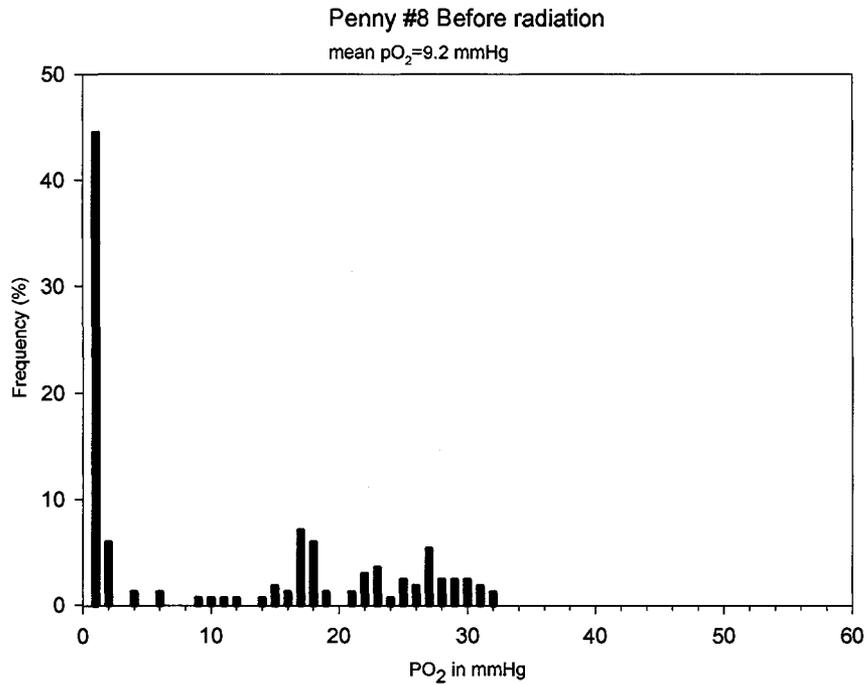


Figure 2.20. Oxygen measurements in tumor #8, mammary carcinoma, at the same location before and after radiation.

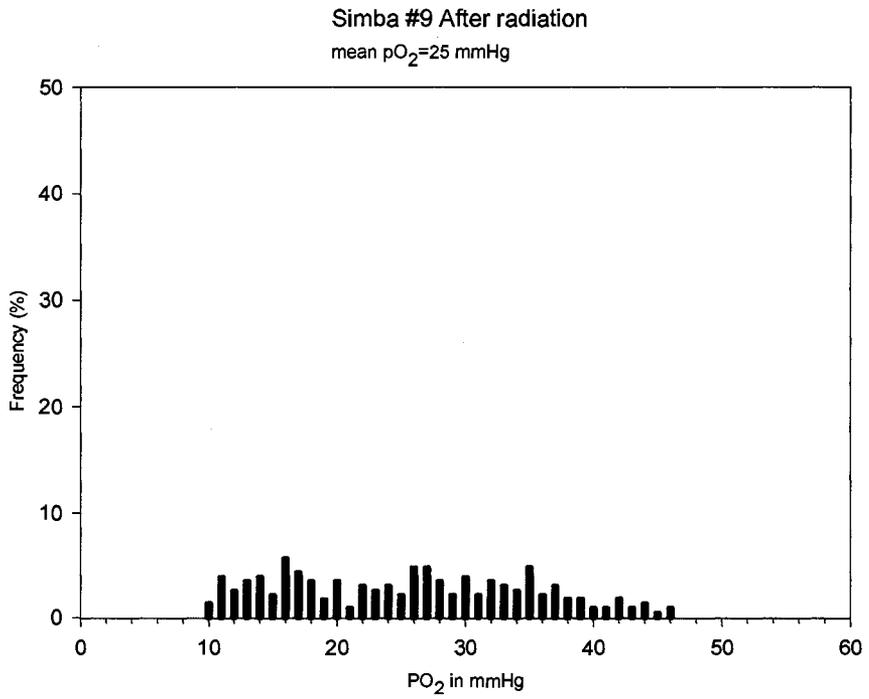
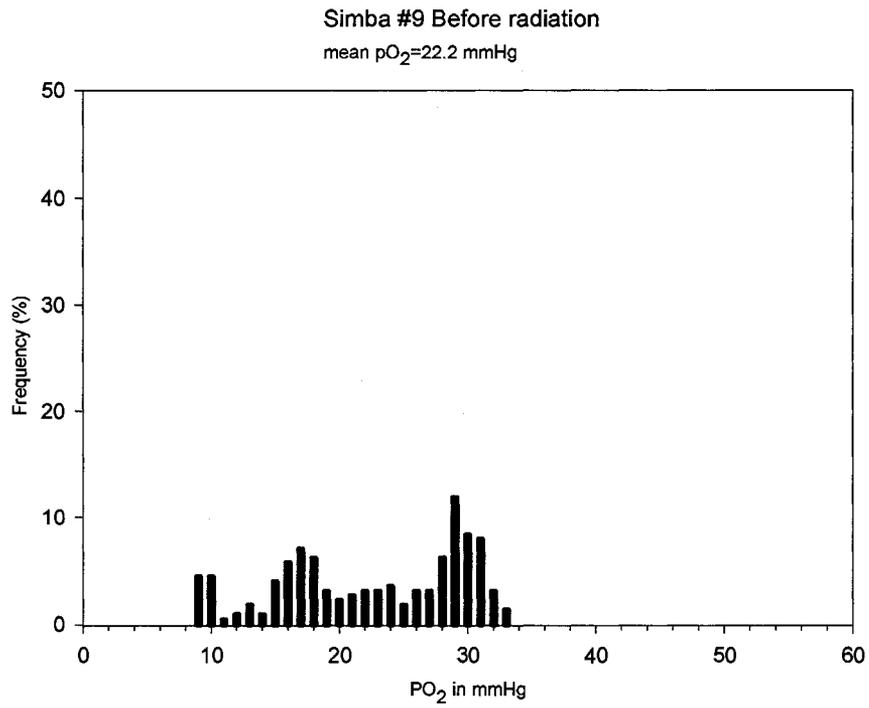


Figure 2.21. Oxygen measurements in tumor #9, multilobular osteochondrosarcoma, at the same location before and after radiation.

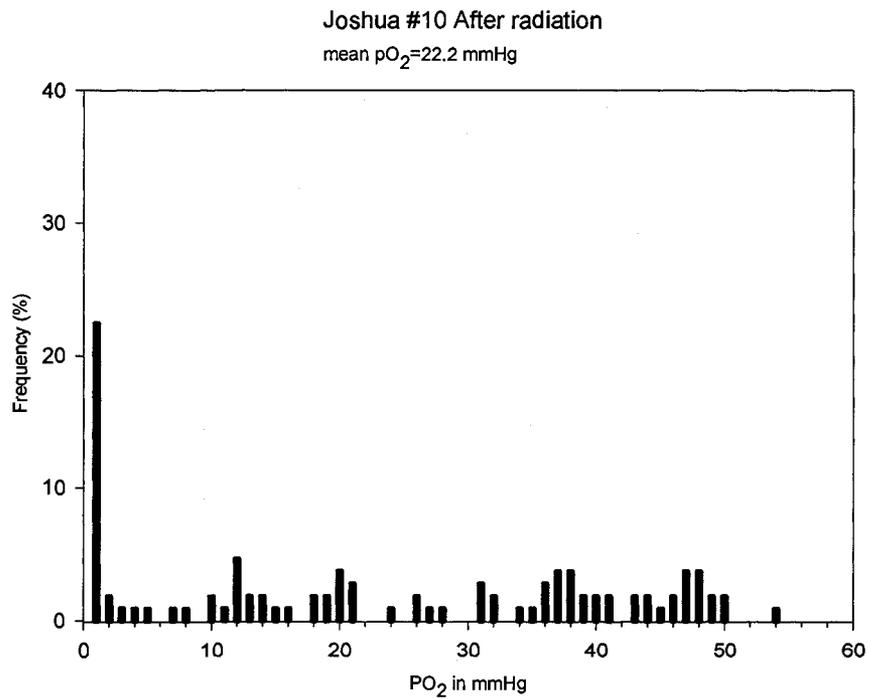
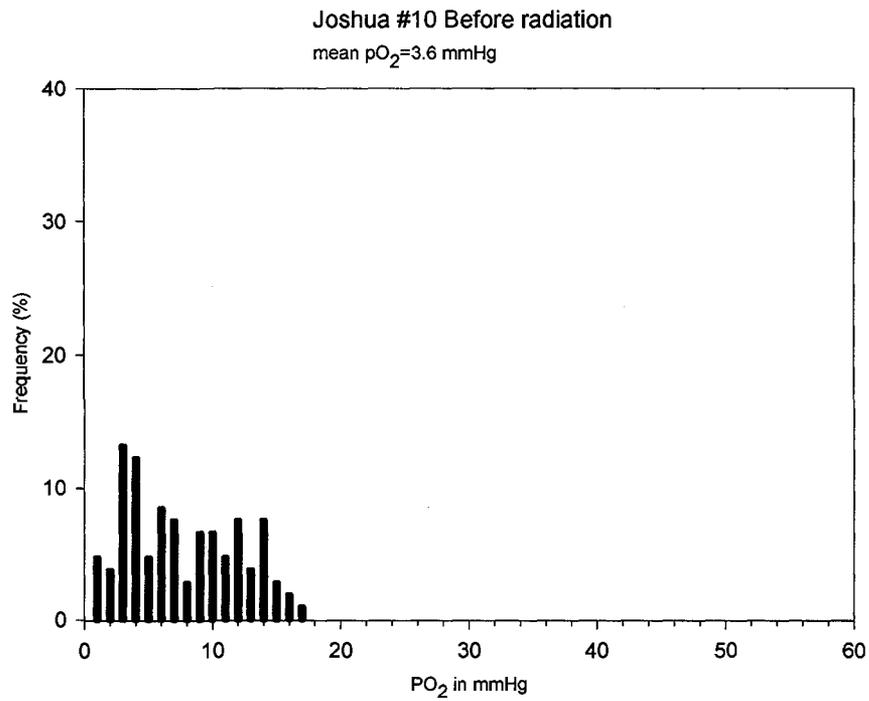


Figure 2.22. Oxygen measurements in tumor #10, soft tissue sarcoma, at the same location before and after radiation.

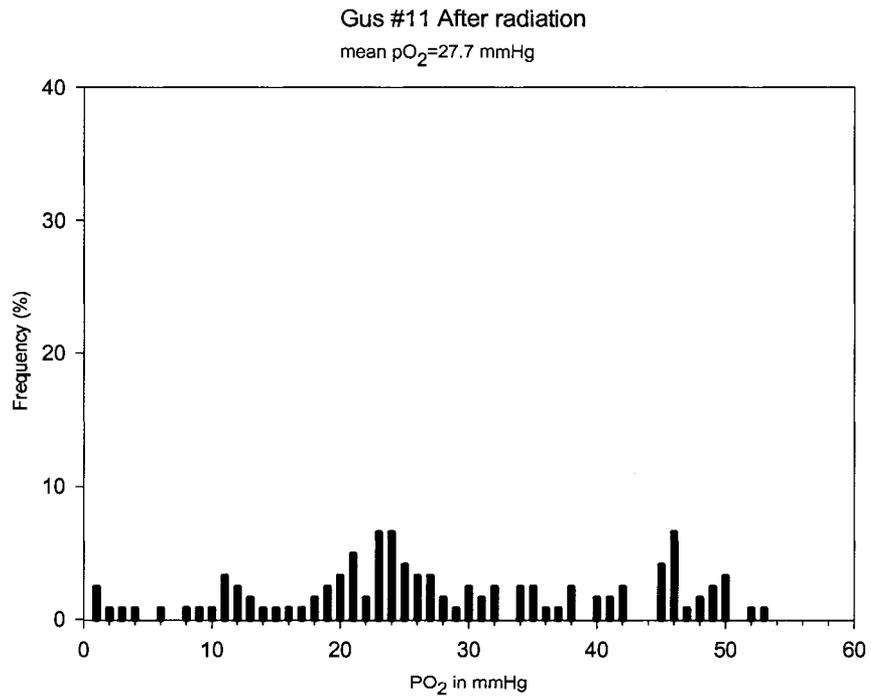
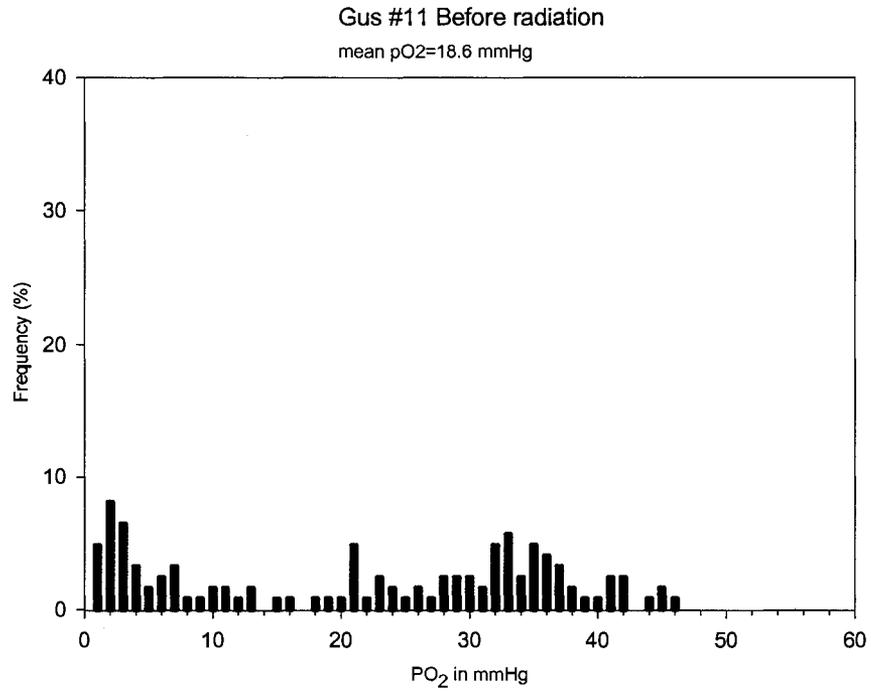


Figure 2.23. Oxygen measurements in tumor #11, fibrosarcoma, at the same location before and after radiation.

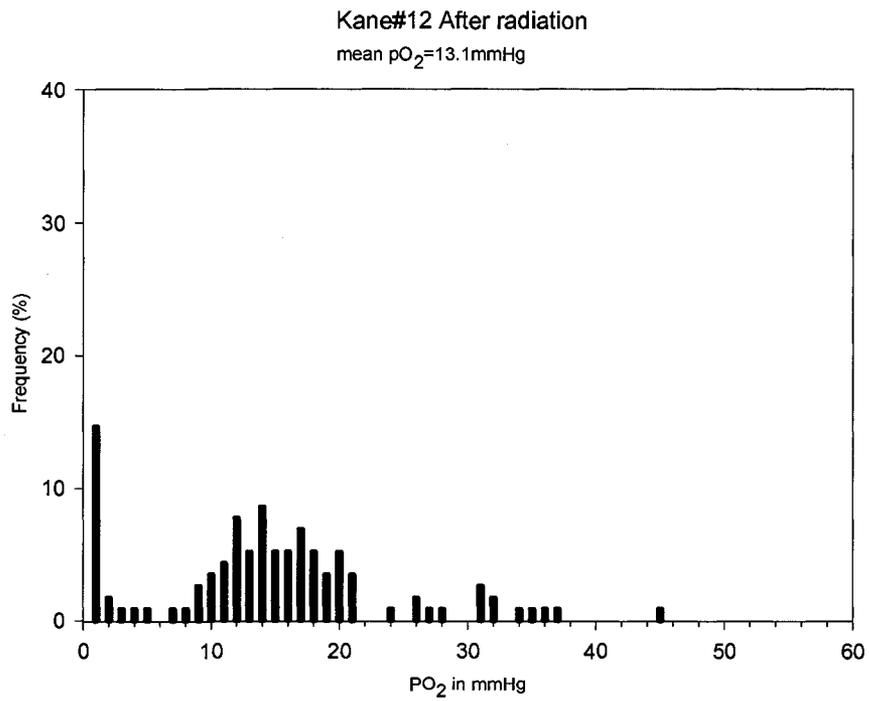
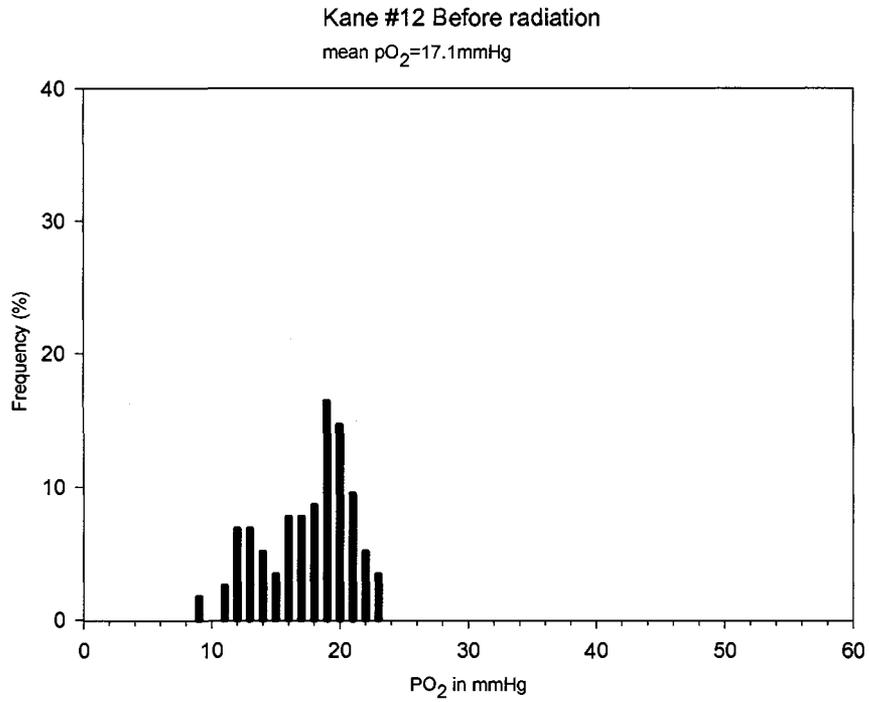


Figure 2.24. Oxygen measurements in tumor #12, liposarcoma, at the same location before and after radiation.

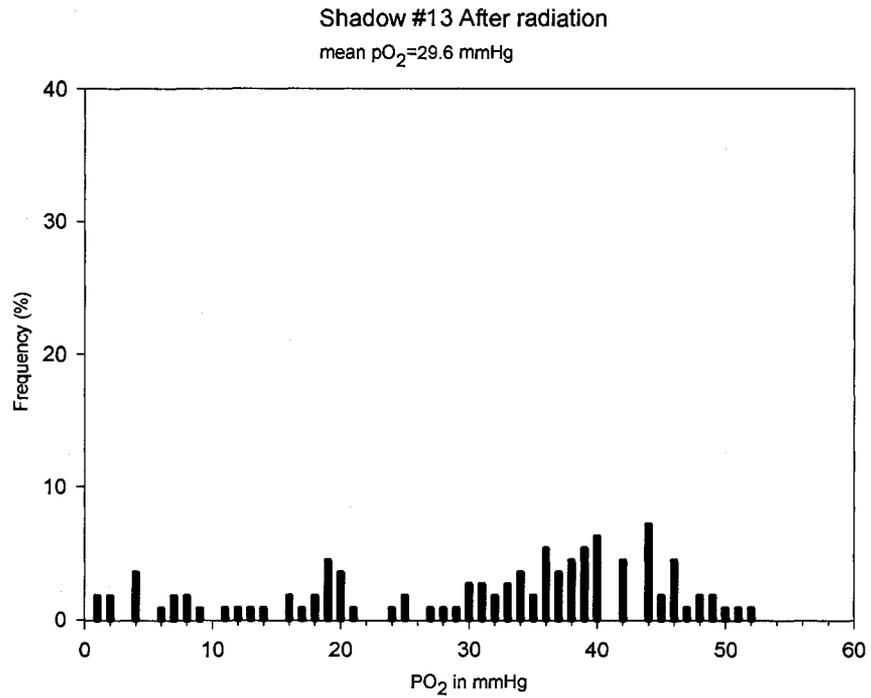
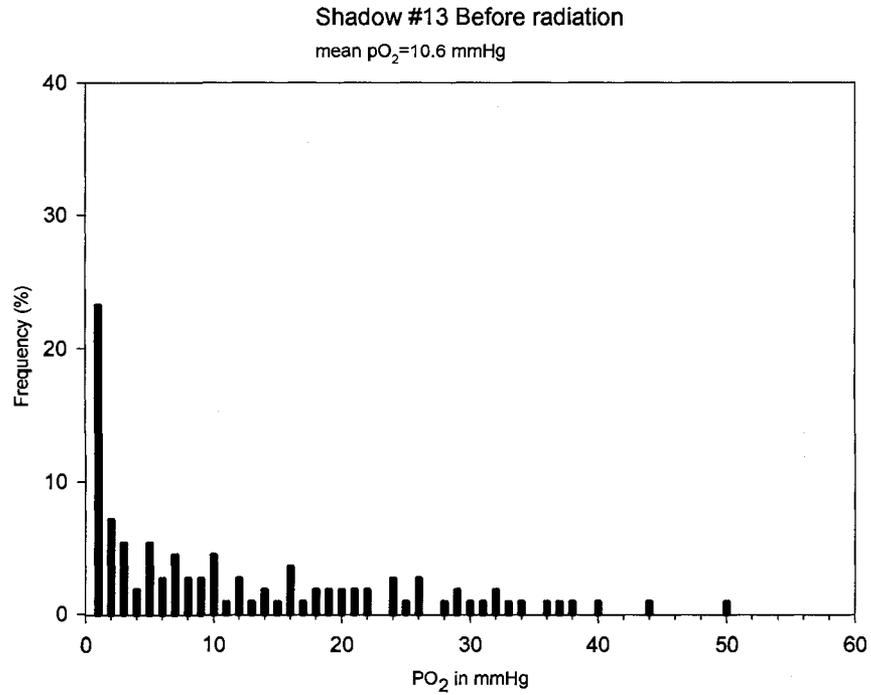


Figure 2.25. Oxygen measurements in tumor #13, soft tissue sarcoma, at the same location before and after radiation.

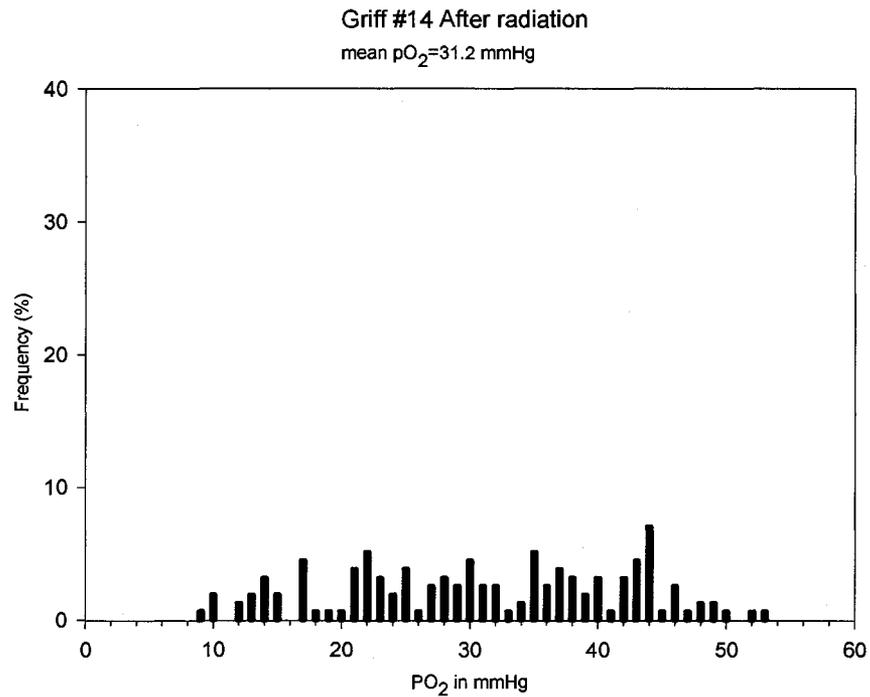
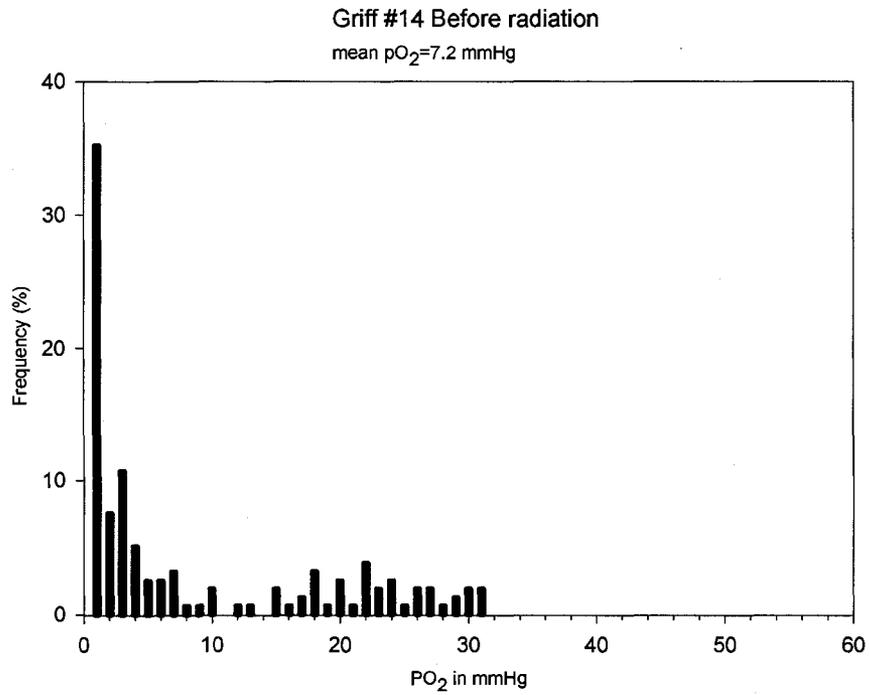


Figure 2.26. Oxygen measurements in tumor #14, fibrosarcoma, at the same location before and after radiation.

Interstitial fluid pressure

Mean IFP decreased after radiation in 9 out of 14 tumors. In 4 of the remaining tumors it did not change more than 0.05-0.12mmHg, and only one tumor had increased IFP post-radiation (Table 2.1).

Table 2.1. IFP measurements presented as means of measurements before and after radiation.

IFP Measurements		
Dog #	Before	After
1	8.8	4.99
2	0.26	0.37
3	3.37	1.56
4	-0.59	-3.41
5	-7.11	-7.21
6	-0.48	-0.53
7	1.02	0.9
8	1.03	0.34
9	1.58	-0.18
10	3.33	-0.68
11	9.83	3.85
12	-0.65	-7.45
13	8.6	0.63
14	1.8	10.45

In Figure 2.11, 2.12, and 2.13 the before and after pressure data from each tumor is graphed.

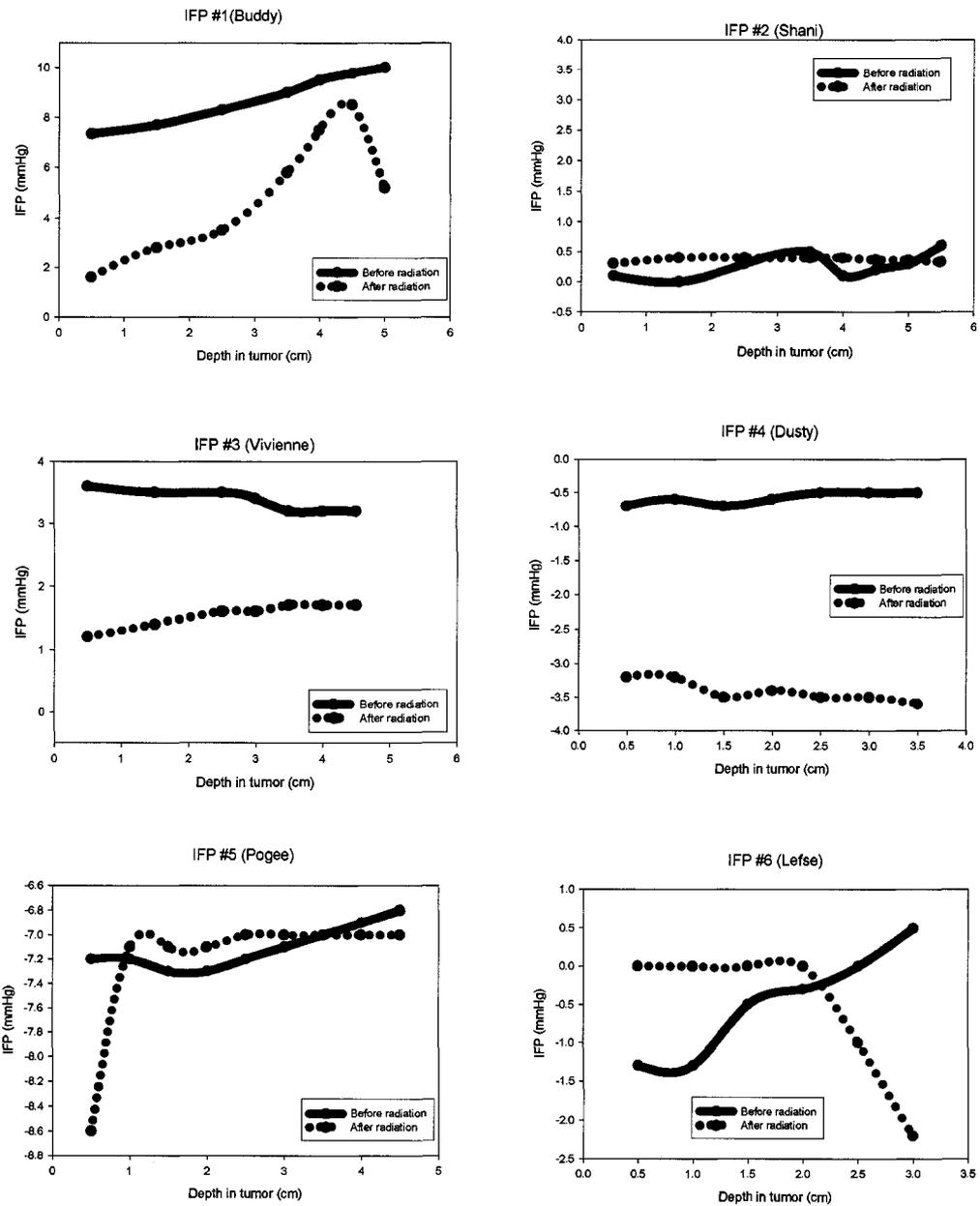


Figure 2.11. IFP before (full line) and after radiation (dotted line) for six tumors.

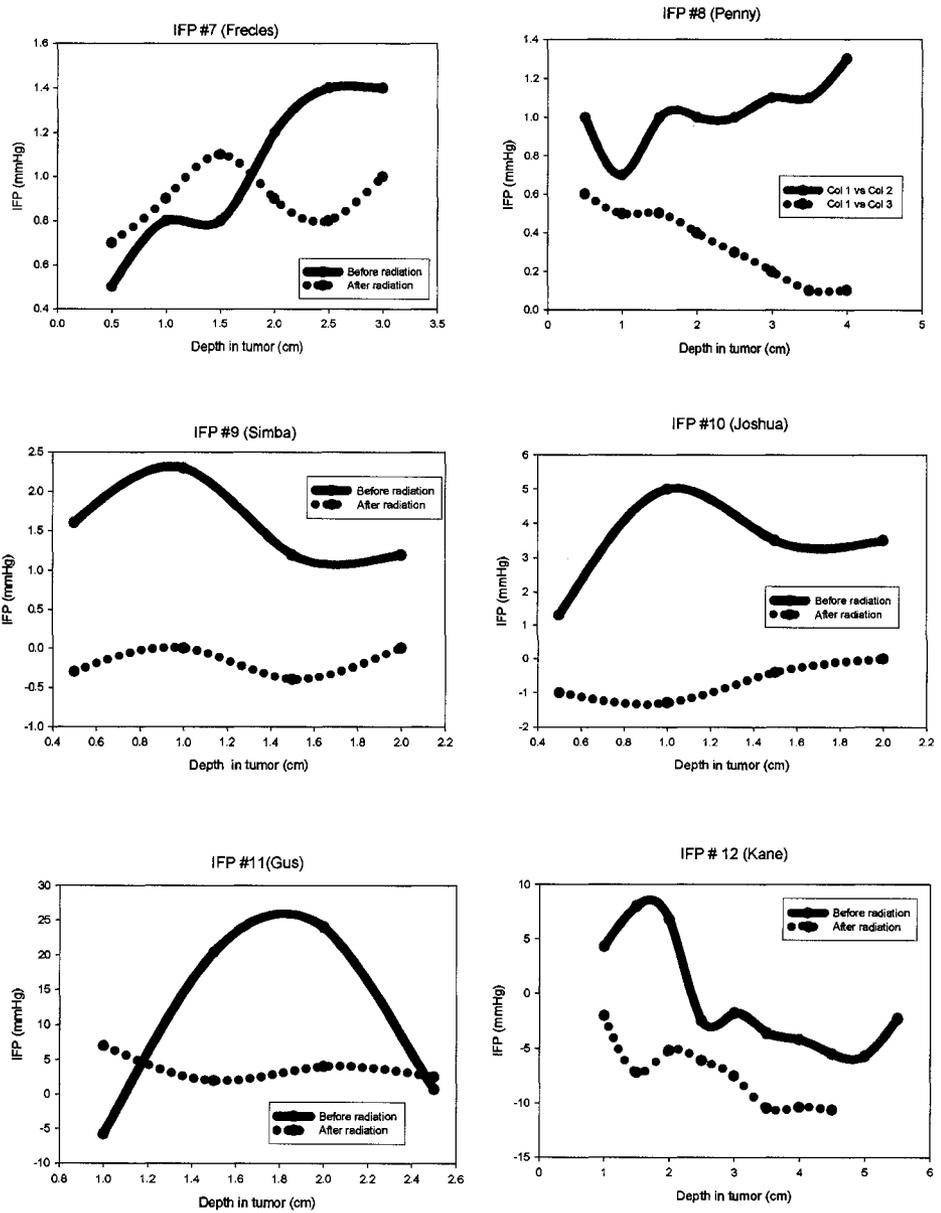


Figure 2.12. IFP before (full line) and after radiation (dotted line) for six tumors.

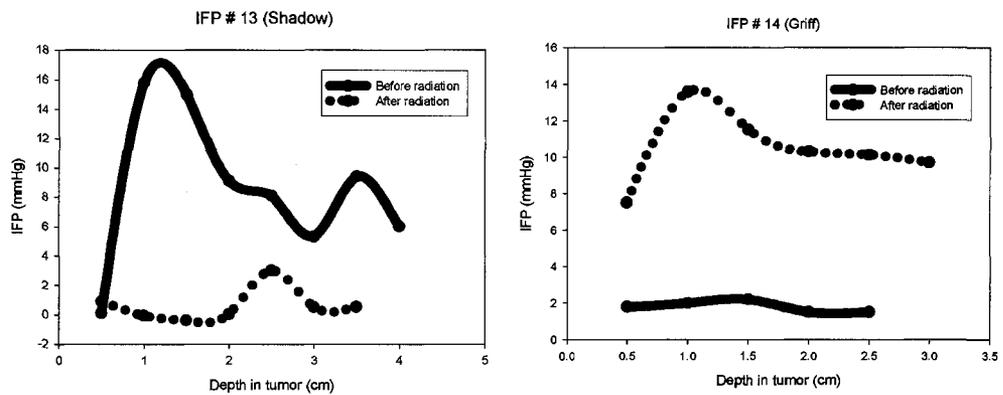


Figure 2.13. IFP before (full line) and after radiation (dotted line) for two tumors.

Microvascular perfusion measurements

Laser Doppler flowmetry data are expressed in relative blood pressure units (BPU) and was obtained in 13 out of 14 dogs. LDF showed an increased mean BPU after radiation in 5 tumors, and decreased mean BPU after radiation in 8 tumors. DCE CT was performed in 5 tumors and indicated an increase in tumor perfusion after radiation in 1 tumor (results that do not correlate to LDF data in this one case). DCE MRI for microvascular perfusion was obtained in 9 tumors and indicated that it was decreased in all 9 tumors after radiation (in four cases these data did not correlate to LDF results). Microvascular perfusion data obtained for each tumor are summarized in Table 2.3.

Table 2.3. Microvascular perfusion estimates in 14 tumors using two techniques for each tumor. Laser Doppler means of measurements are in BPU, and DCE CT/MRI measurements are presented as relative perfusion indexes (RPIs).

DOG#	LDF PERFUSION		CT/MRI PERFUSION	
	BPU before	BPU after	RPI before	RPI after
1	101.88	73.63	0.050335	0.047402
2	50.37	42.22	0.037031	0.004243
3	27.12	8.11	0.370206	0.173572
4	495.41	288.71	0.181723	0.253197
5	191.74	227.5	0.032	-0.0336
6	214.18	128.93	14.26	8.21
7	92.47	193.85	11	-3.3477
8	97.12	136.9	23.72	-0.5478
9	132.8	94.7	21.04	16.813
10	244.4	159.7	34.73	16.25
11	204.81	N/A	9.52	7.68
12	123.63	422.46	9.33	4.18
13	340.03	235.99	16.34	9.38
14	119.44	132.08	24.31	20.42

Microvascular perfusion data obtained for each tumor by LDF are also presented in graphs in Figures 2.27, 2.28, 2.29, 2.30, and 2.31.

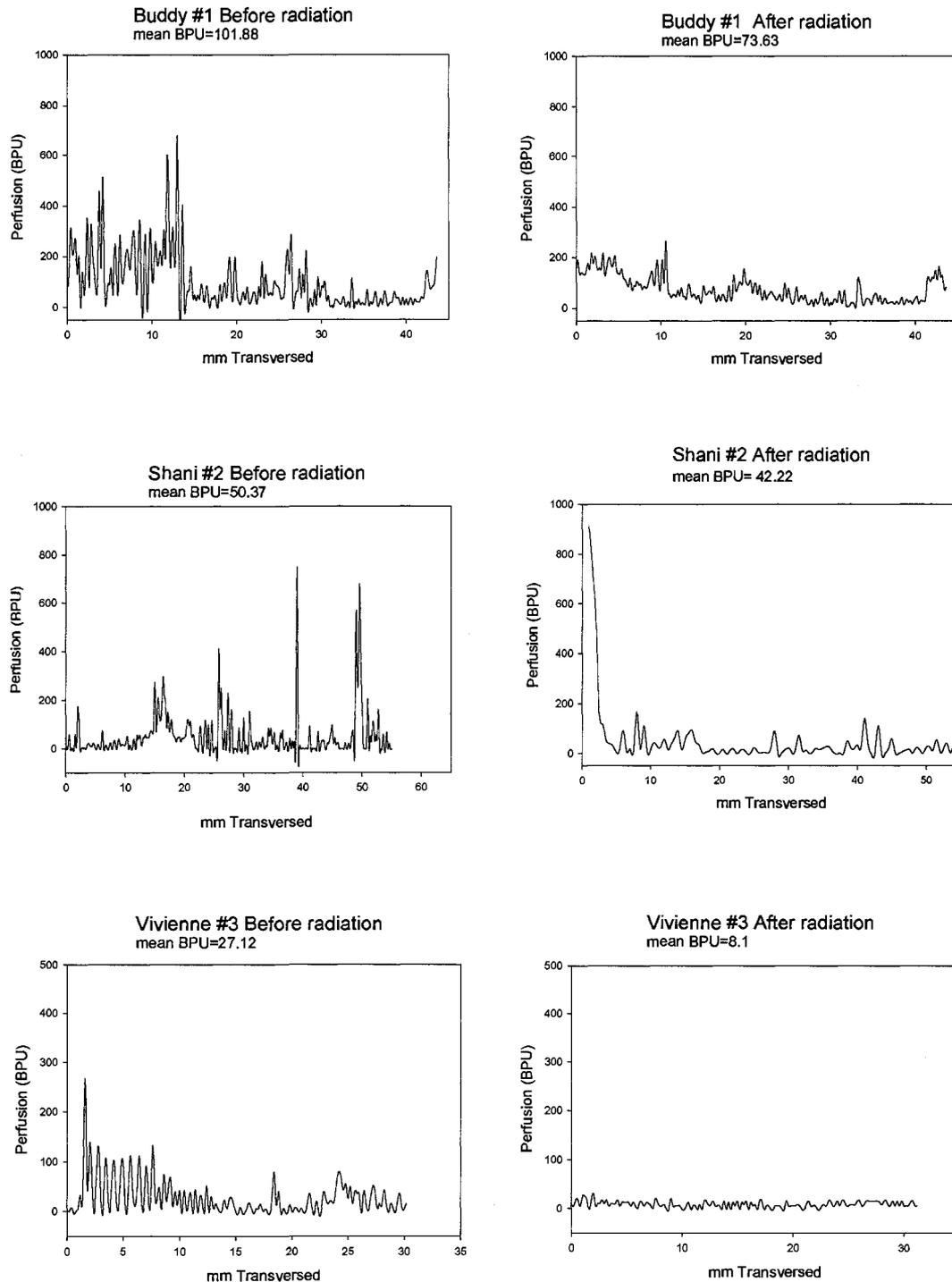


Figure 2.27. LDF perfusion measured with OxyFlow at the time of the pO₂ measurement with OxyLite, using combined perfusion/oxygen/temperature probes, before and after radiation dose of 3Gy in three different tumors.

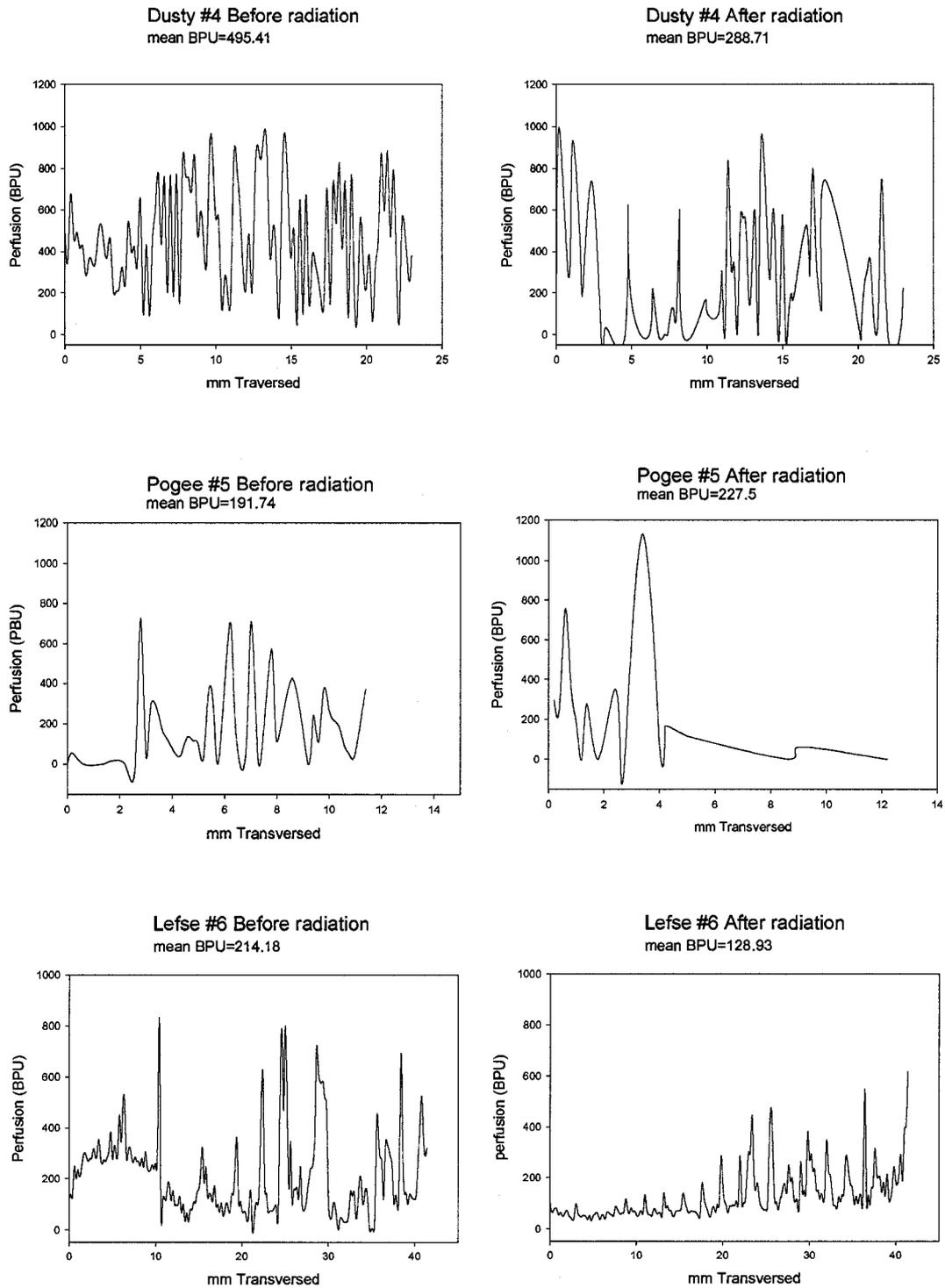


Figure 2.28. LDF perfusion measured with OxyFlow at the time of the pO_2 measurement with OxyLite, using combined perfusion/oxygen/temperature probes, before and after radiation dose of 3Gy in three different tumors.

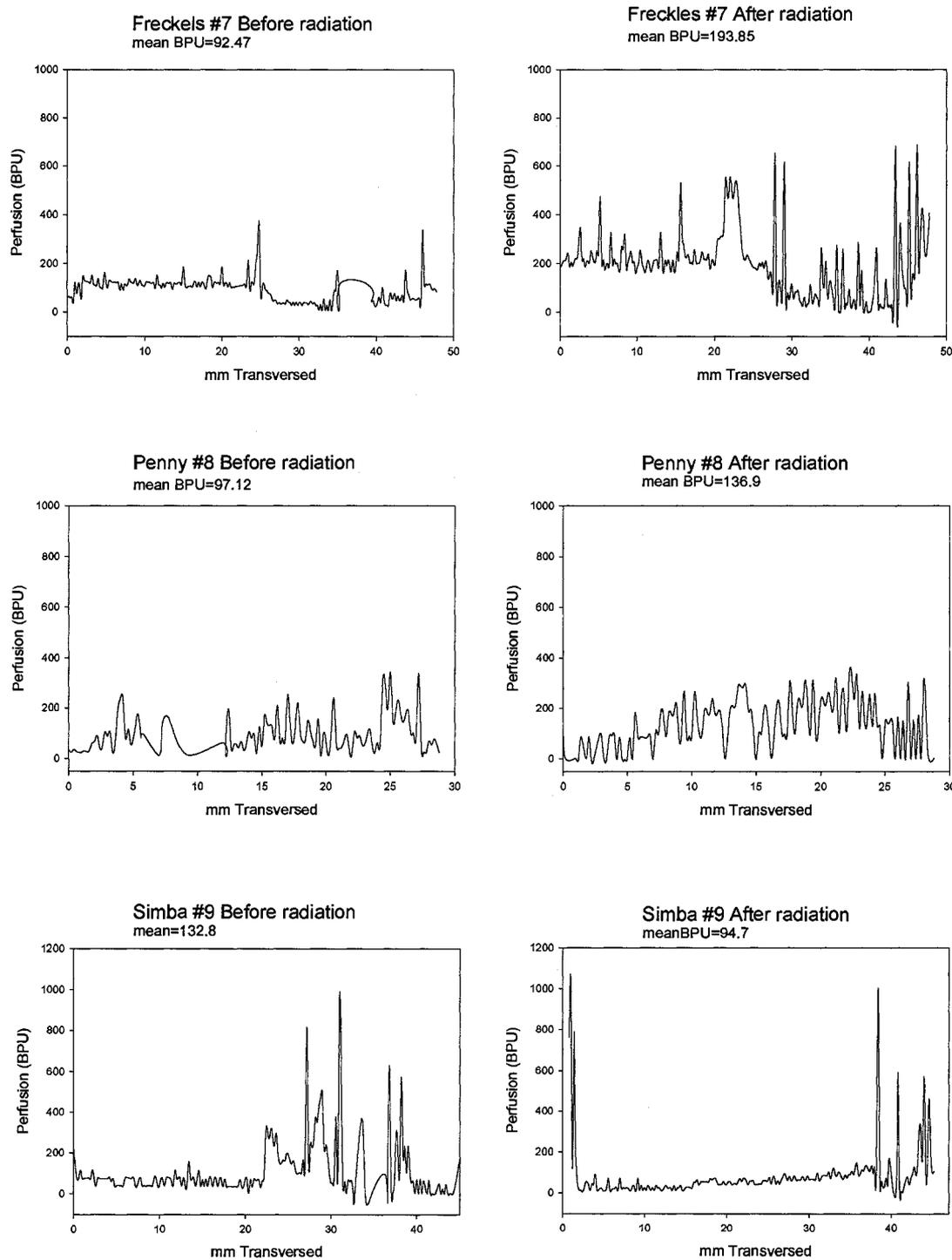


Figure 2.29. LDF perfusion measured with OxyFlow at the time of the pO₂ measurement with OxyLite, using combined perfusion/oxygen/temperature probes, before and after radiation dose of 3Gy in three different tumors.

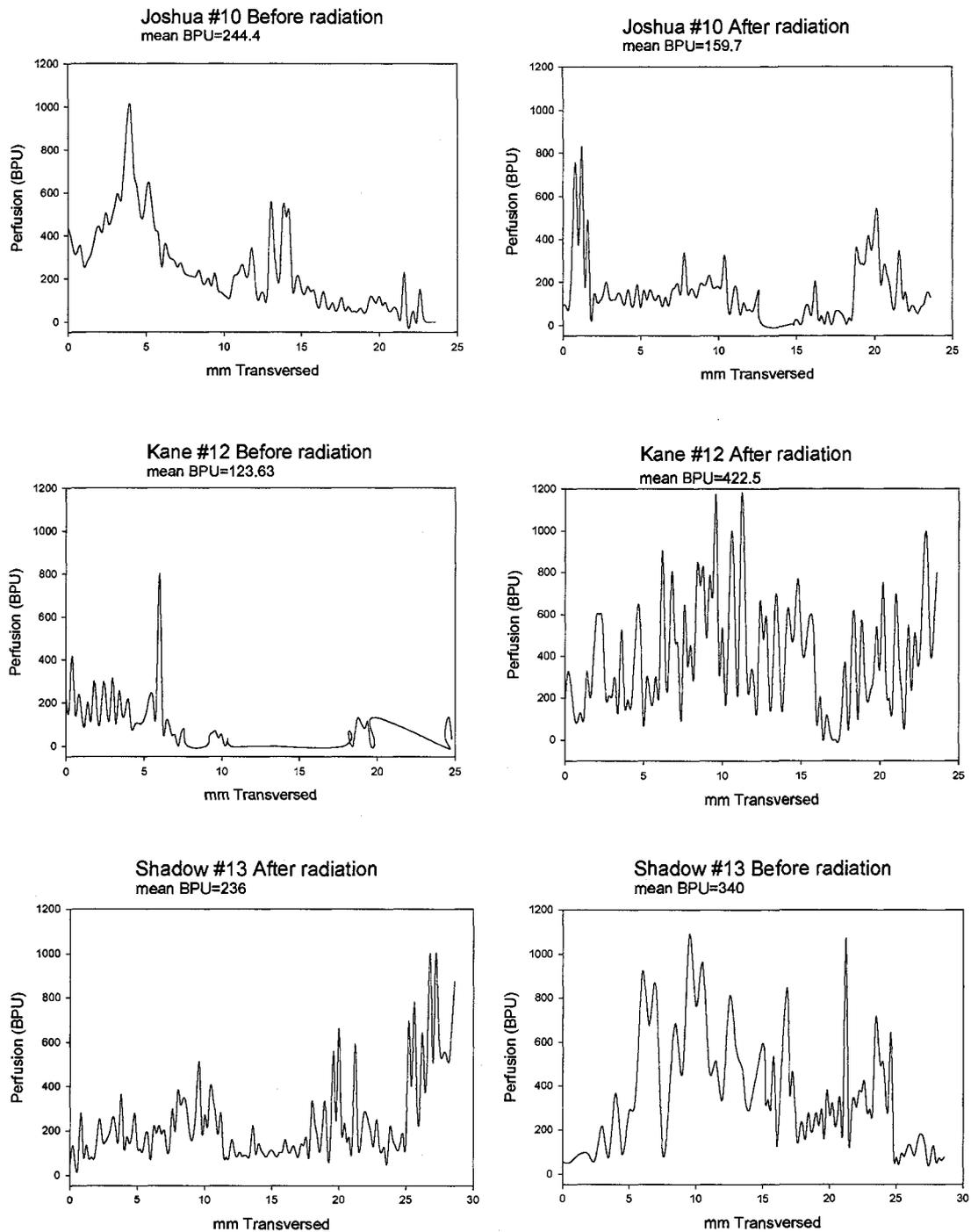


Figure 2.30. LDF perfusion measured with OxyFlow at the time of the pO_2 measurement with OxyLite, using combined perfusion/oxygen/temperature probes, before and after radiation dose of 3Gy in three different tumors.

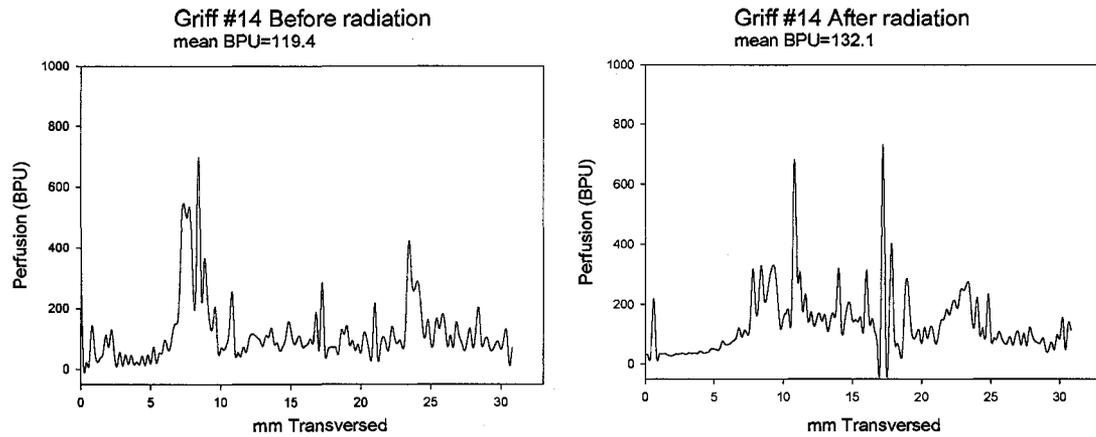


Figure 2.31. LDF perfusion measured with OxyFlow at the time of the pO₂ measurement with OxyLite, using combined perfusion/oxygen/temperature probes, before and after radiation dose of 3Gy.

Dynamic contrast enhanced CT and MRI were done along with LDF measurements in all tumors. RPIs were calculated and presented in Table 2.3. Graphs for average RPI for the entire tumor (for all tumors) and each tumor RPIs for regions of interest are presented in figures 2.32, 2.33, 2.34, 2.35, 2.36, and 2.37 provided by Dr. Susan Kraft.

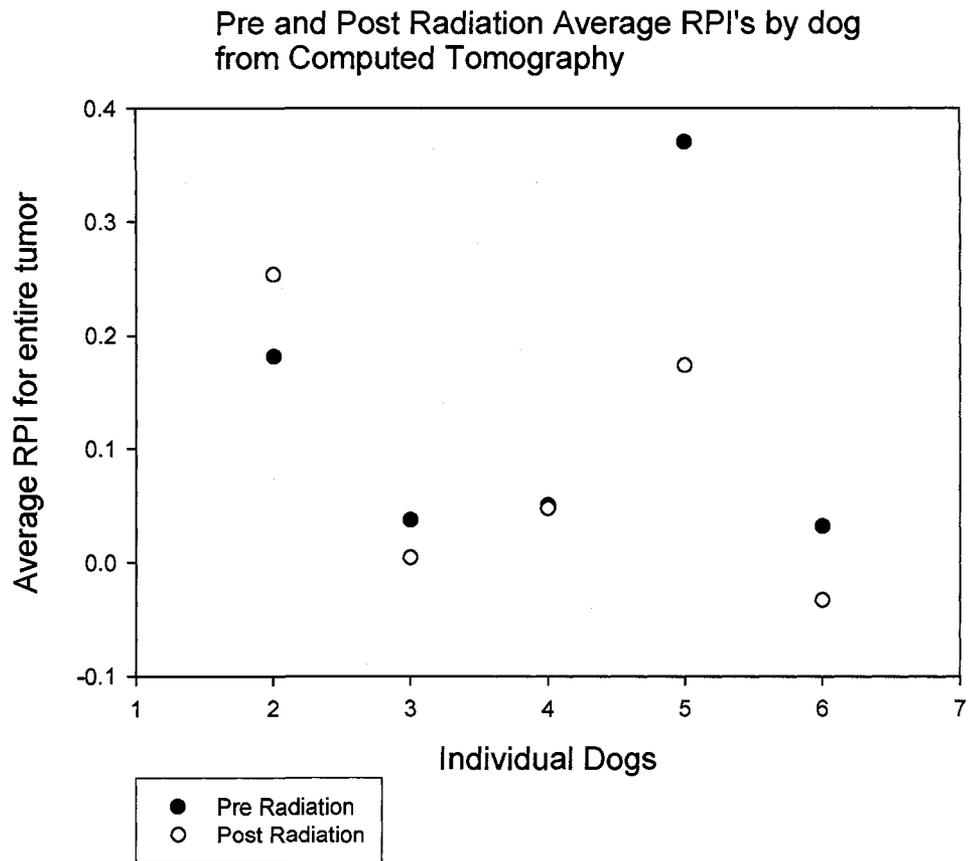


Figure 2.32. Average RPIs for whole tumor in 5 dogs, calculated from DCE CT pre- and post-radiation.

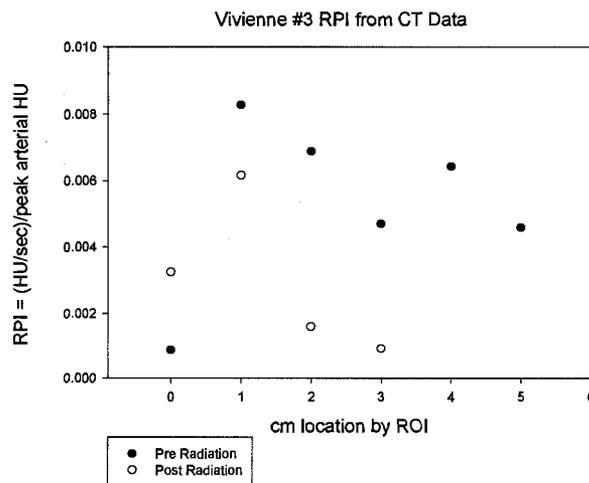
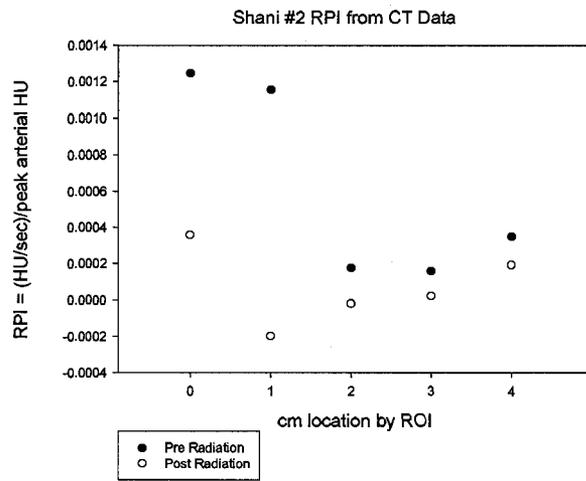
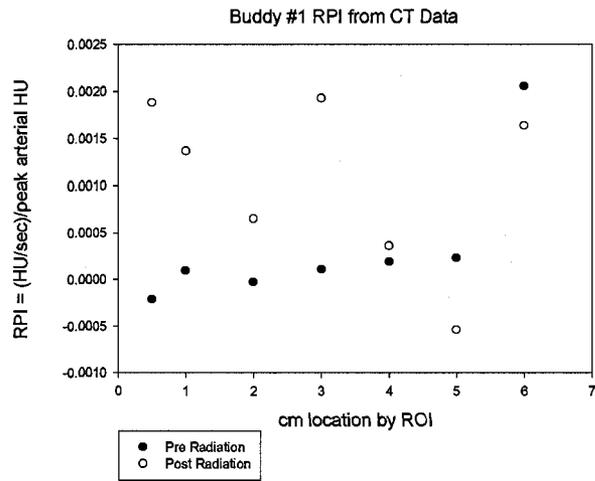


Figure 2.33. Individual tumors RPI calculated for ROIs at different depths in tumors, pre- and post-radiation.

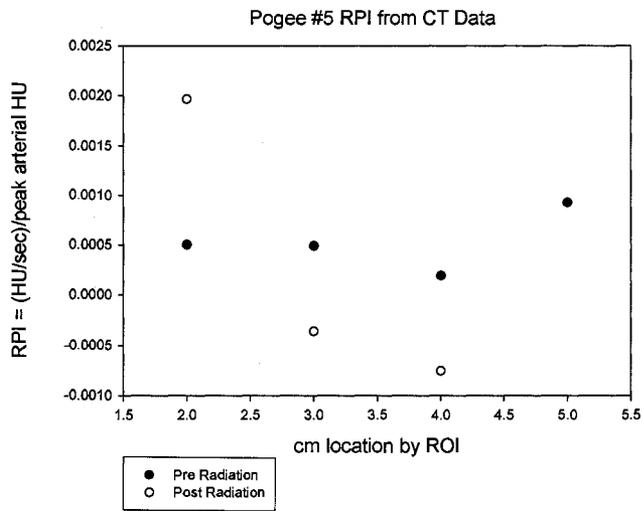
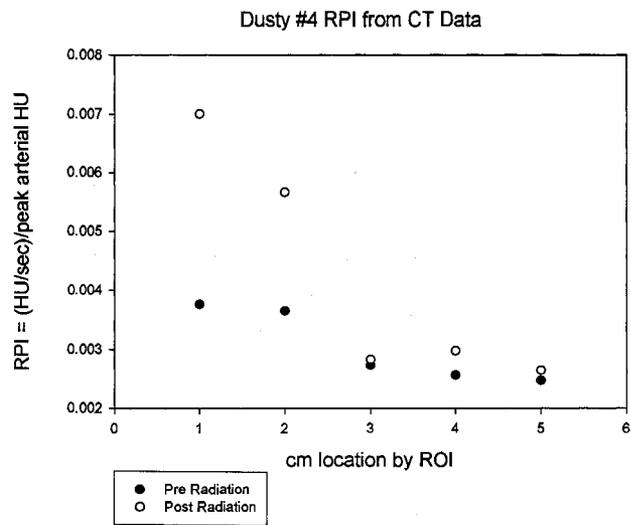


Figure 2.34. Individual tumors RPI calculated for ROIs at different depths in tumors, pre- and post-radiation.

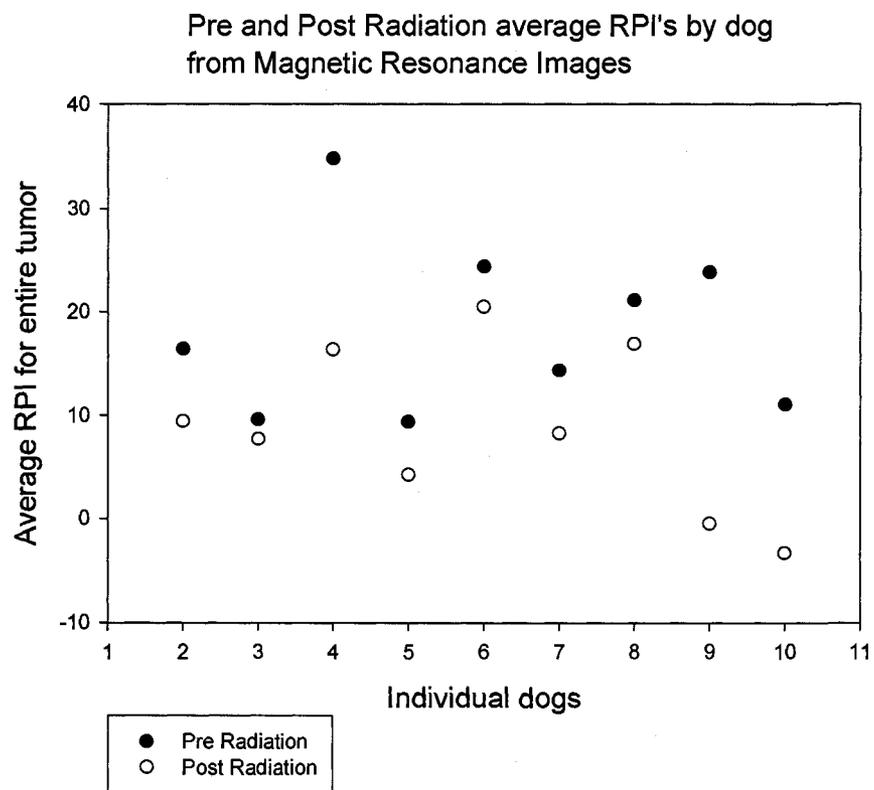
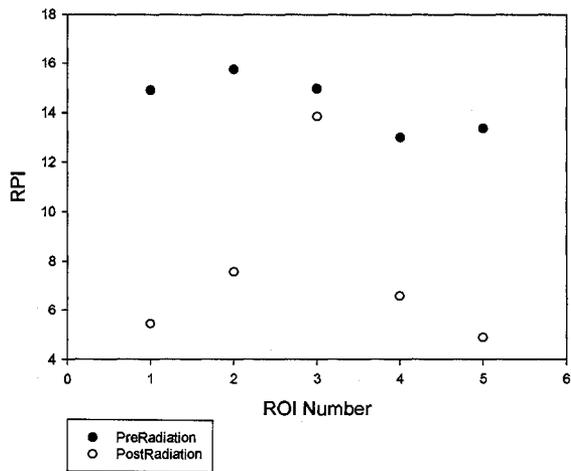
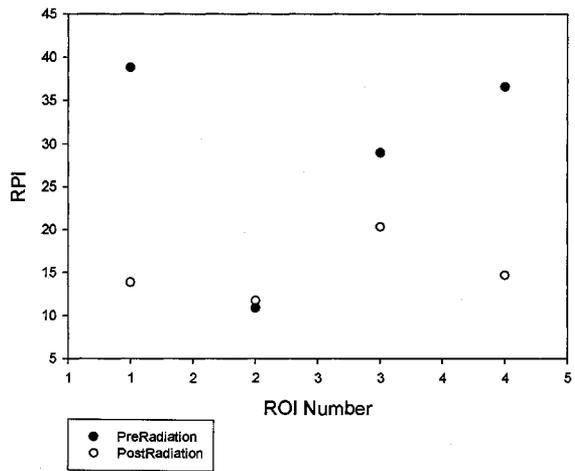


Figure 2.35. Average RPIs for whole tumor in 9 dogs, calculated from DCE MRI pre- and post-radiation.

Lefse #6 RPI from MRI Data



Joshua #10 RPI from MRI Data



Gus #11 RPI from MRI Data

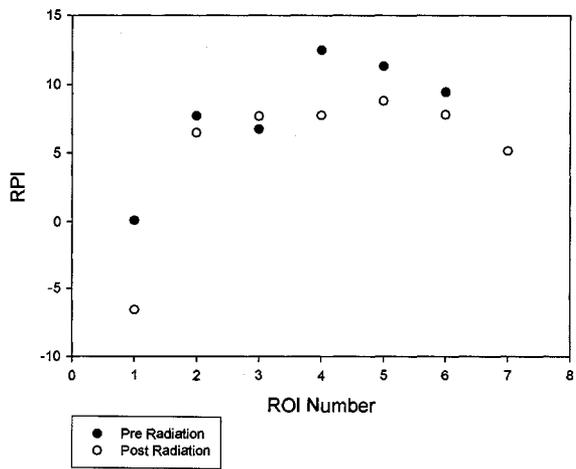


Figure 2.36. Individual tumors RPI calculated for ROIs at different depths in tumors, pre- and post-radiation.

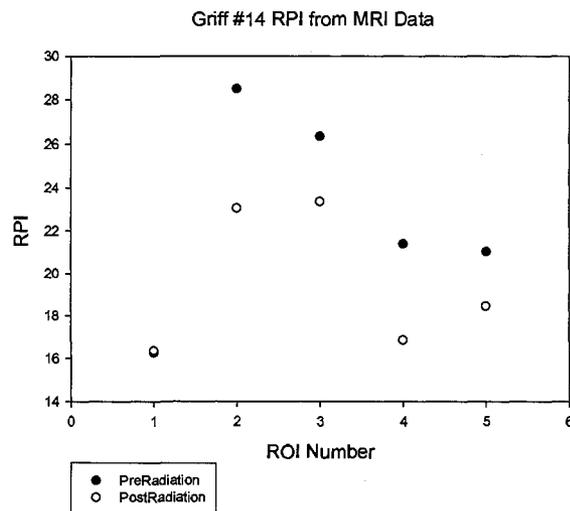
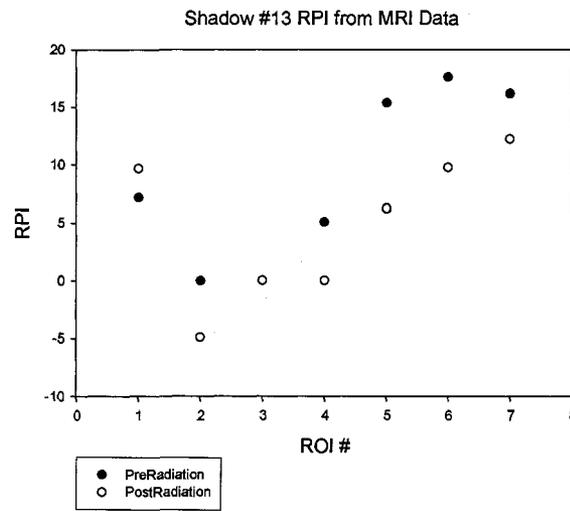
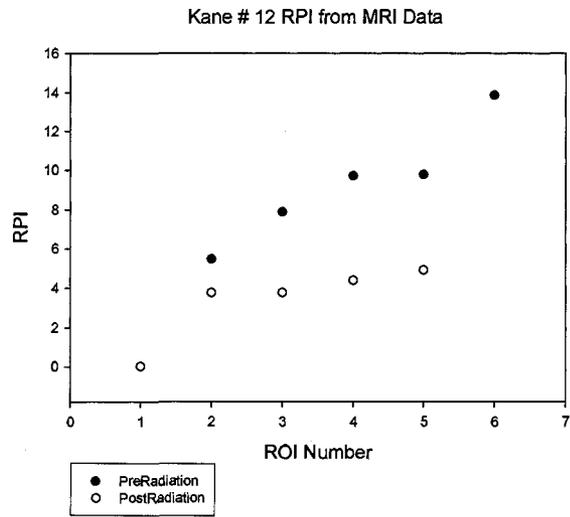


Figure 2.37. Individual tumors RPI calculated for ROIs at different depths in tumors, pre- and post-radiation.

Quantification of tumor cell apoptosis

Pretreatment frequency of apoptosis differed among the tumors (Table 2.4). After radiation, the apoptotic index was significantly increased in all tumors at both 6 and 24 hours (at 24 hours P=0.0015). The apoptotic index (AI) was greatest at 6 hours after radiation (P= 0.00093, two-tailed *t* test) (Figure 2.38).

Table 2.4. Apoptotic Indexes for 14 tumors

Dog #	AI %		
	before IR	6 h after	24 h after
1	12.2		39.7
2	4.3		8.5
3	4.5		17.8
4	3.4		10.1
5	18.9	21.1	19.6
6	6.5	20.8	13.5
7	10.9	33.1	11.39
8	4.2	13.1	13.8
9	13.1	20.1	17
10	13.3	17.2	16.5
11	6.7	23.3	22.3
12	4.9	15.6	16.2
13	8.5	15	9.8
14	7	11.5	12.1
	before IR	6 h after	24 h after

Table 2.4 AI for 14 tumors analyzed from biopsy sections taken before radiation and 6 and 24 hours after dose of 3Gy. First 4 tumors had only before and 24h after radiation results.

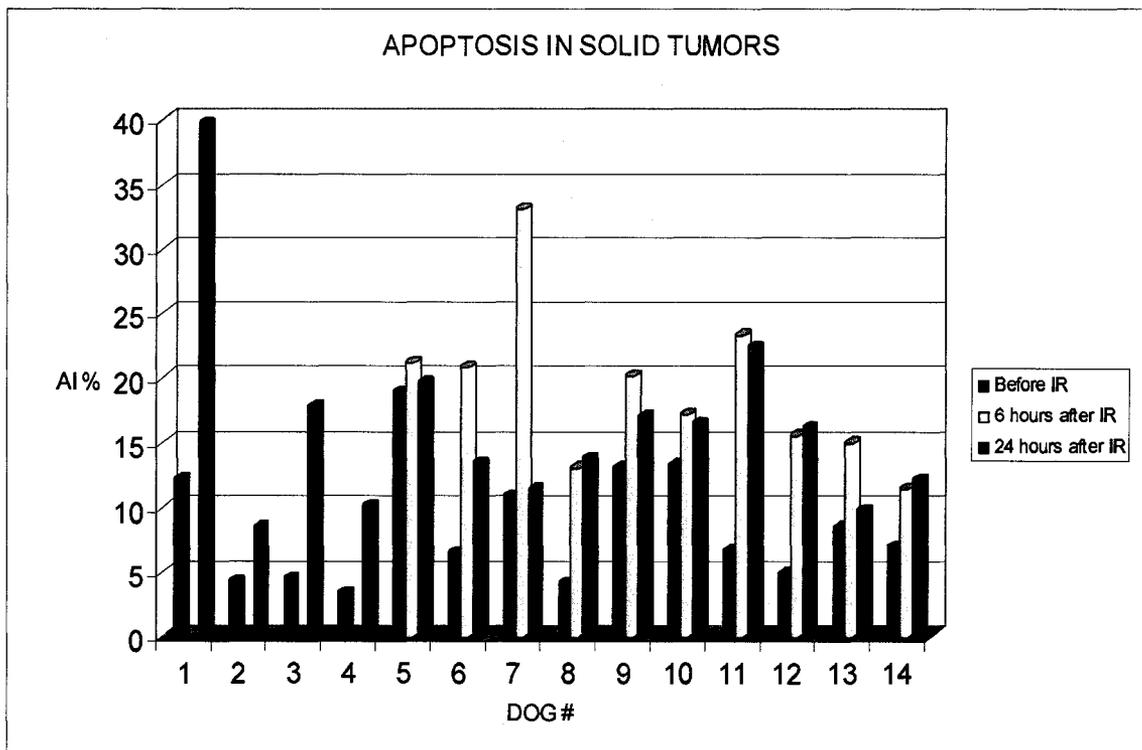


Figure 2.38. Apoptotic Index for each of 14 tumors showing values before (black), 6 hours (yellow), and 24 hours (red) after radiation.

Apoptosis in solid canine tumors

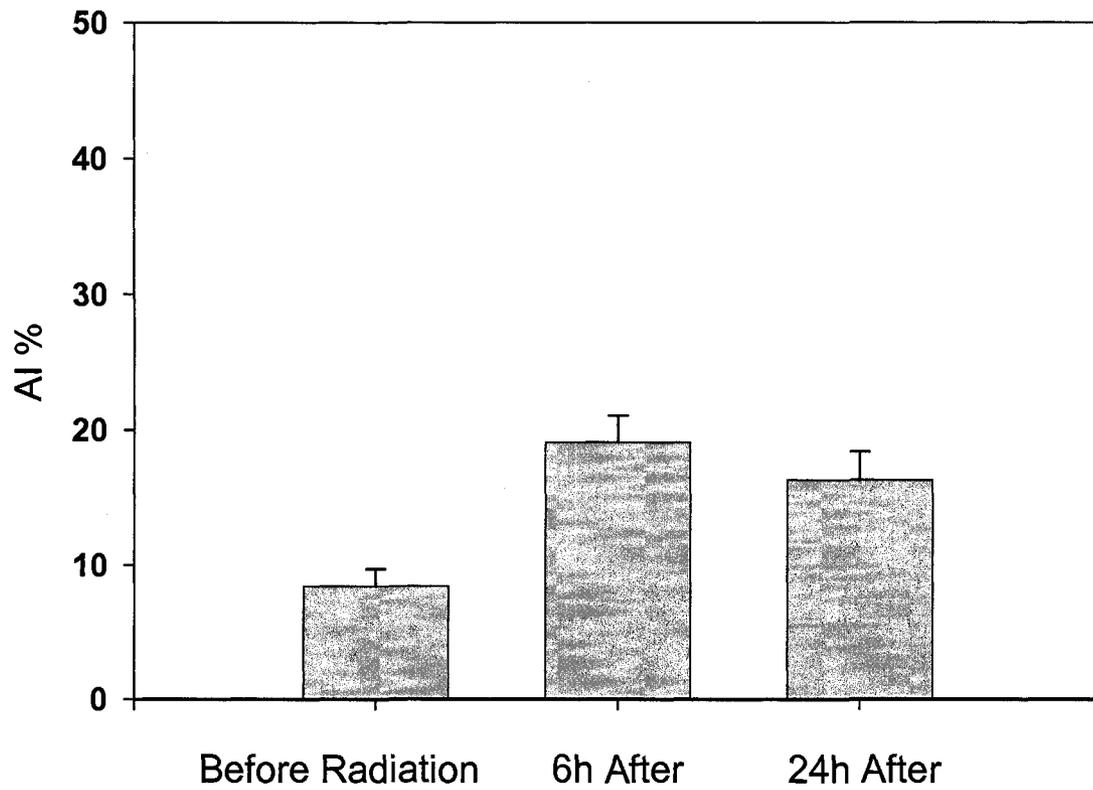


Figure 2.39. Tumor cell apoptosis. Mean values of AI for 14 tumors before, 6 hours, and 24 hours after radiation. Bars=SEM.

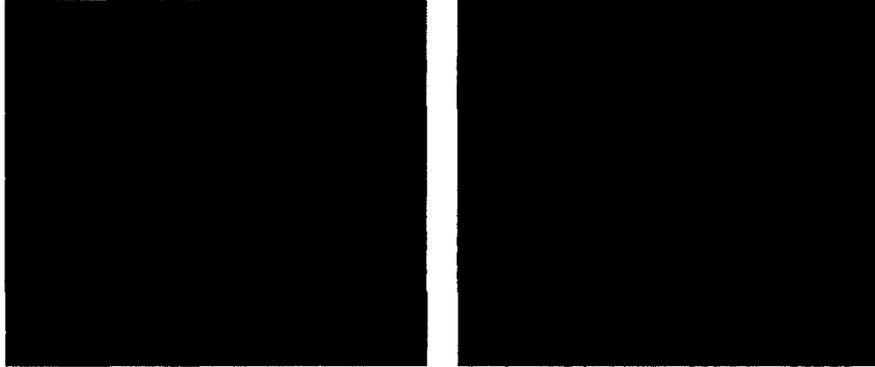


Figure 2.40. Adenocarcinoma tumor sections were stained with TUNEL as described earlier. Green fluorescence marked TUNEL positive apoptotic cells in tumor tissue before radiation (left panel), and after dose of 3 Gy radiation (right panel).

Microvascular density

Microvessels immunohistochemically detected using staining of endothelial cells for factor VIII-related antigen, showed a wide range of counts for different tumors, from 6 to 44 microvessels per field (Table 2.5).

After radiation MVD increased in 6 tumors and decreased in 8 tumors (Figure 2.41) with no correlation to changes in oxygen or other parameters investigated in this study.

Table 2.5. MVD for 14 tumors analyzed from biopsy sections taken before radiation and 24 hours after dose of 3Gy.

Dog #	VASCULAR DENSITY	
	Before	After
1	27	19
2	53	46
3	29	26
4	6	3
5	14	18
6	44	17
7	15	23
8	17	11
9	11	9
10	10	14
11	31	17
12	38	50
13	8	14
14	22	32

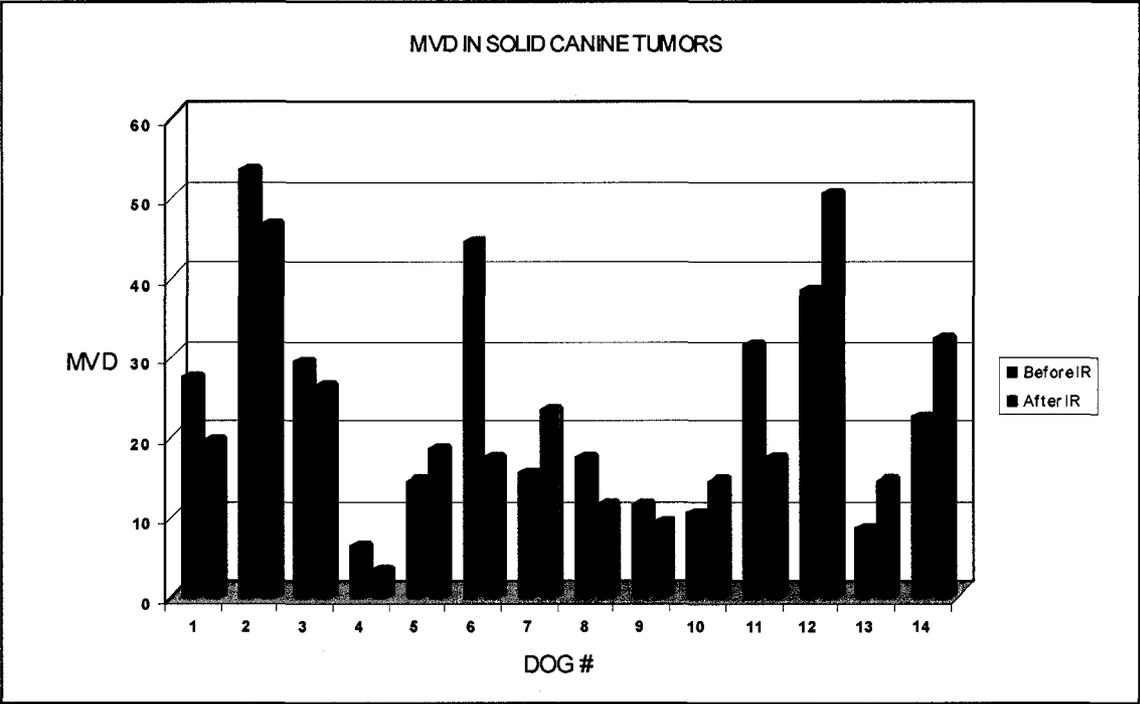


Figure 2.41. Microvessel density for each of 14 tumors showing values before (black), and 24 hours (red) after radiation.

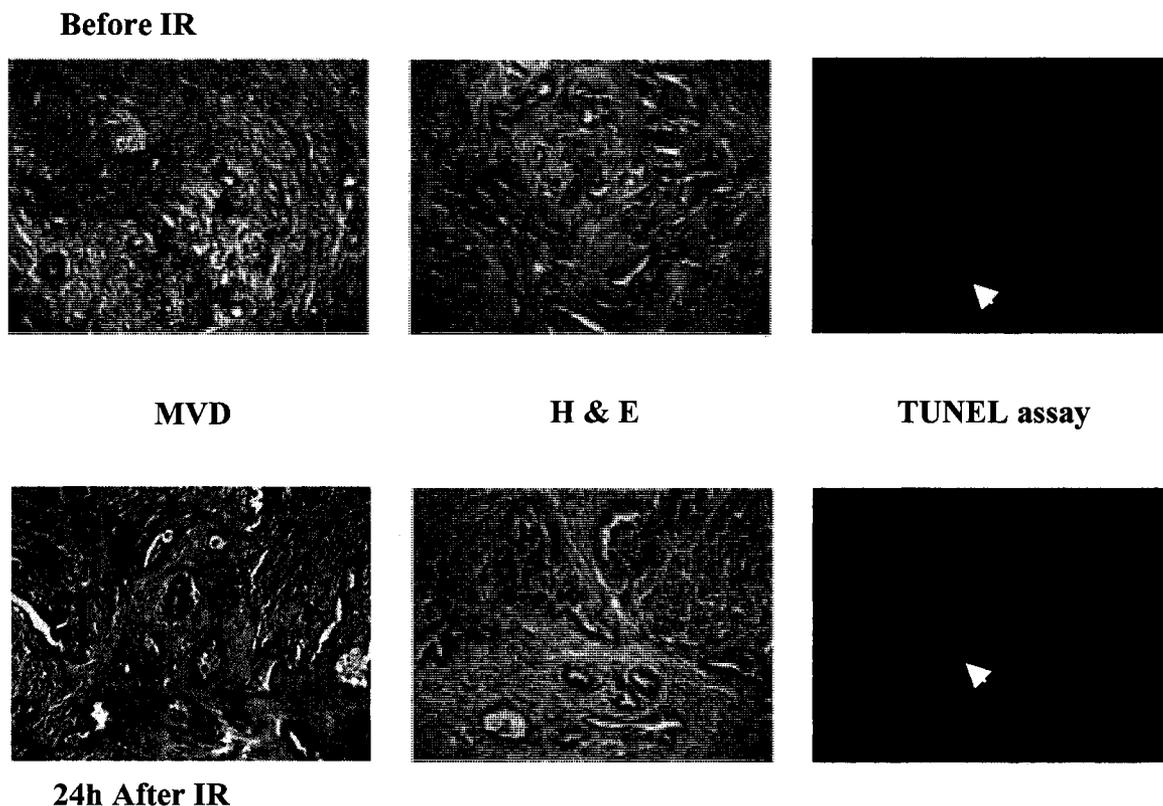


Figure 2.42. Immunohistochemical stainings in adenocarcinoma biopsy specimens pretreatment (upper panel), and 24 hours after irradiation (lower panel). Tumor sections were stained with anti-factor VIII related antibody for MVD quantification, H&E, and TUNEL as described in Materials and Methods.

Integrated Results

Statistical analysis integrating all parameters was provided with assistance from Dr. Annette Bachand and is included in this chapter with original tables, and summaries. As a summary of the study the table with all results for each tumor and each parameter included in this study is presented here (Table 2.6).

Table 2.6. Summary of all results for 14 dogs in the reoxygenation multiparameter study

DOG #	O		X		Y		G		E		N		pO ₂		LDF PERFUSION		CT/MRI PERFUSION		VASCULAR DENSITY		IFP Measurements		APOPTOSIS	
	Before mean±SD	After mean±SD	Before mean±SD	After mean±SD	Before median O ₂	After median O ₂	Before median O ₂	After median O ₂	%<10 mmHg Before	%<10 mmHg After	%<5m mHg Before	%<5m mHg After	%<2.5 before	%<2.5 after	BPU before	BPU after	RPI before	RPI after	Before	After	Before	After	Before	After
1	2.2	12.3	0.3	0.1	0.3	0.1	0.1	0.1	0.1	0.1	0.1	68.2	61.1	101.88	73.63	0.050335	0.047402	27	19	8.8	4.99	12.2	39.7	
2	7.2	2.8	0.4	2.4	0.4	2.4	0.4	0.4	0.4	0.4	0.4	63.4	84.5	50.37	42.22	0.037031	0.004243	53	46	0.26	0.37	4.3	8.5	
3	8.7	38.9	0.3	37.5	0.3	37.5	0.3	0.3	0.3	0.3	0.3	76.5	0	27.12	8.11	0.370206	0.173572	28	28	3.37	1.56	4.5	17.8	
4	21.9	28.1	22.3	26.6	22.3	26.6	22.3	22.3	22.3	22.3	22.3	0	0	486.41	288.71	0.181723	0.253197	6	3	-0.59	-3.41	3.4	10.1	
5	19.4	10.9	21.5	11	21.5	11	21.5	21.5	21.5	21.5	21.5	0	16.7	191.74	227.5	0.032	-0.0336	14	18	-7.11	-7.21	18.9	19.6	
6	30.5	21	32.1	14.2	32.1	14.2	32.1	32.1	32.1	32.1	32.1	2.5	35.9	214.18	128.93	14.26	8.21	44	17	-0.48	-0.53	6.5	13.5	
7	19.5	13.3	17.8	19.8	17.8	19.8	17.8	17.8	17.8	17.8	17.8	0	15.8	92.47	193.85	11	-3.3477	15	23	1.02	0.9	10.9	11.39	
8	9.2	23.2	0.4	14.2	0.4	14.2	0.4	0.4	0.4	0.4	0.4	51.5	0	97.12	136.9	23.72	-0.5478	17	11	1.03	0.34	4.2	13.8	
9	22.2	25	23.7	25.3	23.7	25.3	23.7	23.7	23.7	23.7	23.7	0	0	132.8	94.7	21.04	16.813	11	9	1.58	-0.18	13.1	17	
10	3.6	22.2	2.9	19.9	2.9	19.9	2.9	2.9	2.9	2.9	2.9	47.2	25.7	244.4	159.7	34.73	16.25	10	14	3.33	-0.68	13.3	16.5	
11	16.6	27.7	20.9	26.1	20.9	26.1	20.9	20.9	20.9	20.9	20.9	28	4.5	204.81	N/A	9.52	7.68	31	17	9.83	3.85	6.7	22.3	
12	17.1	13.1	16	12.7	16	12.7	16	16	16	16	16	0	17.2	123.63	422.46	9.33	4.16	38	50	-0.65	-7.45	4.9	16.2	
13	10.6	29.6	6.1	34.3	6.1	34.3	6.1	6.1	6.1	6.1	6.1	38.6	4.5	340.03	235.89	16.34	9.38	8	14	8.6	0.63	8.5	9.8	
14	7.2	31.2	1.8	31	1.8	31	1.8	1.8	1.8	1.8	1.8	55.3	0	119.44	132.08	24.31	20.42	22	32	1.8	10.45	7	12.1	

Table 2.6 All mean and median pO₂ for 14 canine tumors, with percent measurements less than 10, 5, and 2,5 mmHg, microvascular perfusion estimates measured with laser Doppler flowmetry (LDF), and with dynamic contrast enhanced (DCE) computed tomography (CT) (first 5 dogs) and magnetic resonance imaging (MRI), microvessel density, interstitial fluid pressure (IFP), and apoptotic index before and after 3 Gy radiation. Red numbers in the oxygen measurements indicate increase in mean/median pO₂, and decrease in hypoxic fractions presented as percentages of measurements less than 10, 5, and 2,5 mmHg.

In Tables 2.7 through 2.16, statistical analyses are presented with interpretations and conclusions.

Table 2.7. Shapiro-Wilk test for normality p-value, paired t-test p-value, signed rank test p-value, and mean and Standard deviation of the difference between measurements taken after radiation and measurements taken prior to radiation – all 14 dogs.

Variable	Shapiro-Wilk p-value	Paired t-test p-value	Signed Rank test p-value	Mean	Std
post-pre O ₂ mean	0.4891	0.0538	0.0701	7.24	12.78
post-pre O ₂ median	0.5491	0.1105	0.1763	7.29	15.93
post-pre O ₂ 1 st quartile	0.9291	0.2214	0.2749	4.89	14.23
post-pre O ₂ 3 rd quartile	0.9996	0.0507	0.0676	10.23	17.78
post-pre % O ₂ < 10 mmHg	0.3134	0.1579	0.2676	-15.3	38.08
post-pre % O ₂ < 5 mmHg	0.3608	0.1350	0.0923	-14.8	34.83
post-pre % O ₂ < 2.5 mmHg	0.4652	0.1713	0.1294	-12.8	33.09
post-pre perfusion (LDF)	0.1871	0.8461	0.5879	-6.60	120.0
post-pre perfusion (CT/MRI)	0.0045	0.0106	0.0009	-6.10	7.66
post-pre microvascular density	0.3626	0.5183	0.7964	-1.86	10.47
post-pre interstitial fluid pressure	0.0898	0.0963	0.0245	-1.94	4.05
post-pre % apoptosis	0.0281	0.0015	0.0001	7.85	7.33
In (post-pre % apoptosis)	0.4788	0.0002	0.0012	1.57	1.17

Table 2.8. Shapiro-Wilk test for normality p-value, paired t-test p-value, signed rank test p-value, and mean and Standard deviation of the difference between measurements taken after radiation and measurements taken prior to radiation – 7 hypoxic dogs (median pO₂ before radiation <10mmHg)

Variable	Shapiro-Wilk p-value	Paired t-test p-value	Signed Rank test p-value	Mean	Std
post-pre O ₂ mean	0.7484	0.0089	0.0313	15.93	11.08
post-pre O ₂ median	0.4677	0.0177	0.0625	17.94	14.66
post-pre O ₂ 1 st quartile	0.3315	0.0438	0.0625	12.26	12.74
post-pre O ₂ 3 rd quartile	0.0494	0.0465	0.1094	19.57	20.71
post-pre % O ₂ < 10 mmHg	0.3935	0.0192	0.0469	-40.8	33.98
post-pre % O ₂ < 5 mmHg	0.5732	0.0203	0.0313	-38.1	32.22
post-pre % O ₂ < 2.5 mmHg	0.7980	0.0267	0.0313	-34.4	31.20
post-pre perfusion (LDF)	0.6960	0.2065	0.2969	-27.4	51.18
post-pre perfusion (CT/MRI)	0.0503	0.0840	0.0156	-7.69	9.83
post-pre microvascular density	0.2847	0.8398	0.8438	-0.57	7.16
post-pre interstitial fluid pressure	0.3840	0.5112	0.3750	-1.36	5.16
post-pre % apoptosis	0.0716	0.0366	0.0156	9.17	9.06
ln (post-pre % apoptosis)	0.9945	0.0031	0.0156	1.81	1.00

Table 2.9. Shapiro-Wilk test for normality p-value, paired t-test p-value, signed rank test p-value, and mean and Standard deviation of the difference between measurements taken after radiation and measurements taken prior to radiation in 7 non-hypoxic dogs (median pO₂ before radiation ≥10mmHg)

Variable	Shapiro-Wilk p-value	Paired t-test p-value	Signed Rank test p-value	Mean	Std
post-pre O ₂ mean	0.3588	0.6259	0.6250	-1.44	7.43
post-pre O ₂ median	0.4849	0.3311	0.4688	-3.36	8.40
post-pre O ₂ 1 st quartile	0.9643	0.6102	0.5781	-2.49	12.23
post-pre O ₂ 3 rd quartile	0.6708	0.7569	0.8125	0.89	7.23
post-pre % O ₂ < 10 mmHg	0.5489	0.2555	0.2188	10.27	21.62
post-pre % O ₂ < 5 mmHg	0.6299	0.2605	0.4375	8.46	18.01
post-pre % O ₂ < 2.5 mmHg	0.6235	0.2342	0.4375	8.80	17.61
post-pre perfusion (LDF)	0.9514	0.8130	1.0000	17.65	173.5
post-pre perfusion (CT/MRI)	0.1523	0.0526	0.0469	-4.52	4.96
post-pre microvascular density	0.5888	0.5604	0.8125	-3.14	13.50
post-pre interstitial fluid pressure	0.0860	0.0579	0.0156	-2.52	2.85
post-pre % apoptosis	0.5895	0.0203	0.0156	6.53	5.52
ln (post-pre % apoptosis)	0.1801	0.0403	0.0781	1.33	1.35

Summary:

In hypoxic dogs the mean, median, 1st and 3rd quartile of the pO₂ measurements increased significantly and the percentage of pO₂ measurements below 10 mmHg, 5 mmHg and 2.5 mmHg decreased significantly, but a similar trend was not observed in non-hypoxic dogs.

In all dogs (hypoxic, non-hypoxic and combined) microvascular perfusion decreased significantly when microvascular perfusion was measured by CT/MRI but not when it was measured by LDF In all dogs (hypoxic, non-hypoxic and combined) microvascular

density did not change significantly. In all dogs (hypoxic, non-hypoxic and combined) interstitial fluid pressure decreased, but the decrease was not significant in hypoxic dogs. In all dogs (hypoxic, non-hypoxic and combined) percent apoptosis increased significantly.

	Variables	Pearson correlation coefficient	Pearson p-value	Spearman correlation coefficient	Spearman p-value
post-pre O ₂ mean	post-pre perfusion (LDF)	-0.29330	0.3308	-0.19780	0.5171
	post-perfusion (CT/MRI)	-0.12304	0.6752	-0.09011	0.7593
	post-pre microvascular density	0.21014	0.4709	0.16520	0.5725
	post-pre IFP	0.04081	0.8898	-0.33626	0.2398
	post-pre % apoptosis	0.22957	0.4298	0.27473	0.3418
	ln (post-pre % apoptosis)	0.32657	0.2545	0.27473	0.3418
post-pre O ₂ median	post-pre perfusion (LDF)	-0.22037	0.4694	-0.25860	0.3936
	post-pre perfusion (CT/MRI)	-0.12011	0.6825	-0.11881	0.6858
	post-pre microvascular density	0.35638	0.2111	0.14774	0.6142
	post-pre IFP	0.08529	0.7719	-0.22662	0.4359
	post-pre % apoptosis	0.00249	0.9932	0.12101	0.6803
	ln (post-pre % apoptosis)	0.11636	0.6920	0.12101	0.6803
post-pre O ₂ 1 st quartile	post-pre perfusion (LDF)	-0.15327	0.6171	-0.23659	0.4364
	post-pre perfusion (CT/MRI)	0.05273	0.8579	-0.00440	0.9881
	post-pre microvascular density	0.28931	0.3157	0.06836	0.8164
	post-pre IFP	0.04966	0.8661	-0.22662	0.4359
	post-pre % apoptosis	0.14898	0.6112	0.21782	0.4544
	ln (post-pre % apoptosis)	0.21261	0.4655	0.21782	0.4544
post-pre O ₂ 3 rd quartile	post-pre perfusion (LDF)	-0.29740	0.3237	-0.31319	0.2974
	post-pre perfusion (CT/MRI)	-0.21310	0.4645	-0.20000	0.4930
	post-pre microvascular density	0.06819	0.8168	0.00881	0.9762
	post-pre IFP	-0.04414	0.8809	-0.29670	0.3030
	post-pre % apoptosis	0.31071	0.2796	0.33187	0.2464
	ln (post-pre % apoptosis)	0.37650	0.1846	0.33187	0.2464
pre perfusion (LDF)	pre perfusion (CT/MRI)	0.03564	0.9037	0.21319	0.4643
post perfusion (LDF)	post perfusion (CT/MRI)	-0.05481	0.8588	0.01099	0.9716

	Variables	Pearson correlation coefficient	Pearson p-value	Spearman correlation coefficient	Spearman p-value
post-pre O ₂ mean	post-pre perfusion (LDF)	-0.13566	0.7718	-0.10714	0.8192
	post-pre perfusion (CT/MRI)	-0.08792	0.8513	-0.25000	0.5887
	post-pre microvascular density	0.56200	0.1892	0.75000	0.0522
	post-pre IFP	0.08776	0.8516	-0.07143	0.8790
	post-pre % apoptosis	-0.03433	0.9418	-0.03571	0.9394
	ln (post-pre % apoptosis)	0.01710	0.9710	-0.03571	0.9394
	post-pre O ₂ median	post-pre perfusion (LDF)	-0.15559	0.7391	-0.07207
post-pre perfusion (CT/MRI)		0.00799	0.9864	-0.27028	0.5577
post-pre microvascular density		0.64014	0.1215	0.77481	0.0408
post-pre IFP		0.11970	0.7982	-0.01802	0.9694
post-pre % apoptosis		-0.34906	0.4428	-0.10811	0.8175
ln (post-pre % apoptosis)		-0.26852	0.5604	-0.10811	0.8175
post-pre O ₂ 1 st quartile		post-pre perfusion (LDF)	0.10289	0.8263	0.10811
	post-pre perfusion (CT/MRI)	0.19526	0.6748	-0.30632	0.5040
	post-pre microvascular density	0.40367	0.3692	0.70273	0.0782
	post-pre IFP	0.22970	0.6203	0.09009	0.8477
	post-pre % apoptosis	-0.14497	0.7565	0.00000	1.0000
	ln (post-pre % apoptosis)	-0.02576	0.9563	0.00000	1.0000
	post-pre O ₂ 3 rd quartile	post-pre perfusion (LDF)	-0.16105	0.7301	0.00000
post-pre perfusion (CT/MRI)		-0.25324	0.5837	-0.42857	0.3374
post-pre microvascular density		0.36804	0.4166	0.53571	0.2152
post-pre interstitial fluid pressure		-0.09667	0.8367	-0.07143	0.8790
post-pre % apoptosis		0.17227	0.7119	0.07143	0.8790
ln (post-pre % apoptosis)		0.18666	0.6886	0.07143	0.8790
pre perfusion (LDF)		pre microvascular perfusion (CT/MRI)	0.55729	0.1937	0.57143
	post perfusion (LDF)	0.55644	0.1945	0.32143	0.4821

	Variables	Pearson correlation coefficient	Pearson p-value	Spearman correlation coefficient	Spearman p-value
post-pre O ₂ mean	post-pre perfusion (LDF)	-0.42967	0.3952	-0.20000	0.7040
	post-pre perfusion (CT/MRI)	0.42441	0.3426	0.50000	0.2532
	post-pre microvascular density	-0.09710	0.8359	-0.10714	0.8192
	post-pre IFP	-0.57471	0.1771	-0.78571	0.0362
	post-pre % apoptosis	0.56758	0.1838	0.42857	0.3374
	ln (post-pre % apoptosis)	0.55325	0.1977	0.42857	0.3374
	post-pre O ₂ median	post-pre perfusion (LDF)	-0.17530	0.7397	-0.25714
post-pre perfusion (CT/MRI)		0.15667	0.7373	0.42857	0.3374
post-pre microvascular density		0.26113	0.5716	-0.14286	0.7599
post-pre IFP		-0.48098	0.2745	-0.64286	0.1194
post-pre % apoptosis		0.30444	0.5068	0.25000	0.5887
ln (post-pre % apoptosis)		0.23998	0.6042	0.25000	0.5887
post-pre O ₂ 1 st quartile		post-pre perfusion (LDF)	-0.11465	0.8288	-0.25714
	post-pre perfusion (CT/MRI)	0.25210	0.5855	0.42857	0.3374
	post-pre microvascular density	0.20839	0.6539	-0.14286	0.7599
	post-pre IFP	-0.54117	0.2097	-0.64286	0.1194
	post-pre % apoptosis	0.41012	0.3608	0.25000	0.5887
	ln (post-pre % apoptosis)	0.23571	0.6109	0.25000	0.5887
	post-pre O ₂ 3 rd quartile	post-pre perfusion (LDF)	-0.67128	0.1443	-0.77143
post-pre perfusion (CT/MRI)		0.64918	0.1146	0.53571	0.2152
post-pre microvascular density		-0.56464	0.1866	-0.67857	0.0938
post-pre IFP		-0.44502	0.3170	-0.42857	0.3374
post-pre % apoptosis		0.66766	0.1012	0.67857	0.0938
ln (post-pre % apoptosis)		0.80674	0.0283	0.67857	0.0938
pre perfusion (LDF)		pre perfusion (CT/MRI)	-0.58323	0.1693	-0.21429
post perfusion (LDF)	post perfusion (CT/MRI)	-0.47717	0.3386	-0.42857	0.3965

Summary:

In all dogs (hypoxic, non-hypoxic and combined) no consistent statistically significant correlations were observed between changes in tumor pO₂ levels (mean, median, 1st or 3rd quartile) and changes in microvascular perfusion, microvascular density, interstitial fluid pressure or percent apoptosis.

While in hypoxic dogs the association between changes in tumor pO₂ levels (mean, median and 1st quartile) and changes in microvascular density was borderline significant based on the Spearman correlation coefficients, it was not significant based on the Pearson correlation coefficients.

While in non-hypoxic dogs the association between changes in mean tumor pO₂ levels and changes in interstitial fluid pressure was significant based on the Spearman correlation coefficient, it was not significant based on the Pearson correlation coefficient. Furthermore, no significant association was observed between changes in interstitial fluid pressure and changes in median, 1st quartile or 3rd quartile tumor pO₂ levels.

While in non-hypoxic dogs, the associations between changes in the 3rd quartile of tumor pO₂ levels and several other variables were significant at the 0.1 level based on the Spearman correlation coefficient, all but one of these associations were not significant based on the Pearson correlation coefficient. There were no statistically significant corresponding associations observed when changes in the mean, median or 1st quartile of tumor pO₂ levels were considered.

In all dogs (hypoxic, non-hypoxic and combined) no significant correlation was observed between before and after microvascular perfusion measured by LDF and measured by CT/MRI.

To further explore whether there was an association between changes in tumor pO₂ levels and changes in microvascular perfusion, microvascular density, interstitial fluid pressure and percent apoptosis, all variables were dichotomized. The cutpoints (table 2.14) were determined based on the data shown in table 2.13.

Table 2.13. Changes in mean and median tumor pO₂ levels and changes in microvascular perfusion, microvascular density, interstitial fluid pressure and percent apoptosis for all 14 dogs

id	post-pre O ₂ mean	post-pre O ₂ median	post-pre perfusion (LDF)	post-pre perfusion (CT/MRI)	post-pre microvascular density	post-pre IFP	post-pre % apoptosis
1	10.1	0.0	-28.25	-0.0029	-8	-3.81	27.50
2	-4.4	0.0	-8.15	-0.0328	-7	0.11	4.20
3	30.2	37.8	-19.01	-0.1966	-3	-1.81	13.30
4	6.2	4.6	-206.70	0.0715	-3	-2.82	6.70
5	-8.5	-10.8	35.76	-0.0656	4	-0.10	0.70
6	-9.5	-17.3	-85.25	-6.0500	-27	-0.05	7.00
7	-6.2	-2.2	101.38	-14.3477	8	-0.12	0.49
8	14.0	13.8	39.78	-24.2678	-6	-0.69	9.60
9	2.8	2.3	-38.10	-4.2270	-2	-1.76	3.90
10	18.6	16.6	-84.70	-18.4800	4	-4.01	3.20
11	9.1	5.2	.	-1.8400	-14	-5.98	15.60
12	-4.0	-5.3	298.83	-5.1500	12	-6.80	11.30
13	19.0	28.2	-104.04	-6.9600	6	-7.97	1.30
14	24.0	29.2	12.64	-3.8900	10	8.65	5.10

Table 2.14. Cutpoints for dichotomizing the change in O₂ levels, microvascular perfusion, microvascular density, interstitial fluid pressure and percent apoptosis variables

Variable	0 if	1 if
post-pre O ₂ mean	≤0	>0
post-pre O ₂ median	≤0	>0
post-pre microvascular perfusion (LDF)	≤0	>0
post-pre microvascular perfusion (CT/MRI)	≤ -0.2	> -0.2
post-pre microvascular density	≤0	>0
post-pre interstitial fluid pressure	≤ -0.2	> -0.2
post-pre % apoptosis	≤ 1.5	> 1.5

Table 2.15. Observed and expected number of observations and Chi Square test and Fisher's Exact test p-values for the change in mean pO₂ vs. the change in microvascular perfusion, microvascular density, interstitial fluid pressure and percent apoptosis for all 14 dogs

post-pre O ₂ mean		Obs	Exp	Obs	Exp	Chi Square test p-value	Fisher's Exact Test p-value
	post-pre microvascular perfusion (LDF)	0		1		0.2070	0.2929
0		2	3.07692	3	1.92308		
1		6	4.92308	2	3.07692		
	post-pre microvascular perfusion (CT/MRI)	0		1		0.8030	1.0000
0		3	3.21429	2	1.78571		
1		6	5.78571	3	3.21429		
	post-pre microvascular density	0		1		0.3340	0.5804
0		2	2.85714	3	2.14286		
1		6	5.14286	3	3.85714		
	post-pre interstitial fluid pressure	0		1		0.0099	0.0230
0		1	3.21429	4	1.78571		
1		8	5.78571	1	3.21429		
	post-pre % apoptosis	0		1		0.2069	0.5055
0		2	1.07143	3	3.92857		
1		1	1.92857	8	7.07143		

Table 2.16. Observed and expected number of observations and Chi Square test and Fisher's Exact test p-values for the change in median pO₂ vs. the change in microvascular perfusion, microvascular density, interstitial fluid pressure and percent apoptosis for all 14 dogs

post-pre O ₂ median		Obs	Exp	Obs	Exp	Chi Square test p-value	Fisher's Exact Test p-value
	post-pre microvascular perfusion (LDF)	0		1		0.4285	0.5921
0		3	3.69231	3	2.30769		
1		5	4.30769	2	2.69231		
	post-pre microvascular perfusion (CT/MRI)	0		1		0.3340	0.5804
0		3	3.85714	3	2.14286		
1		6	5.14286	2	2.85714		
	post-pre microvascular density	0		1		0.6400	1.0000
0		3	3.42857	3	2.57143		
1		5	4.57143	3	3.42857		
	post-pre interstitial fluid pressure	0		1		0.0363	0.0909
0		2	3.85714	4	2.14286		
1		7	5.14286	1	2.85714		
	post-pre % apoptosis	0		1		0.3472	0.5385
0		2	1.28571	4	4.71429		
1		1	1.71429	7	6.28571		

Summary

There was evidence of a statistically significant association between the change in mean tumor pO₂ levels (≤ 0 vs. > 0) and the change in interstitial fluid pressure (≤ -0.2 vs. > -0.2), and there was evidence of a statistically significant association between the change in median tumor pO₂ levels (≤ 0 vs. > 0) and the change in interstitial fluid pressure (≤ -0.2 vs. > -0.2).

Among dogs with a post-pre mean $pO_2 \leq 0$, fewer than expected (based on an assumption of independence) experienced a change in interstitial fluid pressure of ≤ -0.2 and more than expected experienced a change in interstitial fluid pressure of > -0.2 .

Among dogs with post-pre pO_2 mean > 0 , more than expected (based on an assumption of independence) experienced a change in interstitial fluid pressure of ≤ -0.2 and fewer than expected experienced a change in interstitial fluid pressure of > -0.2 .

Results for the change in median pO_2 levels were similar.

In other words, dogs that experienced an increase in mean (median) tumor pO_2 levels had an increased likelihood of experiencing a decrease of more than 0.2 in interstitial fluid pressure, whereas dogs who experienced a decrease in mean (median) tumor pO_2 levels had a decreased likelihood of experiencing a decrease of more than 0.2 in interstitial fluid pressure.

DISCUSSION

Changes in partial pressure of oxygen (pO_2) of canine tumors following a fraction of radiation were evaluated. These tumors were heterogeneous, and the initial oxygen levels in the tumors as well as the changes post-radiation varied but there were two general patterns. Hypoxic tumors became better oxygenated, while well oxygenated tumors did not change out of normoxic range. These changes were analyzed in relation with changes in interstitial fluid pressure, microvascular perfusion, frequency of apoptosis, and microvessel density. Multiparameter analysis was used to try to elucidate underlying mechanisms of tumor reoxygenation. Different tumor microenvironmental

parameters did not interact as hypothesized prior the study. The only evident relationship was the inverse correlation between values of oxygen levels and interstitial fluid pressures.

Oxygen tension

The pO₂ was increased 24 hours after 3 Gy in 9 tumors, and decreased in 5 tumors. More importantly, oxygen levels increased in hypoxic tumors, and only in 1 hypoxic tumor pO₂ decreased (#2, soft tissue sarcoma). All tumors that reoxygenated in our study had a significantly decreased fraction of pO₂ measurements below 10 mm Hg, 5 mm Hg, and 2.5 mm Hg, meaning that the hypoxic fraction of these tumors decreased after radiation. Changes in well oxygenated tumors were not relevant for the treatment outcome since after radiation the mean/median pO₂ in these tumors if decreased, did not decrease below 10 mm Hg. Similar observations have been reported in studies on human cervix tumors, breast tumors, head and neck tumors, and nonsmall cell lung tumors (Lyng et al, 2000; Pappova et al, 1982; Lartigau et al, 1998; Lyng et al, 1999; Koh et al, 1995). As was reported in studies in human cervical tumors (Lyng et al, 2000; Dunst et al, 1999), hypoxic tumors may became better oxygenation during radiation therapy, whereas the oxygenation most often decreased in well-oxygenated tumors, similar to our results. Most of the studies of changes in oxygenation status are reporting different doses used, different tumor models, different time points of measurements. All this makes it very difficult to compare results from all these different studies and to make general conclusions about tumor microenvironment behavior following irradiation. In human tumors measurements were made during fractionated radiation therapy after two weeks of

radiation therapy (Lartigau et al, 1998; Gabalski et al, 1998; Lyng et al, 2000), after four weeks of radiation (Fyles et al, 1998; Cooper et al, 1999), or at the end of the treatment. A benefit of the spontaneous tumor model in dogs allowed me to look at oxygen levels at a time point that may be more relevant.

There is evidence that the reoxygenation of tumors occurs 24-72 hours after irradiation (Vaupel et al, 1984; Kallman et al, 1986; Koutcher et al, 1992; Goda et al, 1995; Znati et al, 1996; Bussink et al, 2000). This is closer to the time point we chose in our study.

However, most of these studies obtained data after single high irradiation dose and in experimental animal tumors. Some studies that reported oxygen changes up to 24 hours following clinically relevant dose (2 Gy) were also in experimental murine tumors that are not heterogeneous as naturally developing tumors in. Nevertheless, some studies reported no significant change in pO_2 post-radiation in regard to pre-treatment values (Fyles et al, 1998) or decrease in the overall oxygenation of the tumors after radiation treatment (Gabalski et al, 1998; Achermann et al, 2004).

The discrepancy between findings of the different studies may have a number of reasons. The timing of the post-radiation measurement may be important, as well as the fractionation scheme used. Another contribution to the differences in these findings may be measurement related, consisting of intratumor heterogeneity, measurement method and operator variability.

I investigated the changes of oxygenation level and other relevant microenvironmental parameters in tumors following a fraction of radiation using a fraction size similar to those applied to human malignancies. I chose to look after a single time point to focus on the underlying mechanisms of reoxygenation. Changes of oxygen levels after single dose

of fractionated treatment are of relevance for the eventual manipulation in subsequent fractionation scheduling. Our findings are in agreement with earlier reported observations that these changes vary among different tumors (even same type tumors) and the extent of the reoxygenation is different.

Interstitial fluid pressure

Interstitial fluid pressure in this study was shown to decrease in most tumors after irradiation. It decreased in 9 out of 14 tumors. In 4 tumors it did not change more than 0.2 mm Hg, and in one tumor IFP increased after irradiation. A significant inverse correlation existed between changes in IFP and changes in oxygen levels in tumors after irradiation. This was the only significant relationship among microenvironmental parameters in this study. We did not see a relationship between the other parameters and IFP in this study. This may be due to the large number of factors that play a role in tumor IFP such as capillary pressure, the resistance of fluid leakage across the capillary walls, and the resistance of fluid percolation through the interstitium (Milosevic et al, 1999; Baxter et al, 1989; Tufto et al, 1999).

An inverse relation between tumor IFP and oxygenation was first suggested based on measurements taken in three patients with cervical carcinoma (Roh et al, 1991). A later study with a much larger population of patients (77 cervical carcinoma patients) demonstrated an inverse association between these parameters (Milosevic et al, 1998). However, with further increase of the number of patients in the study, the strength of this association diminished, but this study was the first to demonstrate a strong independent prognostic effect of IFP (Milosevic et al, 2001). Studies of IFP and the oxygenation in

animal tumors have similarly failed to show a correlation between them (Boucher et al, 1995; Tufto et al, 1996; Znati et al, 1996).

Our study demonstrated moderate negative correlation between the changes in pO_2 and the changes in the IFP in solid canine tumors after single dose of radiation. Considering the size of our patient population and reviewing studies previously mentioned here, it may be necessary to obtain more data for more conclusive demonstration of the pO_2 -IFP relationship we found here.

It was reported from work with human tumor xenografts in mice (Znati et al, 1996), that irradiation with doses smaller than 10 Gy (delivered in 2.5 and 5 Gy fractions) did not affect the IFP of the tumor. The association between IFP and pO_2 is presumed to be due to changes in tumor blood flow and oxygen delivery (Jain et al, 1988; Boucher et al, 1992). It is also possible that IFP provides information about tumor physiology that is unrelated to perfusion (Milosevic et al, 2001). Some of the characteristics of tumors that lead to elevated IFP include abnormal vessel structure and organization, and high vascular permeability. My study found that perfusion actually decreased in most tumors after irradiation, and that decreased IFP and increased oxygenation were not related to increase of perfusion. A possible explanation may be a change of vascular permeability. Decrease in vascular permeability consequently could increase transvascular resistance, which would decrease the amount of fluid entering the interstitium. Understanding how tumor vasculature responds to irradiation seems important for understanding the relationship between IFP and tumor vasculature. It has been demonstrated recently that irradiation induces secretion of VEGF, a potent angiogenic protein, and that VEGF

enhances endothelial cell radioresistance, protecting tumors from radiation damage by minimizing vascular damage (Gorski et al, 1999; Moeller et al, 2004).

Tumor microvascular perfusion

Two different techniques used to estimate perfusion in each tumor, LDF and DCE (CT/MRI), did not show the same pattern of changes in perfusion in irradiated tumors.

More uniform findings were obtained from dynamic contrast enhancement techniques: in 13 out of 14 tumors, they indicated decreased perfusion 24 hours after irradiation. Data obtained from LDF were different: 8 out of 13 tumors showed decreased perfusion post-radiation. In one of the tumors post-radiation data were not obtained (dog #11).

For the dogs #7, 8, and 9, individual RPI graphs could not be obtained. This is because there were motion artifacts on either the pre or post-radiation MRI scan, making it invalid to calculate RPI measurements for individual ROI's. The ROI's at the edges of those tumors could not be compared due to excess motion. Instead, Dr. Kraft calculated RPI for a central tumor ROI, which was a similar tissue region before and after irradiation. Those are the RPI numbers included in the results table (Table 2.3) and for those three dogs the average RPIs are included in the Figure 2.35.

The data obtained from LDF were difficult to present and analyze. There were numerous out of range values caused by both movement of the patient and movement of the probe during sampling. Most of the data reported in the literature was generated from stationary measurements (Lan et al, 2000; Thews et al, 2002) utilizing a constant probe location. A laser is used as the stable source of light in these instruments so that Doppler shift (i.e. the frequency change that light undergoes when reflected by object in motion, such as red

blood cells) could be utilized. We used a combined pO₂/ temperature/ LDF probe and in order to record tumor spatial heterogeneity, we moved the probe along the track of measurements. There were measurement artifacts as a result of the probe movements that manifested in the sudden changes of the total backscattered light. I excluded those values from the final evaluation. When that happens in a few instances during the recording it did not change the outcome of the evaluation of the measurements. We had probe withdrawn each 5 seconds for 0.2mm, and removing many of the spikes in flow signal, compromised the accuracy of the LDF tumor perfusion estimate.

Non-invasive tumor perfusion measurements by DCE-CT have been reported in studies in head and neck squamous cell carcinoma in human patients (Hermans et al, 1997, 1999; Brix et al, 1999), and in canine nasal tumors (Van Camp et al, 2000). They proved that CT-determined perfusion measurements are feasible; the procedure is safe and easy to perform. Studies using Gd-DTPA as MRI contrast agent in experimental murine tumors demonstrated the sensitivity of the DCE-MRI technique and its capability of providing estimates of blood perfusion in normal and tumor tissues (Belfi et al, 1992, 1994).

Results were reported from the studies with experimental animal models (Bjornaes et al, 2000; Bhujwala et al, 2001, 2003; Crockart et al, 2005) and DCE-MRI measurements of cervical tumors of human patients (Lyng et al, 2001; Haider et al, 2007). These studies show a spatial-temporal heterogeneity of perfusion in tumors, consistent with chaotic vascular architecture.

Our finding of decreased tumor perfusion did not support our hypothesis that reoxygenation occurs due to increased microvascular perfusion and reopening of collapsed vessels post-radiation. This finding was in agreement with recently reported

results from the study of the effect of irradiation of single 10 Gy dose in experimental tumors in mice using perfusion markers (Bussink et al, 2000; Fenton et al, 2001). In a study utilizing irradiation with 2 Gy dose in experimental tumors assessing tumor perfusion with LDF and DCE-MRI (Crokart et al, 2005) measurements were made 4 hours after irradiation and showed increased pO₂, which remained elevated for at least 24 hours, and increased tumor perfusion at 4 hours. Bussink also reported an early increase in perfused blood vessels at 2-7 hours after irradiation) followed by significant decrease, with a minimum value at 26 hours after irradiation. The decrease in tumor blood perfusion has been attributed to radiation-induced edema, thrombosis (Falkvoll, 1990), and an increase in damaged capillaries as a direct effect of irradiation (Goda et al, 1996). Other investigators have suggested that increases in tumor blood flow might be responsible for reoxygenation (Kallman, 1972; Brown, 1979; Rofstad, 1989). Some authors tried to explain reoxygenation, depending on time after radiation it occurred, to be due to acutely or due to chronically hypoxic cells. In the SCCVII murine tumor reoxygenation was found to be very rapid (within the first 6 hours after a 13 Gy radiation). Tumor perfusion increased and was explained by a temporary decrease in perfusion-limited acute hypoxia (Olive, 1994; Kim et al, 1994). Rapid reoxygenation has been believed to be due to acutely hypoxic cells and slow reoxygenation due to chronically hypoxic cells (Brown, 1979; Coleman, 1988). Reoxygenation in C3H mouse mammary carcinoma occurred about 12 hours after a large dose of irradiation and was reported as a slow reoxygenation of the chronic hypoxic population (Horsman et al, 1995).

Apoptosis

Our study found increased levels of apoptosis in all irradiated tumors. These changes in levels of apoptosis were not correlated to any other parameters in the study. We also demonstrated that cell loss due to apoptosis was significant early after radiation, since the apoptotic index was higher at 6 hours post-radiation than at 24 hours. It has been suggested that the elimination of tumor cells by radiation-induced apoptosis can result in tumor reoxygenation. This has been identified in animal models (Meyn et al, 1993; Milas et al, 1995; Rupnow et al, 1998). It was proposed that tumor shrinkage caused by apoptosis would relieve pressure on blood vessels and reduce the level of intermittent hypoxia. However, in the study with human squamous cell carcinoma of the cervix (Sheridan et al, 2000) no relationship was found between tumor shrinkage and the level of pretreatment apoptosis or the change in oxygenation during radiation therapy. Since it has been shown that a reduction in IFP can lead to increased tumor oxygenation (Milosevic et al, 1998), Sheridan et al. hypothesized that reoxygenation may be due to reduced IFP as a result of cell loss via apoptosis. This may relieve pressure on vessels, increase blood flow, and oxygen delivery, without affecting tumor size, which may correlate to our study.

Microvessel density

The change in vascular density did not have significance in the relation with any of tumor microenvironmental parameters, including oxygenation of tumors. MVD was increased in 6 and decreased in 8 tumors post-radiation. Previously reported results are not indicating the importance of the MVD changes in tumor reoxygenation. As shown by

Hittmair and coworkers (Hittmair et al, 1994) radiation therapy caused decreased cell density, while vascular density remained unchanged. The changes in oxygenation during radiation therapy of human breast cancer (Papova et al, 1982) and non-small cell lung cancer (Koh et al, 1995) coincided also with changes in cell density, but were not related to changes in MVD. Radiation-induced changes in the functionality of capillaries may occur (Brown, 1979; Dewhirst et al, 1990), leading to tumor perfusion changes independent of changes in vascular density (Lyng et al, 1999). Lyng et al. also reported no change in vascular density during radiation therapy in human uterine cervical cancer (Lyng et al, 2000).

Mechanisms of the changes in oxygenation

Changes in tumor oxygenation are reported to occur due to changes in the oxygen supply and/or oxygen consumption (Gulledge and Dewhirst, 1996). This study did not answer the question of the mechanisms of the tumor reoxygenation. Increased apoptosis was seen in the reoxygenated tumors, but also in the ones that did not have increased oxygen level after irradiation. If apoptosis played any role in the reoxygenation it was not the main cause for it. Microvessel density may not be associated with early change of oxygenation. The role of the microvascular perfusion is not clear. It could be possible that much earlier post-radiation perfusion increased and reoxygenated tumor tissue, which stayed oxygenated up to 24 hour point of our measurement. A possible explanation may be that the increased blood flow and oxygen supply are due to apoptosis and decreased IFP, but irradiation-damaged vessels are unable to deliver to the tumor tissue. It is important to understand that blood flow is blood movement through the vessels, and

perfusion is a delivery of the blood (with oxygen and nutrients) from the vessels to the mass of tissue in time. Thus the perfusion depends not only on blood flow, but also on the other factors such as resistance to flow through the vessel, pressure difference across its length, viscosity of the blood (Poiseuille's law for the flow of the liquids in tubes), vascular permeability, and pressure gradients between intra-vascular and extra-vascular spaces.

Some factors that we did not include in our study have been investigated by others. The occurrence of an inflammatory process has been reported to occur rapidly after irradiation, causing an increase in blood flow by vasorelaxation (el- Ghazaly et al, 1985; Moore et al, 2004). In their study Crockart et al. (2005) used an anti-inflammatory agent, and found a significant decrease in the level of tumor oxygenation 4 h after irradiation. They also found a significant decrease in the oxygen consumption rate, due to cell loss and reduced oxygen metabolism. 35 years ago, Kallman (1972) pointed out that decreased oxygen consumption by tumor cells allows for improved oxygenation even in the absence of increased perfusion. Decreased oxygen consumption was shown in the study by Olive et al. (1994), and suggested by many investigators as one of the factors playing role in the tumor reoxygenation (Secomb et al, 1995; Bussink et al, 2000). These are the parameters that have been investigated in relation to oxygen changes post-radiation: inflammation, oxygen consumption, and bioenergetic and metabolic status in tumor (distribution of ATP, lactate, and glucose (Thews et al, 1999)). They also may play a role in the changes in tumor microenvironment, and could be considered for some future multiparameter reoxygenation studies.

For the improvement of this study I would propose a better patients selection in regard to tumor location. We have learned that thoracic wall tumors were difficult to analyze by DCE-MRI. There was large movement of the thorax due to respiration, and consequently motion artifacts. For microvascular perfusion estimates I would choose DCE techniques. Even though there is now available artifact rejection technology from the Oxford Optronix, whose laser Doppler flowmetry equipment we use, my experience with constantly moving probes does not promise much more reliable LDF results. Since changes in MVD did not influence oxygenation status in tumors 24 hours post-radiation, as well as apoptosis was not related to changes in oxygenation, evaluation of these parameters could be omitted in eventual future study. I would more carefully evaluate a standardization of repeated procedures: precise localization and guidance of probe placements. Sampling in the same tumor region is a very important factor to overcome tumor heterogeneity since difference in the measurements may occur between very small intratumoral distances. I would like to include non-invasive techniques for assessment of tumor pH and tumor bioenergetic status by magnetic resonance spectroscopy (^{31}P -MRS, phosphorus MRS).

It is important to incorporate a combination of parameters to adequately describe the mechanisms underlying the changes in tumor after irradiation, since all parameters of the tumor microenvironment interact very closely and the change in one of them influences many other in this very complex system.

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PART II

MUTAGENIC EFFECT OF HYPOXIA ON A_L HYBRID CELLS

CHAPTER 3

GENETIC INSTABILITY AND THE TUMOR MICROENVIRONMENT

Genetic Instability

Genetic instability is a characteristic feature of malignancy. Over the past two decades investigations have identified numerous genetic alterations in the genes that control tumor cells growth. Tumor progression has been correlated with genetic instability (Nowell, 1976; Loeb, 1991). Specific gene defects that lead to genomic instability include the DNA mismatch repair genes associated with hereditary colon cancer (Bronner et al, 1994), and the p53 gene, which is inactivated more frequently than any other gene in a wide range of human cancers (Greenblatt et al, 1994). Mutations in critical genes contribute to genetic instability through alterations in DNA repair and alterations in the cell cycle. Environmental factors like carcinogen exposure also play role in DNA damage.

In addition to these endogenous and environmental factors, tumor microenvironment itself is shown to be mutagenic leading to tumor progression and evolution of malignant phenotype (Reynolds et al, 1996). The tumor microenvironment is characterized by regions of hypoxia, nutrient deprivation and acidity (Moulder and Rockwell, 1987; Rockwell, 1992). Since this specific microenvironment influences tumor

metabolism and physiology, it may also cause increased spontaneous damage to DNA or inhibit DNA repair processes needed to maintain their genomic integrity (Yuan and Glazer, 1998).

Hypoxia

Hypoxia, the most extensively studied of microenvironmental factors, may lead to significant genomic alterations, and evidence exists suggesting that tumor hypoxia plays a key role in the development of aggressive tumor phenotypes and genetic instability. Tumor hypoxia is associated with increased DNA damage and impairments in DNA repair pathways. Several studies using both reporter genes and endogenous loci have demonstrated increased mutation rates in cells grown in tumors relative to those in identical cells grown in cultures (Reynolds et al, 1996; Paquette and Little, 1994; Li et al, 2001). One of the first experiments examining the role of tumor microenvironment in genetic instability used the mouse cell line carrying a chromosomally based lambda phage shuttle vector that was implanted subcutaneously into the flanks of nude mice to generate tumors. At the same time, an equal number of cells from the same cell line (LN12) was grown *in vitro* under standard culture conditions. A five-fold increase in the mutation frequency in cells grown in tumors compared to the same cells grown in culture was found (Reynolds et al, 1996). Several other studies also provided evidence of increased mutagenesis following growth of cells in solid tumors (Li et al, 2001). The mutation frequency in the hypoxanthine guanine phosphoribosyl transferase (HGPRT) gene in tumors was also reported to be higher than that found in cultured cells (Wilkinson et al, 1995).

Studies trying to characterize hypoxia-induced DNA damage have shown that hypoxia alone does not induce double-strand breaks (DSBs) (Hammond, 2002). It was shown that reoxygenation, on the other hand, induces significant DNA damage with DSBs mediated by ROS production during post-hypoxia reoxygenation (Hammond et al, 2003). Based on the studies of reperfusion injury, DNA damage is attributed to production of reactive oxygen species (ROS) and increased levels of antioxidant enzyme, superoxide dismutase (Welbourn et al, 1991). For example, oxidative injury may generate excessive levels of 8-oxoguanine, which miscode for A, leading to C: G to A: T transversions (Cheng et al, 1992). Investigations of the effect of hypoxia on cell cycle provided evidence that hypoxia induces G1-phase arrest (Graeber et al, 1994; Gardner et al, 2001), and severe hypoxia (approximately 0.02% O₂) results in an S-phase arrest which is reversible upon reoxygenation (Hammond et al, 2002).

Under low oxygen conditions DNA synthesis is inhibited, due to the suppression of initiation (Probst et al, 1988). Interruption of DNA synthesis is associated with single-strand breaks and double-strand breaks. Since double-strand breaks are not seen after exposure to hypoxia, it seems that hypoxia may only suppress initiation of replication, and not directly cause extensive DNA damage (Bindra and Glazer, 2005). Hypoxia may damage DNA indirectly by inducing endonucleases leading to DNA strand breakage (Russo et al, 1995). Induction of aberrant DNA synthesis following hypoxia-reoxygenation results in DNA overreplication and gene amplification. Many studies have reported DNA overreplication after exposure to hypoxia (Rice et al, 1985, 1986, 1987), and its association with tumor metastasis (Young et al, 1988; Young and Hill, 1990). Gene amplification has been reported to be the most frequent genetic alteration in cancer

cells. Being associated with the overexpression of many oncogenes, this phenomenon is linked to tumor progression (Brison, 1993; Teicher, 1994).

Cells with overreplicated DNA were shown to acquire drug resistance. In one of early investigations by Rice et al. (Rice et al, 1986), exposure of Chinese hamster ovary (CHO) cells to hypoxia followed by recovery in the presence of oxygen led to increased methotrexate resistance resulting from amplification of the dihydrofolate reductase gene. In subsequent studies, it was found that gene amplification caused adriamycin and doxorubicin resistance observed after exposure to hypoxia in several cell lines (Rice et al, 1987; Luk et al, 1990). In these studies hypoxic exposure was followed by a reoxygenation period, and gene amplification has been observed during reoxygenation. Besides these studies that were focusing on large chromosomal rearrangements, there are studies done to detect small-scale mutations that may be induced by hypoxia. It was demonstrated that transient hypoxia resulted in increased mutation frequencies compared to normoxic controls (Reynolds et al, 1996). Furthermore, multiple hypoxia-reoxygenation exposures resulted in even greater mutation frequency.

Low pH and nutrient deprivation

Even though less investigated, other microenvironmental factors can alter cell metabolism and potentially contribute to genomic instability. Low pH has been shown to alter structure and function of proteins involved in DNA replication such as helicases and polymerases (Eckert and Kunkel, 1993a, 1993b). It has been demonstrated that both nutrient deprivation and acidosis can enhance metastatic potential of murine tumor cells (Cuvier et al, 1997; Schlappack et al, 1991). When cells were exposed to pH 6.5 or

starved for glucose followed by recovery in normal growth medium, some cells were found with overreplicated DNA, similar to the effect of hypoxia. Exposure to acidosis even led to a small increase in methotrexate resistance in a murine tumor cell line (Schlappack et al, 1991).

It was shown that serum deprivation can induce increase in mutations. The incubation of CHO cells in serum concentrations below 0.25% resulted in an almost five-fold increase in the mutation rate, and was also associated with a rise in intracellular oxidants (Goncharova et al, 1996). When the low serum was supplemented with antioxidants, the mutation rate was reduced in a dose-dependent manner, suggesting that ROS may be involved in induction of mutagenesis. Serum starvation was associated with increased genetic instability in 4T1 cells, as well (Li et al, 2001). According to the work done in this area, it has been demonstrated that other factors of tumor microenvironment, in addition to hypoxia, may play a role in inducing DNA damage and causing genetic instability.

Alterations in DNA repair pathways under hypoxia

The characteristic tumor microenvironment has been shown to contribute to genetic instability. Intratumoral hypoxia induces alterations in numerous physiological processes, including altered glucose metabolism, up-regulated angiogenesis, increased invasive capacity, and deregulation of apoptosis (Subarsky and Hill, 2003). All the specific changes in cell physiology may lead to conditions that cause either increased damage to DNA or inhibition of DNA repair processes. Decrease in expression of DNA repair genes is a possible mechanism for this effect. Specifically, it has been

demonstrated that hypoxia leads to functional decreases in both the nucleotide excision repair (NER) and mismatch repair (MMR) pathways.

Using UV-induced damage Yuan et al. examined the effects of hypoxia and low pH on the nucleotide excision repair (NER) pathway (Yuan et al, 2000). They reported that exposure of irradiated cells to hypoxia and pH 6.5 exhibited a decrease in DNA repair capacity.

DNA mismatches arise from errors in replication and repair and from intermediates produced during recombinational processes (Modrich and Lahue, 1996; Kolodner, 1996). Those genetic aberrations are repaired via mismatch repair pathway (MMR). MMR is carried out by a series of proteins, including MSH2, MSH3, MSH6, and MLH1 and PMS2 (Kolodner, 1996). The expression of MMR proteins was examined after exposure to hypoxia. It was found that severe hypoxia (0.01%O₂) specifically down-regulates the expression of the MLH1 gene at the level of transcription (at the mRNA level) (Mihaylova et al, 2003). PMS2 protein levels were reduced under hypoxia, probably due to instability of PMS2 in the absence of its heterodimer partner, MLH1 (Chang et al, 2000). It has been proposed that metabolic changes in hypoxic cells create sub-optimal conditions for the activity of some DNA repair enzymes (Bindra et al, 2005), and some studies have revealed that ROS and oxidative stress can inactivate the MMR system (Kondo et al, 2001; Chang et al, 2002). It has also been reported that hypoxia and accompanying low pH enrich for MMR-deficient cells (Hardman et al, 2001).

Considering the complex gene expression changes observed under hypoxia, it has been investigated whether alterations in the expression of other DNA repair genes could also play role in hypoxia-induced genetic instability. It has been reported that the

expression of RAD51, a critical mediator of homologous recombination (HR) in mammalian cells, is specifically down-regulated by hypoxia at the mRNA level. Decreased RAD51 protein expression under hypoxia was observed in numerous cell lines, and more interestingly this decrease persisted even during post-hypoxic phase (Bindra et al, 2004). This is especially relevant to solid tumors, which experience fluctuating blood perfusion that results in temporally and spatially varying oxygen tensions.

These data provide evidence that genetic instability may arise from deregulated DNA repair pathways as well as from increased DNA damage.

Evaluating mechanisms underlying the genetic instability

Proposing different experimental protocols and various culture conditions was used in evaluating mechanisms underlying the genetic instability in developing tumors. However, *in vitro* conditions do not exactly mimic the tumor's very complex microenvironment. Even more, different microenvironmental factors may interact with each other synergistically, producing a bigger effect together than each of them alone. Rotin et al. reported that cellular ATP, energy change and cell viability were reduced after 6 hour exposure to hypoxia at pH 6.0. None of them were influenced by hypoxia or acidosis alone (Rotin et al, 1986). Reynolds et al. investigated tumor hypoxia-induced mutations and found that single exposure of the cells to hypoxia increased mutation frequency 3.4 fold above that for the untreated cells. Cells exposed multiple times to hypoxia showed even higher mutation frequencies, indicating cumulative dose-response effect (Reynolds et al, 1996). This is pointing to conclusion that transient exposures to

low oxygen levels found within tumors are mutagenic. While investigating whether tumor microenvironment could influence cellular repair of DNA damage, Yuan et al. noted that they saw only a small decrease in DNA mismatch repair in cells treated with hypoxia alone. However, when cells were exposed to a combination of hypoxia and acidosis, they observed large differences (Yuan et al, 2000), which was in accordance with other studies reporting a synergistic effect of low oxygen and low pH (Rotin et al, 1986; Boyer and Tannock, 1992). The frequency of mutations in cells grown in a tumor was found to be higher than in identical cells grown in culture for an equivalent period of time (Graeber et al, 1994; Reynolds et al, 1996). A different pattern of mutation was also seen in Reynolds experiment, with significantly more deletions and transversions in tumors, while mutations in cultured cells were point mutations, implicating that strand breaks must be produced by tumor microenvironment.

Tumor microenvironment can contribute to mutations in several ways. A summary of the pathways by which hypoxia, specifically, induces genetic instability is shown in Figure 3.1 (adopted from Bindra and Glazer, 2005)

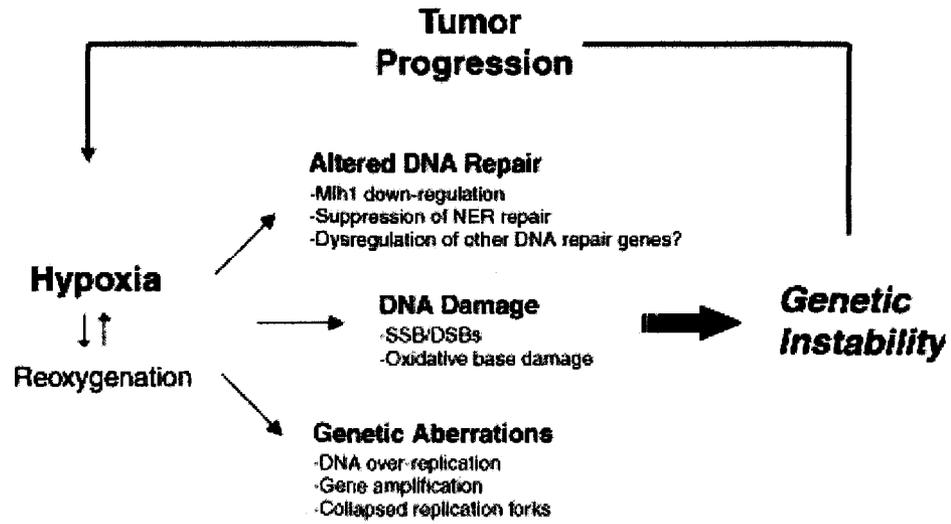


Figure 3.1 Hypoxia, genetic instability and tumor progression. Abbreviations: NER, nucleotide excision repair; SSB/DSBs, Single-strand breaks/double-strand breaks.

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CHAPTER 4

DOES TUMOR HYPOXIA IMPACT MUTAGENESIS?

ABSTRACT

The impact of tumor hypoxia on local tumor control has long been a concern for solid tumors treated with radiation therapy. More recent work has implied that hypoxia of the primary tumor may also be associated with metastatic spread, perhaps by contributing to genetic instability. It has been proposed that tumor microenvironment, with fluctuating hypoxia, low pH and nutrient deprivation may be responsible for diminished DNA repair and increased mutagenesis. I hypothesized that hypoxia alone could lead to genomic alterations. To investigate the hypothesis I used the A_L mutation assay. A_L cells are human-hamster hybrid cells containing a standard set of CHO-K1 chromosomes and single copy of human chromosome 11. Genetic markers on chromosome 11 have been mapped, including the CD59 gene that encodes for the cell surface antigen, CD59. Wild type CD59⁺ cells are killed when the culture is treated with a monoclonal antibody to the CD59 antigen and rabbit complement. Mutant CD59⁻ cells survive and form colonies.

Since the human chromosome is not essential for the viability of the hybrid cell, except for the small segment on the tip of the short arm, mutations ranging from point mutations

to loss of almost the whole chromosome 11 can be detected. We exposed A_L cells to different hypoxic conditions, isolated and cloned CD59⁻ mutants and performed PCR analysis. Only severe hypoxia caused mutations in this system. Levels of oxygen below 0.1% or less than 0.63mm Hg induced mutations in A_L cells. Qualitative analysis indicated that they were possibly point mutations and/or very small deletions on chromosome 11. Cells were also labeled with monoclonal antibodies against the CD59 surface antigen and analyzed by flow cytometry (FCM). Single mutant cells were sorted from the mutant peak. The resulting clonal populations were analyzed using the same methods to determine if mutated cells were truly negative for CD59. The purified DNA from PCR products of four exons, from both types of mutation assays, was sequenced to check for the characteristics of the hypoxia-induced mutants. Sequencing did not detect any changes in the CD59 gene.

INTRODUCTION

The tumor microenvironment is very specific and differs from that of a normal tissue. As a tumor grows, it develops a chaotic and irregular vascular network and insufficient lymphatic system. This unique physiology results in regions of hypoxia, low pH, high lactate levels, nutrient deprivation and interstitial hypertension among solid tumors (Yuan et al, 2000; Vaupel, 2004).

Genetic instability is a commonly observed aspect of tumors (Yuan and Glazer, 1998). The mechanisms underlying genetic instability have been investigated and an important role was attributed to genetic defects influencing cell cycle regulation and

DNA repair, including p53 mutations, defects in DNA mismatch repair (MMR) genes and genes associated with the nucleotide excision repair (NER) pathway (Mihaylova et al, 2003). In addition to genetic factors, it has been proposed that tumor microenvironment itself may be mutagenic and lead to genomic alterations. The evidence has been provided for increased mutation frequency in cells grown in tumors compared to identical cells grown in culture (Reynolds et al, 1996; Wilkinson et al, 1995). This is supported by data demonstrating that exposure of cells to conditions observed in tumors produces chromosomal changes and increases the frequency of drug resistance (Yuan et al, 2000; Reynolds et al, 1996; Rice et al, 1987). Work on experimental models has shown that exposure to hypoxia, glucose deprivation and acidosis have an effect on invasiveness of murine tumor cells (Cuvier et al, 1997; Dewhirst et al, 1994). The association of tumor hypoxia with enhanced metastatic potential of human soft tissue sarcomas, cervix carcinomas and carcinomas of the head and neck (Brizel et al, 1996, 2001; Hockel et al, 1996, 1998; Rofstad et al, 2000) has been reported. These studies suggest an association with modulating gene transcription. Hypoxia, either alone or followed by reoxygenation, has been associated with various DNA lesions, including single-strand breaks, inhibition of replication initiation and gene amplification (Hammond et al, 2002, 2003; Rice et al, 1986). The genetic changes induced by hypoxia may play an important role in the development of genomic instability and more aggressive phenotypes (Koong et al, 2000; Denko et al, 2000, 2003).

Several studies proposed that tumor microenvironment, with fluctuating and chronic hypoxia, low pH and nutrient deprivation, may be responsible for diminished DNA repair and increased mutagenesis (Yuan et al, 2000; Mihaylova et al, 2003; Reynolds et al,

1996; Kondo et al, 2001). It is not known what type of hypoxia is more important for treatment outcome or what the significance of chronic and acute hypoxia is in the development of metastatic disease. I propose that acute hypoxia may play a more significant role in the tumor microenvironment and that acute hypoxia alone can cause genetic instability. Because acute hypoxia is the result of fluctuations in blood flow and not at the limits of oxygen diffusion away from blood vessels like chronic hypoxia, it is supposed that cells exposed to acute hypoxia have higher energy status than chronically hypoxic cells (Fenton et al, 1995; Kim et al, 1993). They are also less likely to be exposed to acidic pH and more likely to survive the complex process of metastasis (Cairns et al, 2003).

To investigate the role of tumor hypoxia alone in the induction of mutagenesis, I used the A_L cell mutation assay. The human-hamster hybrid A_L cell line was developed by Puck et al. (Puck et al, 1971) by fusion of human fibroblasts and the gly⁻A (glycine deficient) mutant of the Chinese hamster ovary cells. The hybrid cells contain a standard set of 20 CHO-K1 chromosomes (Kao and Puck, 1968; Kraemer et al, 2000) and a single copy of un-rearranged human chromosome 11, which is not necessary for cell reproduction (Waldren et al, 1979, 1986, 1999). The principal markers of mutation assay are the cell surface antigen CD59 and the CD59, gene that encodes it, located at 11p13.5, (Kraemer et al, 2001). Wild type A_L cells express a glycosylphosphatidylinositol (GPI) bound human CD59 surface antigen and are lysed quantitatively by anti-CD59 monoclonal antibody E7.1 in the presence of rabbit serum complement. Cells that have lost expression of the CD59 antigen are not killed and grow into colonies. Since human chromosome 11 codes for genes that are not essential for the survival of the cell,

mutations ranging from point mutations and small deletions to loss of almost all of chromosome 11 can be detected using this mutation assay (Waldren et al, 1999, 2004; Kraemer et al, 2001; Hei et al, 1988; Zhu et al, 1996).

A_L cells were exposed to different levels of oxygenation and for varying durations to determine if hypoxia alone (without changing nutrients or pH of the medium), could cause mutations.

MATERIALS AND METHODS

Cell culture, media and reagents

The A_L hybrid cell line has been used in mutation analysis and described in detail previously (Waldren et al, 1979, 1986, 1999, 2004; Kraemer et al, 2001; Hei et al, 1988; Zhu et al, 1996). The A_L cells contain the standard set of CHO-K1 chromosomes and a single copy of human chromosome 11. Hybrid A_LN cells were constructed by transfecting the pSV2neo plasmid into human chromosome 11, but no hamster chromosome, to give the A_LN cells the resistance to killing by neomycin (G418 sulfate, purchased from Sigma-Aldrich, St. Louis, MO). Cells grown in medium containing 0.8mg/ml neomycin are killed if they do not express the pSV2neo vector to select against cells that have lost human chromosome 11 (Kraemer et al, 2001; McGuinness et al, 1995). Cells were cultivated in Ham's F-12 medium supplemented with 3% fetal calf serum and 4% newborn calf serum (Hyclone, Logan, UT), HEPES buffer (Sigma-Aldrich, St. Louis, MO) and penicillin/streptomycin 10,000 IU/ml and 10,000 µl/ml (Mediatech Inc. Cellgro, Hendron, VA). Rabbit serum complement was from Covance

Research Product Inc., Denver, PA., human serum type AB from Sigma, St Louis, MO, and monoclonal antibody E7.1 was provided from Dr. Waldren's lab at Colorado State University. E7.1 was prepared as described (Waldren et al, 1979, 1999). Antiserum from sheep immunized with human erythrocytes was used as a source of antibodies against CD59 antigen.

The A_L mutation assay: principle and protocol

Mutation was measured at the CD59 locus of A_L human-hamster hybrid cells. Mutation was detected as loss of expression of the CD59 cell surface antigen that is encoded by the CD59 gene at 11p13.5. Wild-type cells with the antigen are lysed by monoclonal antibody in the presence of complement. Cells that do not express this antigen are not recognized by the E7.1 antibody and survive to form colonies. Colonies grown after exposure to complement and antibody were used to calculate the number of mutants in surviving cells. Cells were exposed to reduced oxygen levels as a potential mutagen.

A Forma Scientific Water Jacketed incubator with thermal, CO₂, and O₂ control was used to obtain 2.5% and 1% O₂ environments. Cells were maintained in these conditions for 4 or 7 days. An incubator insert chamber [C-274 chamber with PRO-OX Model 110 and PRO-CO₂ (BioSpherix, Redfield, NY)] was used to obtain O₂ levels of 0.1%. To lower oxygen further, an anaerobic chamber BBL™ GasPak™ 100 Jar System, with gas generator envelopes (Fischer Scientific, Houston, TX) was used. This system provided oxygen levels between 0% and 0.1%. Cells in the <0.1% group were exposed for 24 hours. Duration was based on achieving 50% cell survival. Enough cells were plated in

enriched F12 medium to give a surviving population of more than 10^5 cells after exposure to hypoxia (mutagen) (Figure 4.1). The cells were then sub-cultured for 10 days to let them recover from the temporary growth lag and divide as described (Waldren et al, 1979, 1999). Cells were then challenged with 2% rabbit serum as a complement (Covance Research Products Inc., Denver, PA), and 0.5% E7.1, a specific monoclonal antibody against the CD59 antigenic marker (Figure 4.2). Cells with CD59 surface antigens do not survive the complement challenge. Surviving cells formed colonies which were counted as mutant cells. The mutant yield was adjusted for plating efficiency and background mutations.

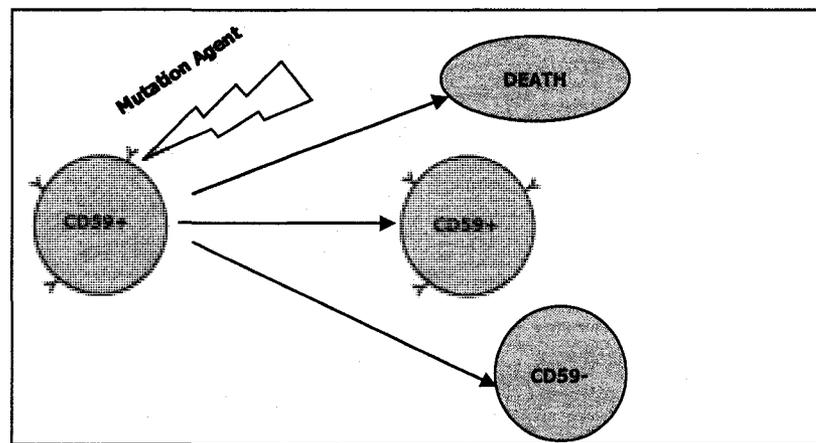


Figure 4.1. Treatment of A_L cells with a mutagen results in survival with wild type CD59, survival with mutated CD59, or death.

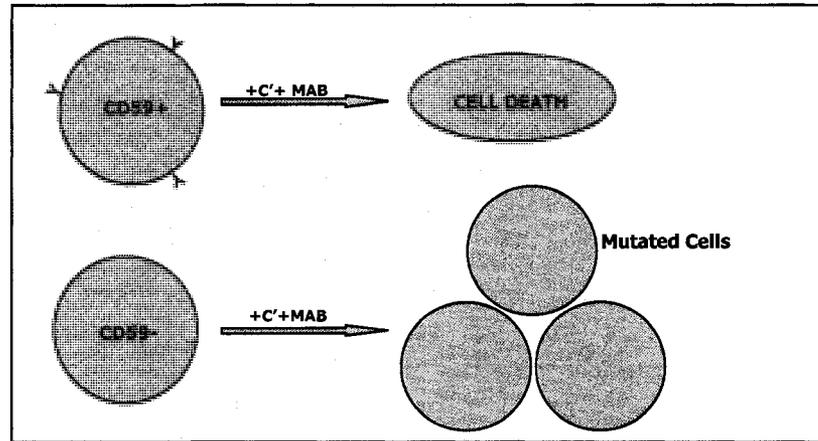


Figure 4.2. Selection of CD59 mutant A_L cells after treatment with CD59 Mab and Rabbit serum; wild type cells are killed, CD59 mutants grow into colonies.

Determination of hypoxic conditions: Survival Curves and A_L mutation assay

A_L cells were first exposed to an environment of 2.5% O_2 . 2.5% is less than in the ambient air; however 2.5% or (15.75 mm Hg) O_2 is not considered hypoxic and we used these data for the background mutations level (Figure 4.3). To further decrease oxygen we used the PRO-OX system which allowed us to achieve O_2 concentrations as low as 0.1% (0.63 mm Hg). Cells were exposed to 1%, 0.2% and 0.1% O_2 for 4 or 7 days. The anaerobic chamber was used to obtain severe hypoxia below 0.1% O_2 (less than 0.63 mm Hg). 2×10^5 cells were plated and placed in the chamber for 1, 3, 24 or 43 hours and a survival curve was constructed to define the optimal time for exposure to hypoxic conditions (Figure 4.4). The subsequent experiment, 24 hours exposure time was used so that at least 10^5 cells survived for challenge with rabbit serum complement and antibody E7.1. To reduce any nonspecific toxicity of the complement, 0.1% human serum was added to the mixture. 7 days after “challenge”, colonies were counted as mutated cells.

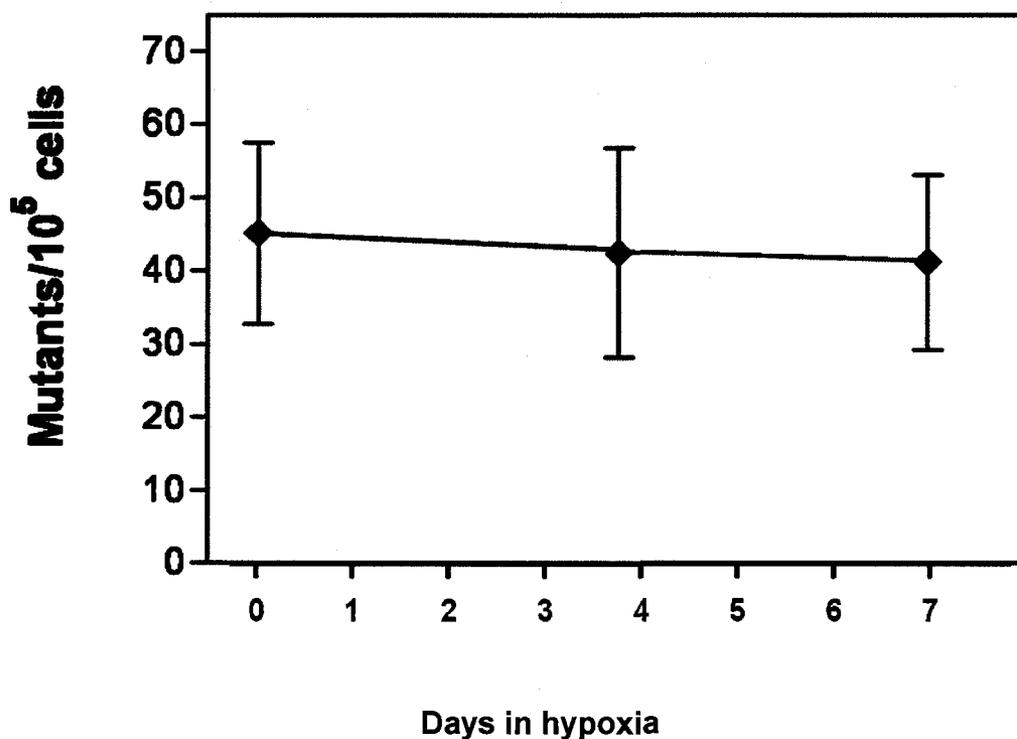


Figure 4.3. Mutant yield for cells exposed to 2.5 % O₂ (15.75 mm Hg). Control cells were grown in normoxic conditions. Presented as mean ± SD for mutants per 10⁵ cells without adjusting for background mutations.

The number of mutated cells per 10⁵ surviving cells (mutant yield) is the average number of colonies on the plates divided by the plating efficiency (PE) of cells exposed to complement without antiserum, so it is corrected for any nonspecific killing due to complement alone (Waldren et al, 1979; McGuinness et al, 1995). The background mutant yield (adjusted number of colonies grown in untreated plates) was subtracted to give the final mutant yield. Colonies were picked and expanded for PCR analysis.

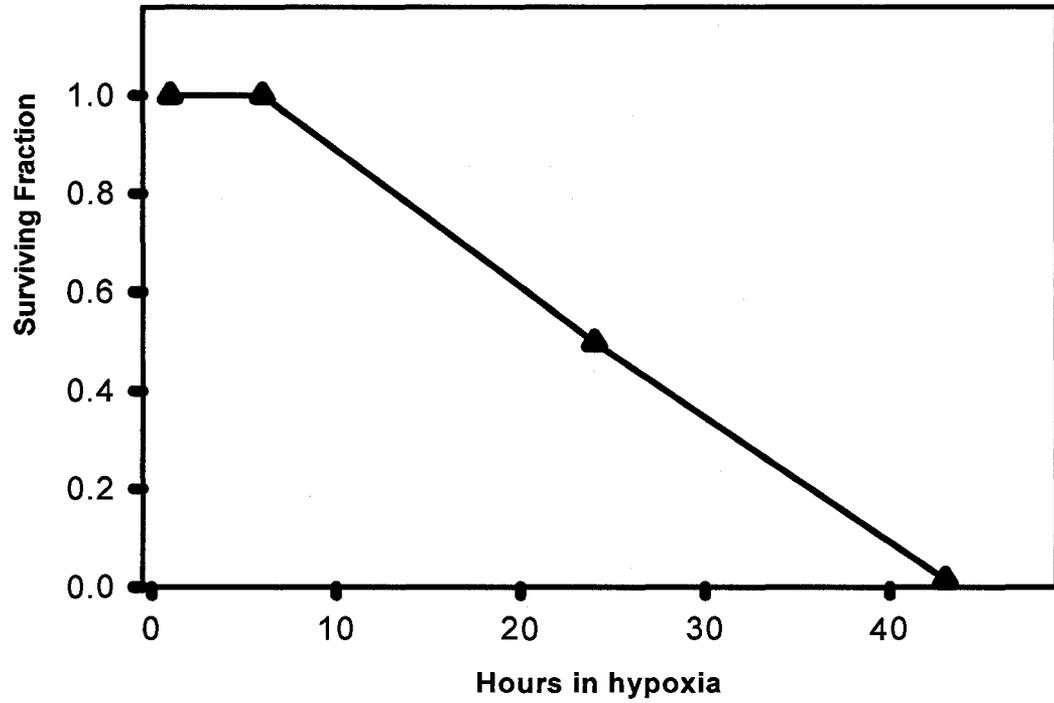


Figure 4.4. Survival curve for CHO AL cells grown in less than 0.63 mmHg (<0.1% O₂).

PCR and Sequencing Analysis

The mutated cells were cloned and DNA was extracted using DNeasy Tissue Kit (Qiagen, Valencia, CA). DNA concentrations were diluted to 100 µg/ml and the presence or absence of five loci on chromosome 11 was determined by PCR. Five DNA marker genes on chromosome 11 (RAS at 11p15.5, LDHA at 11p15.4, Catalase- CAT at 11p13, Centromere and Apolipoprotein A-1- APO at 11q23-24) were chosen because of their positions relative to the CD59 gene (Figure 4.5), and the availability of PCR primers for the coding regions of these genes (Zhou et al, 1999; Hei et al, 1998).

The primers, synthesized by Macromolecular Resources (Fort Collins, CO) were:

RAS: Forward GAC GGA ATA TAA GCT GGT GG
 Reverse TGG ATG GTC AGC GCA CTC TT

LDHA: Forward ATA CAC TTT GGG GGA TCC AAA AGG A
 Reverse AAA AAA TGT TGG ACT AGG CAT GTT C

CAT: Forward TTA GCG TTC ATC CGT GTA ACC
 Reverse TCC AAT CAT CCG TCA AAA CA

CENTROMERE: Forward AAT TTC TTC TCC ACC CAC CC
 Reverse TTG CAT GCC ATT GTG GAG

APO: Forward GCT TCA AGG TCA GCT TCC TG
 Reverse GGA AAC GTT TAT TCT GAG CAC C

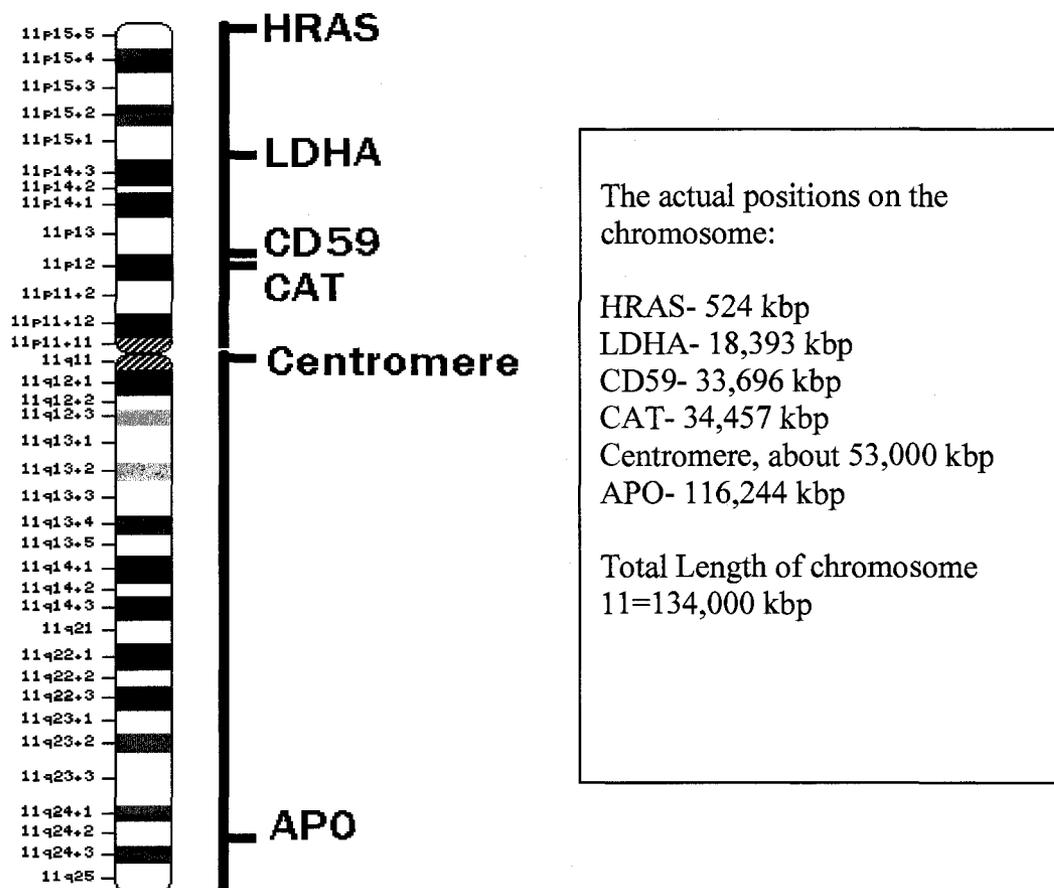


Figure 4.5. Diagram of human chromosome 11, showing the CD59 gene and the relative position of other markers used in the PCR analysis for determination of the extent of the mutations. The two nearest markers to CD59 are separated by about 16 Mbp.

To determine the presence or absence of the four exons of the CD59 gene (Figure 4.6), PCR was done using the following primers obtained from Macromolecular Resources as previously described (Waldren et al, 1999).

STRUCTURE OF CD59

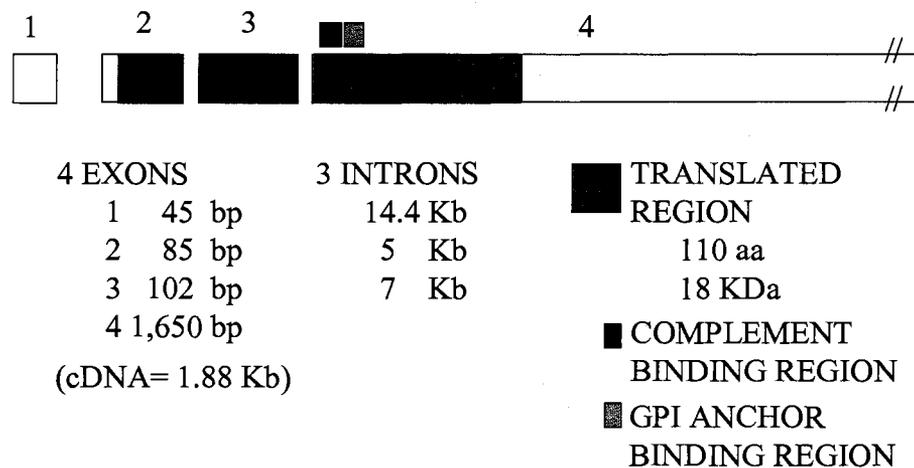


FIGURE 4.6. Structure of the CD59 gene, exons, introns and their sizes in base pairs (bp) and kilo base pairs (Kb). Binding site for complement and GPI anchor are encoded by exon 4 (Courtesy of Diane Vannais). Exon 2 translated region 67 bp, untranslated 18 bp; exon 4 translated region 215 bp, untranslated 1435 (Petranka et al, 1992).

Exon 1: Forward CTG GAG CGA AAG ATT GCG

Reverse: TTC GGG CCT TCT TAC CTG

Exon 2: Forward TTG AGA CAA CCA GCA GTC

Reverse TAA GAA GGG AGT TCA TGG

Exon 3: Forward GGA AGT ATA CCA CAA GTT GC

Reverse GCC TAA TGA GGA TTA CAG TG

Exon 4: Forward ACA AGT GTA TAA CAA GTG TGG

Reverse TCC CTG CAA ACA GGA CTG

Extracted DNA was diluted 1:50 to measure its concentration by spectrophotometry. All samples were diluted to 100 ng/ μ l using the formula $C_1V_1 = C_2V_2$ (concentration X volume). The PCR reactions of 50 μ l were set up using 100 ng of DNA, 5 μ l of each primer (10 μ M) and 25 μ l of Taq PCR Master Mix Kit (Quiagen, Valencia, CA). $MgCl_2$ concentration and annealing temperature were adjusted according to Table 4.1.

Amplifications were performed in a MultiBlock PCR System (MBS) Thermal Cycler (Hybaid, Franklin, MA). The thermal protocol was: 95° C, 5 min, each of 30 PCR cycles consisted of denaturation at 94° C for 45 sec, annealing temperature (given in Table 1) for 45 sec, and extension at 72° C for 45 sec. After the last cycle, the samples were incubated at 72° C for an additional 20 min. Samples were analyzed using electrophoresis on 2% agarose gels in TAE and stained with ethidium bromide (0.5 μ l/ml). The gels were scanned on a Typhoon 9410 imager (Amersham Biosciences Corp., Piscataway, NJ).

The post-PCR reaction products of four exons of CD59 were purified using ExoSAP-IT (USB Corporation, Cleveland, OH) adding 1 μ l of cleaning product to the 5 μ l of reaction product directly following PCR. After incubation at 37° C for 15 min to degrade remaining primers and nucleotides, the mixture was incubated at 80° C for 15 min to inactivate ExoSAP-IT. DNA sequences were analyzed in both forward and reverse directions using an ABI3100 Genetic Analyzer (Applied Biosystems, Foster City, CA).

The sequenced exon fragments were compared with those in the Genebank database by BLAST analysis.

Table 4.1. PCR program adjustments for amplification of different gene markers.

Gene Marker	Annealing Temp (°C)	MgCl ₂ (mM)	Product Size (bp)
RAS	55	1.5	63
LDH A	57	3	407
CAT	65	4.5	207
CENTROMERE	62.5	3	130
APO	53	1.5	109
Exon 1	53.5	1.5	87
Exon 2	55	3.5	205
Exon 3	55	3.5	350
Exon 4	55	3.5	401

For DNA sequencing analysis the following programs and web sites were used:

1. For the DNA sequencing chromatogram viewing: FinchTV (Figure 4.7)

<http://www.geospiza.com/finchtv>

2. For the DNA assembly: The CAP3 Sequence Assembly Program

<http://pbil.univ-lyon1.fr/cap3php>

3. DNA multiple alignments of the nucleotide sequences: ClustalW

<http://www.ebi.ac.uk/clustalw/>

Output format: aln wo/numbers

Output order: input

and was done with manual adjustment.

4. DNA sequence editing: Boxshade

http://www.ch.embnet.org/software/BOX_form.html

Output format: RTF_new

Consensus Line: consensus line with letters

Input sequence format: ALN

And for editing also used BioEdit- Biological sequence alignment editor

<http://www.mbio.ncsu.edu/BioEdit/bioedit.html>

Exon 4 Control Sequence

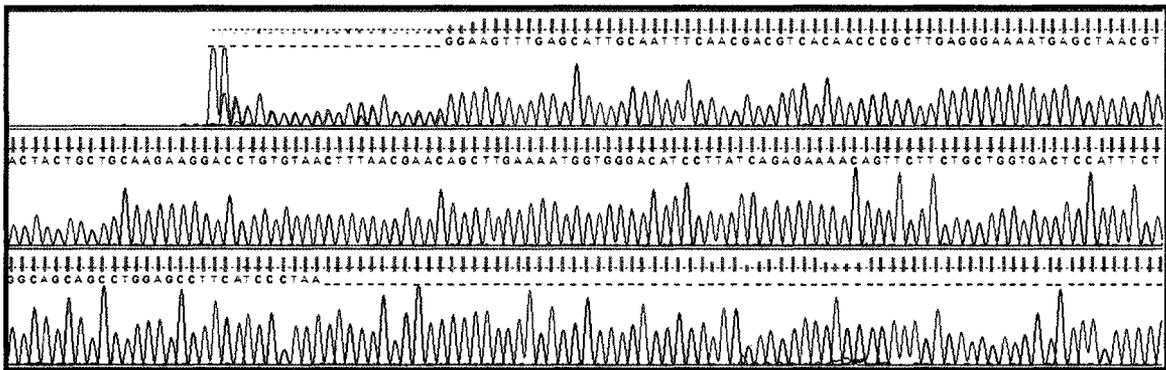


Figure 4.7. Exon 4 of CD59 gene, control sequence from DNA sample depicted on Finch TV, allowing the analysis and comparison of the whole sequence in one view.

Flow Cytometry

Flow cytometric quantification of mutant fractions was done using a CyAn flow cytometer (Dako, Fort Collins, CO) using 488 nm excitation and a 545 nm dichroic long pass and 575 nm band pass filter. 4×10^5 A_L cells were plated in six 15 mm Petri dishes,

3 control and 3 for treatment. Cells were placed in the anaerobic chamber for 24 hours for hypoxia treatment as described earlier and then transferred to normoxic conditions in a humidified incubator at 37 ° C. One day after hypoxia treatment marked as day 2, cells were passed (1.5×10^5 control cells passed to T75 flasks, 3×10^5 treated cells passed to T75 flask). On day 6, 1.5×10^5 cells were passed for control and treatment. On day 9, 2×10^5 cells were passed. On day 12, 1×10^6 cells were isolated from each of the three controls and treatment replicates. Cells were centrifuged and the pellet was suspended in 1 ml FACS buffer. After the cells were centrifuged a second time, they were suspended in 50 μ l of CD59 specific monoclonal antibody conjugated to Phycoerythrin (PE) (1:40 dilution in FACS buffer). Cells were then incubated in a humidified 37° C environment containing 5% CO₂ for 30 minutes.

One ml cold FACS was then added to the cells and they were again centrifuged. Cells were finally suspended in 0.5 ml cold FACS and transferred to flow cytometry sample tubes on ice. 1×10^5 cells from each sample were analyzed on the flow cytometer.

Within the PE histogram, the mutant region was defined as cells with fluorescence intensity less than 1% of the mean fluorescence intensity of the positive control peak (CD59⁺) on a log scale (Figure 4.8).

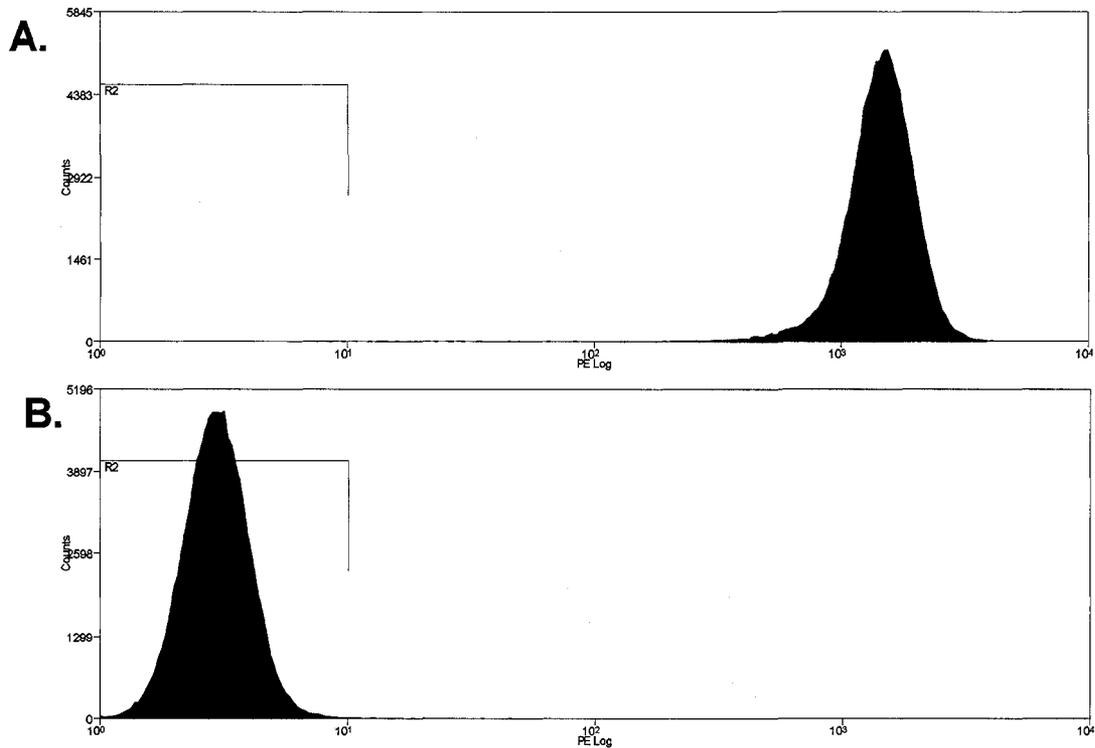


Figure 4.8. A. A_L CD59 positive stock cells. B. CD59 negative cells gated within a region set as 1% of the mean of the positive peak.

Mutant fractions were calculated as mutants per 1×10^5 cells by subtracting background mutants (control cells) from mutants of the hypoxia treated cells.

Single cells were sorted from the mutant region of hypoxia treated cells on day 12 after treatment using a Dako MoFlo cell sorter (same cell preparation as the flow cytometry analysis). These cells were allowed to form colonies in 96 well plates. After 21 days clones were transferred to T25 plates and expanded. 1×10^6 cells were isolated and run on the flow cytometer using the previous procedure to determine if cells sorted from the mutant region were truly negative for CD59.

RESULTS

Survival Curves

The cells were exposed to different pO_2 and for various durations to determine the optimum time of exposure for each hypoxia level. As described earlier, I determined the exposure time that gave 50% survival, which left enough surviving cells (more than 10^5) to perform the challenge with complement and antibody. Figure 4.4. and Figure 4.9. are examples of the survival curves constructed for two experimental conditions. They show the optimum time of exposure to 0.1% pO_2 is four days, while for the severe hypoxia below 0.1% O_2 optimum it is 24 hours.

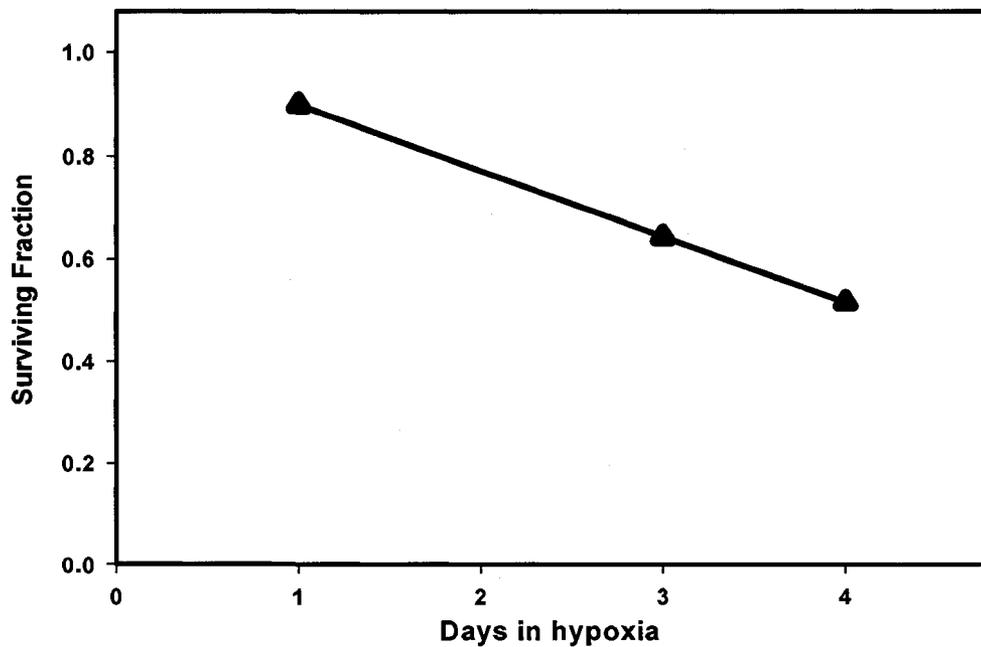


Figure 4.9. Survival curve for A_L cells grown in 0.1% O_2 (0.63 mmHg)

Mutant induction

Cells exposed to 2.5% pO₂ (15.75 mm Hg) were mutated at the rate of 29-58 mutations per 10⁵ cells (Figure 4.3). Radiobiological hypoxia is the level of hypoxia that results in attenuated tumor cell death due to radiation, and by definition partial radioresistance begins at oxygen tensions of 10 mmHg (Steen, 1991). Thus, mutants from cells exposed to 15.75 mm Hg were regarded as background mutants. For cells treated with 1% pO₂, I found inconsistent results in repeated assays and the average number of mutants was no different after four days in this hypoxic condition from the cells kept in standard conditions. For the cells exposed to 1% pO₂ for seven days the average number of mutants per 10⁵ cells was 19. Cells grown in 0.1% pO₂ for four days had an average of 17 mutants per 10⁵ surviving cells. Significant mutation induction was seen only among the cells exposed to severe hypoxia, pO₂ less than 0.63 mmHg (0-0.1%) for one day. Under these conditions the number of mutants was on average 130 per 10⁵ surviving cells (Figure 4.10).

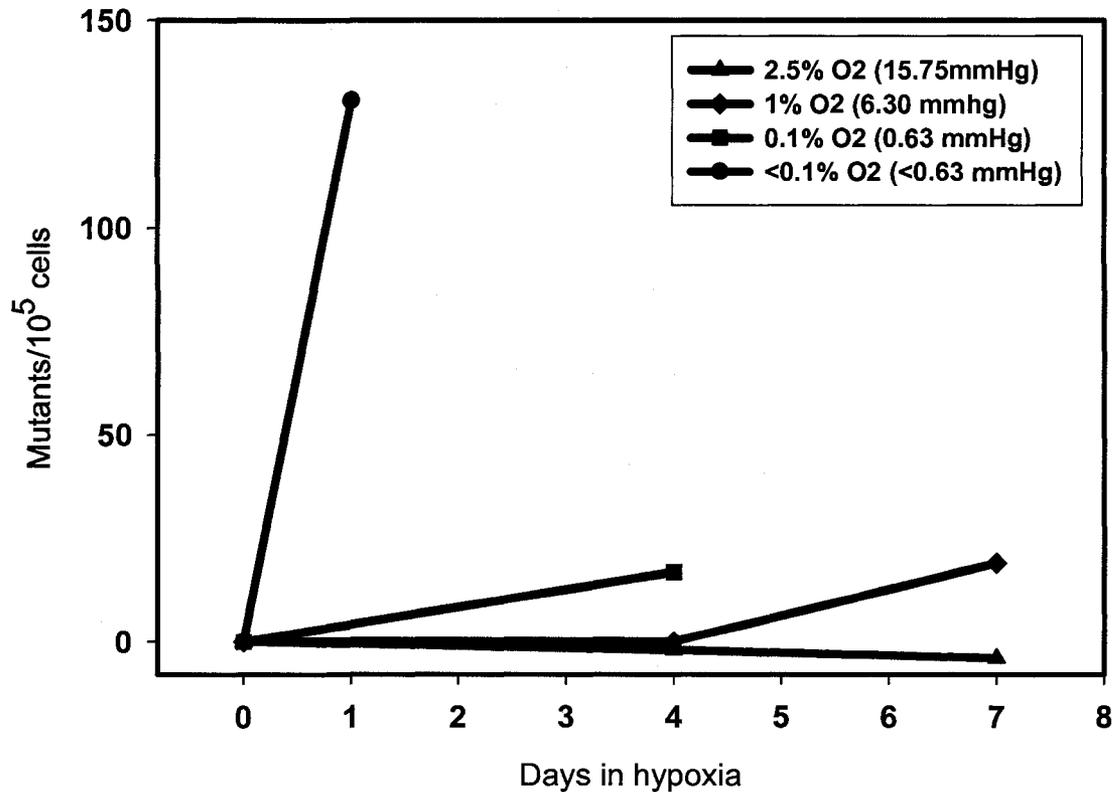


Figure 4.10. Mutant yield for CHO A_L cells treated with different hypoxic conditions. The number of mutants is corrected for background mutants.

*Flow Cytometry*¹

The development of flow cytometric analysis of CD59 mutants using the A_L cell line, without the need for a complement-mediated cytotoxicity assay, significantly reduces the time needed for each experiment. The proportions of CD59⁻ and CD59⁺ cells can be analyzed in one step by flow cytometry (Ross et al, 2005; Wedemeyer et al, 2001; Zhou et al, 2006).

¹ These experiments were done by Steve Keysar in Dr. Fox's lab

It is very important to have sufficient fluorescence separation between cells expressing the CD59 antigen (CD59⁺) and mutated CD59⁻ cells, in order to adequately differentiate and quantify mutants (French et al, 2006). The mutant region was gated as 1% of the mean fluorescence intensity of the positive control peak (Figure 4.11). This gave a 400-fold separation in fluorescence intensity between the two peaks, which is adequate to differentiate CD59⁻ from CD59⁺ cells.

Cells were treated with less than 0.1% O₂ for 24 hours, the same as the traditional complement/antibody assay. 10⁵ cells were analyzed for each experiment for statistical significance. The number of mutants per 10⁵ surviving cells on average was 136, about the same compared to results from complement/antibody assays (Table 4.2).

Flow cytometry histograms from these experiments demonstrate the quantification of CD59 mutants from control cell population and cell population treated with hypoxia (Figure 4.11).

To determine whether these CD59⁻ cells were really mutants and not just CD59 downregulated and temporarily expressed as mutants, single cells were sorted from the mutant region of hypoxia treated cells, allowed to grow into colonies, and after 21 days these cells were analyzed by flow cytometry. Out of 21 clonal populations, 16 fell within the mutant region they were sorted from while 5 clones showed intermediate or normal CD59 expression. This demonstrated that most cells scored as mutants are truly negative for CD59 (Figure 4.12).

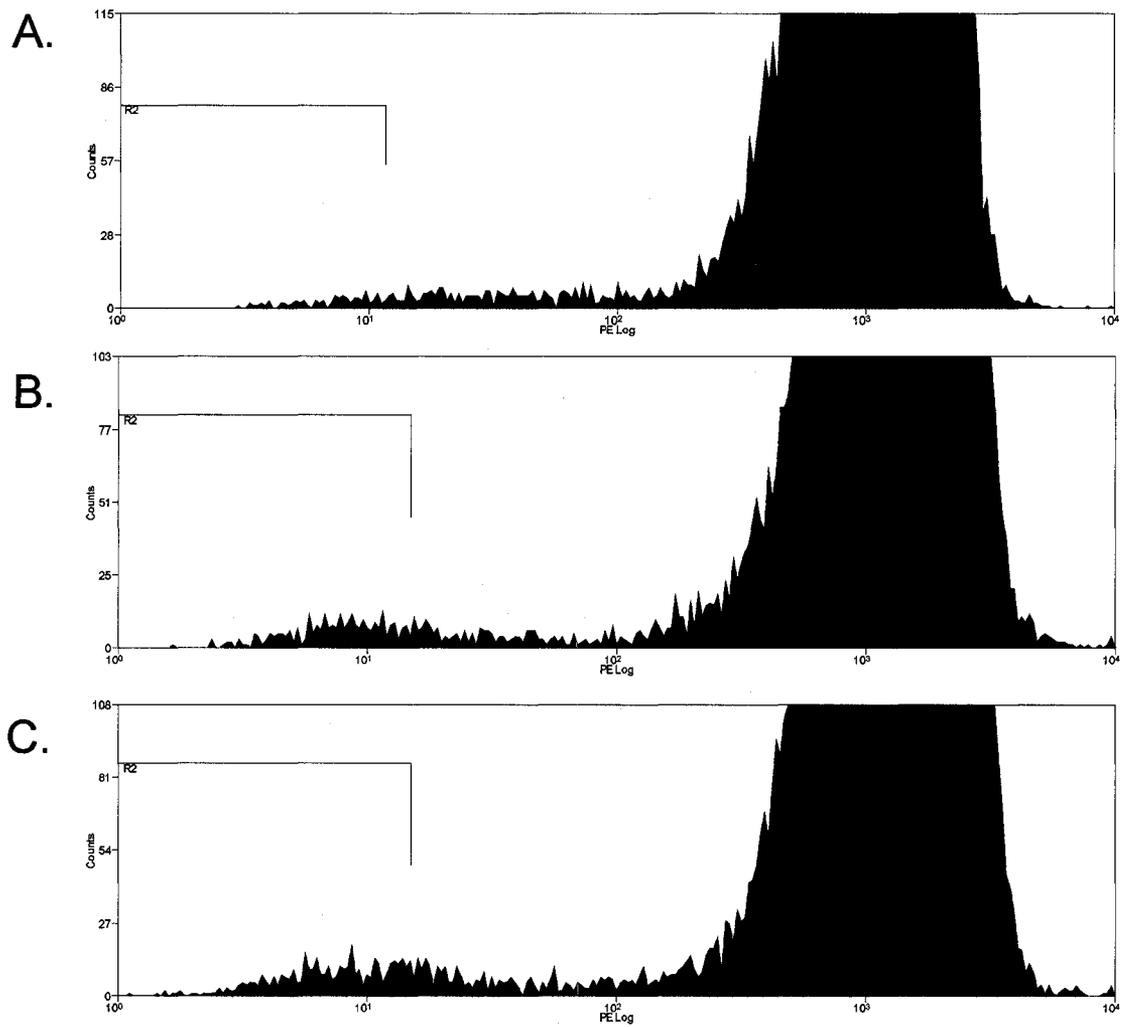


Figure 4.11. A. Control stained cells with gated region set as 1% of the positive peak and used to measure CD59 mutants. C. and B. Day 12 histograms of cells which were hypoxic for 24 hours.

Table 4.2. Flow cytometry analysis of mutants in A_L cells treated with <0.1 % pO₂ (<0.63 mm Hg). Mutant fraction reported as number of mutants per 10⁵ surviving cells and after subtracting background mutations.

Experiment 1			Experiment 2			Experiment 3		
Replicate	Control 1	Treatment 1	Replicate	Control 2	Treatment 2	Replicate	Control 3	Treatment 3
A	165	264	A	182	365	A	117	261
B	143	281	B	169	251	B	128	213
C	NA	281	C	NA	404	C	116	260
Average	154	275	Average	176	340	Average	120.33	244.66
SEM	11	5.7	SEM	6.5	45.9	SEM	3.8	15.8
mutant fraction			mutant fraction			mutant fraction		
121			165			124		
P value <0.01								

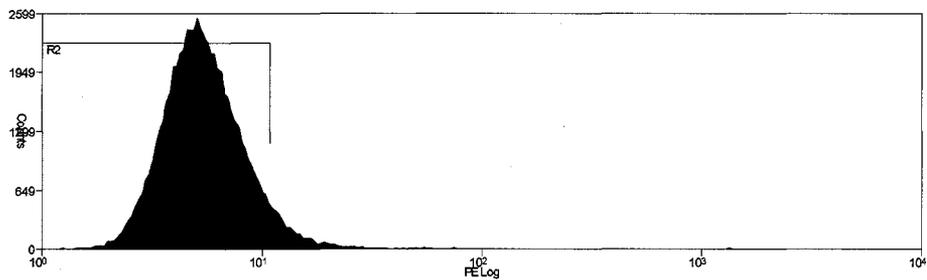


Figure 4.12. Hypoxia clone twenty days after sorting, then stained with monoclonal antibodies against CD59. 95% of the sample falls within the CD59 negative region it was sorted from.

Mutant spectra

To determine the types of mutation that cause the CD59⁻ phenotype in hypoxia-treated A_L cells, we isolated individual clones and applied PCR. Five marker genes on chromosome 11 were amplified to determine the presence or absence of corresponding PCR products (Figure 4.5). In this study CD59⁻ mutants retained all five of the human chromosome 11 markers (Figure 4.13). PCR analysis of the CD59 gene was obtained by providing primer pairs for the four exons of CD59 gene. PCR analysis of the four exons of the CD59 gene from CD59⁻ mutants (Figure 4.14) shows no loss of these markers. As no deletions were detected on the chromosome 11 with the chosen markers, and mutations in the human chromosome were smaller than 27 kb (the size of the CD59 gene) the analyses indicate the induction of point mutations or very small deletions in the A_L cells grown in severe hypoxia.

DNA Sequencing results

The same primers used for the PCR analysis of the four exons of the CD59 gene were utilized to produce DNA sequences for further analysis of the mutants induced by hypoxia. Since exon 1 is a non-coding exon of the gene, only exons 2, 3, and 4 were sequenced. The human reference sequence used was NM_000611.4 (from NCBI website). The analysis did not show mutations in DNA sequences that were examined (Figure 4.15). For exon 4, only one replicate was done because the one direction was unsuccessful, possibly due to inadequate DNA template or primers (Figure 4.16).

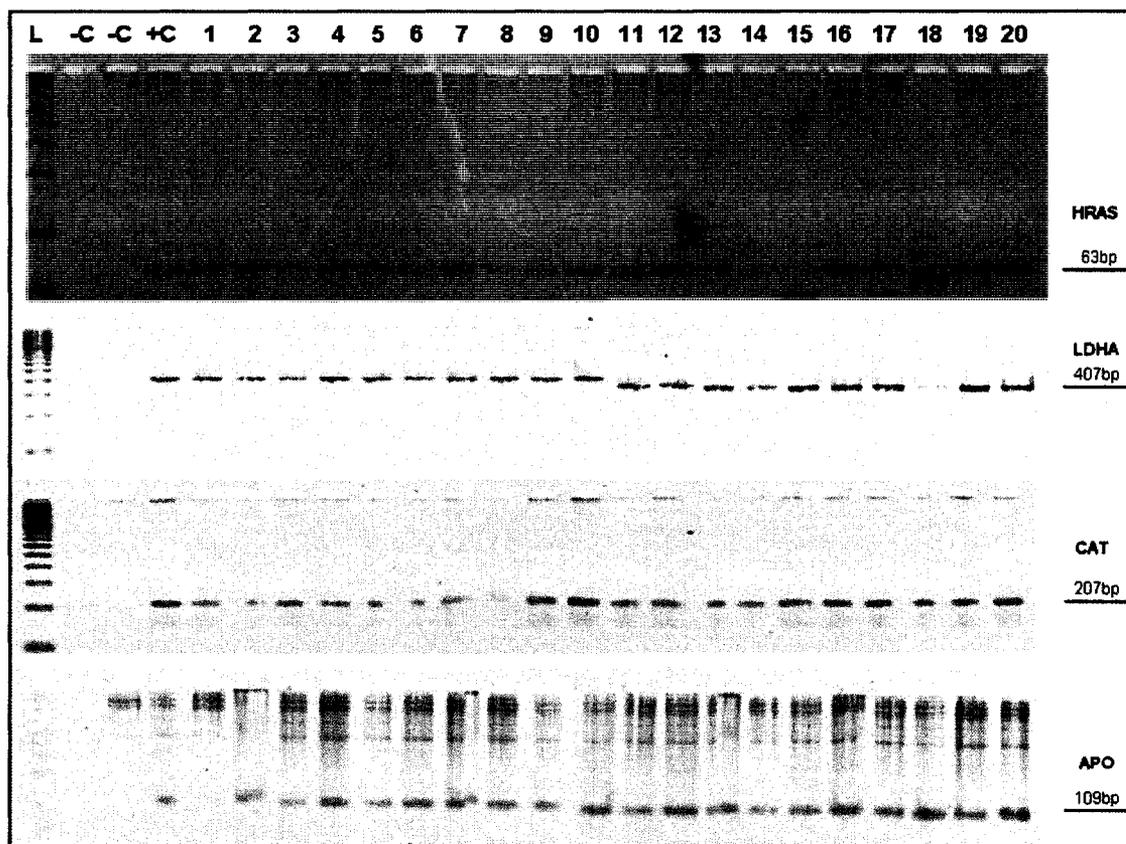


Figure 4.13. Gel electrophoresis of PCR products using DNA from CD59- mutants as templates and primers for RAS, LDHA, CAT, and APO. In each first lane is a size ladder (L), than (-C) are negative controls (no DNA, and CHO cells), next lane as a positive control wild-type CD59+ cells, and 1-20 are CD59-mutants induced by hypoxia. All samples show no loss of these markers.

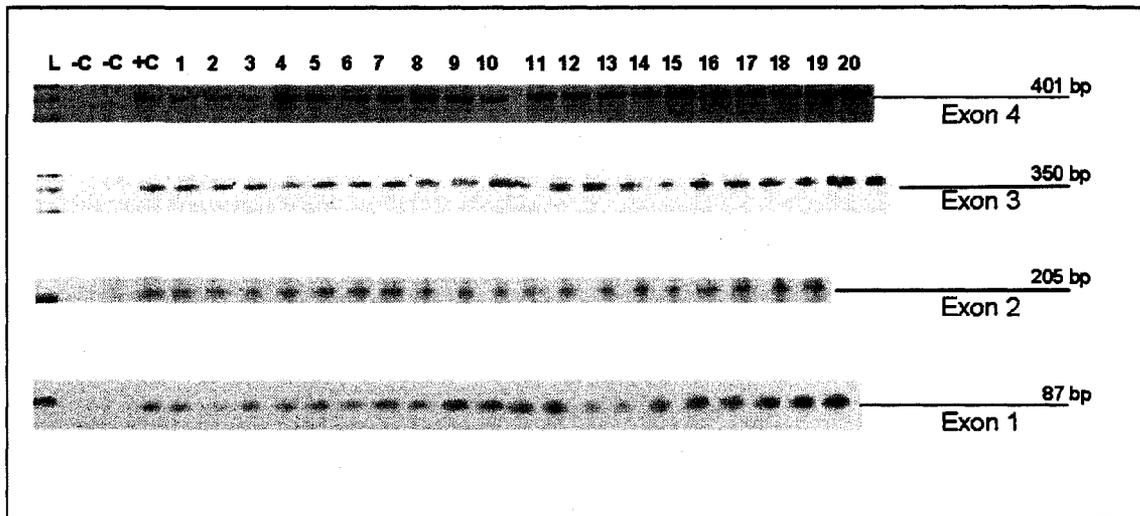
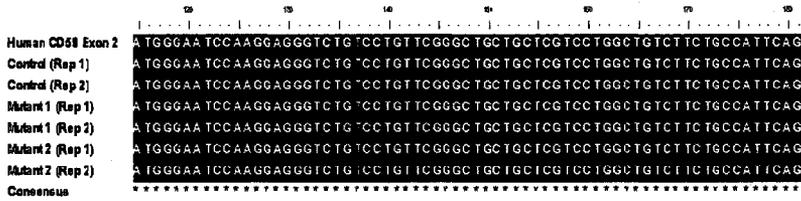


Figure 4.14. Gel electrophoresis of PCR products using DNA from CD59- mutants as templates and primers for four exons of CD59. Gels are done and marked the same as in Figure 4.13. All samples show no loss of these markers.

CD59

Exon 2 (67 bp)



Exon 3 (102 bp)

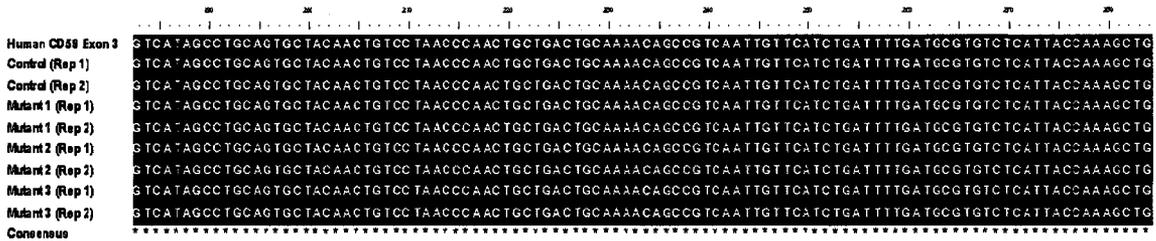


Figure 4.15. Alignment of human CD59 gene sequences, control DNA sequences and DNA sequences from mutant cells, for double replicas of exon 2 and exon 3. It shows no mutation in depicted sequences.

Exon 4 (218 bp)



Figure 4.16. Alignment of human CD59 gene sequence, control DNA sequence and DNA sequences from mutant cells, for one replica of exon 4. It shows no mutation in depicted sequences. “~” symbol for unreadable first 24 nucleotides (8 amino acids).

DISCUSSION

The results of this study indicated that exposure to severe hypoxia induces mutations in A_L cells, and there was a quantitative difference in mutant induction depending on the level of the oxygen present. The mutants reported in this study were induced by radiobiological hypoxia at the CD59 locus of A_L cells.

It has previously been reported that tumor microenvironment or conditions mimicking that milieu *in vitro*, are responsible for increased mutations (Reynolds et al, 1996; Wilkinson et al, 1995), increased drug resistance (Yuan et al, 2000; Reynolds et al, 1996; Rice et al, 1987), and are associated with various DNA lesions (Hammond et al, 2002, 2003; Rice et al, 1986). Hypoxia found in human malignant tumors was associated with more clinically aggressive phenotypes (Brizel et al, 1996, 2000; Hockel et al, 1996, 1998; Rofstad et al, 2000; Walenta and Mueller-Klieser, 2004). There is growing evidence that hypoxia induces proteome changes which may lead to the impairment of tumor growth activating anaerobic metabolism, angiogenesis, tissue remodeling, and may promote tumor propagation (Hockel and Vaupel, 2001). Exposure to hypoxic and acidic environments has been shown to induce changes in gene expression. As noted before, tumor microenvironment is characterized by nutrient deprivation, low pH, and hypoxic regions, and each of these factors has been shown to cause changes in cell metabolism and physiology (Yuan and Glazer, 1998; Reynolds et al, 1996). According to work done in this field, there is abundant evidence that tumor microenvironment is associated with the induction of mutagenesis. Tumor microenvironment may induce DNA damage

(Reynolds et al, 1996), and as shown recently, is also associated with deregulation of DNA repair pathways (Yuan et al, 2000; Mihaylova et al, 2003; Bindra et al, 2004). In this study I evaluated whether hypoxia alone could induce mutations and if so, to what extent. The A_L assay has been proven useful in showing a spectrum of chromosome mutations that can range up to deletions of 140 million base pairs (Waldren et al, 1998). I changed only the oxygen status in the experiments, and kept nutrition and pH of media (pH measurements were between 7.2 and 7.5) the same for all cells, both those exposed to hypoxia and cells in normal conditions. Hypoxia, or hypoxia/reoxygenation, induced mutations in CHO A_L cells that were significant at partial pressure of oxygen less than 0.1% (0.63 mm Hg). These results confirm the reliability of the A_L assay in detecting mutants induced experimentally by different mutagens. Ionizing radiation (Kraemer et al, 2000; Hei et al, 1988; Ueno et al, 2002; Ross et al, 2005) and a variety of chemical agents (Waldren et al, 1999; Zhou et al, 1999; Hei et al, 1998; French et al, 2006), produced mutants that have lost CD59 gene or larger portions of human chromosome 11 (Waldren et al, 1999; Kraemer et al, 2001).

Hypoxia did not produce drastic deletions as some other clastogens did, but induced mutations that in tumor cells may lead to more progressive tumor phenotypes. The difference in mutation induction depending on hypoxia intensity indicates that hypoxia alone, rather than reoxygenation, caused these changes. After the exposure to hypoxic conditions, cells were kept in normoxia while subculturing during the expression period in which the surface expression of CD59 is lost (Hei et al, 1988).

It appears that hypoxia alone can produce only SSBs and a possible explanation for my results may be found in the fact that hypoxia can result in an S-phase arrest (reversible

after reoxygenation) (Hammond et al, 2002). Thus hypoxia is involved in inhibition of initiation of replication, and consequently can not directly cause considerable DNA damage (Bindra and Glazer, 2005). Our results are consistent with the findings that hypoxia can induce point mutations without inducing DSBs (Reynolds et al, 1996; Hammond et al, 2002). In this study, flow cytometry analysis of mutants confirmed that an extremely low level of oxygen is associated with mutation induction. Single cells that were sorted from the mutant region of hypoxia treated cells and allowed to form colonies were subsequently analyzed using the same flow cytometry analysis method. The majority of the clones remained within the mutant region from which they were originally sorted. Only 5 out of 21 clonal populations showed some CD59 expression. This could possibly be due to sorting error, and more experiments could be needed to verify these results. The sorting results demonstrated that most cells scored as mutants were truly negative for CD59.

Since PCR analysis and DNA sequencing analysis that was performed in these experiments did not detect changes in different genes on chromosome 11, or in exons of the CD59 gene, to further exploit hypoxia-produced changes it may be useful to perform analysis of a greater number of mutants, and maybe do better primers design for DNA sequencing. There is a possibility that loss of expression of the CD59 surface antigen can be caused by mutations in the CD59 gene or by mutation in any one of about a dozen CHO genes involved in expression of the GPI anchor that attaches CD59 antigen to the cell surface (Kraemer et al, 2001). Therefore, one of the directions in the future investigations could be analysis of the CHO genes that encode the GPI anchor (Kinoshita et al, 1997; Nakamura et al, 1997).

It has recently been shown that nearly half of ionizing radiation-induced mutants in CD59 also lost the expression of CD90, another gene on chromosome 11 that is anchored by GPI. Direct analysis of the GPI anchor showed that 33% of the double mutants were defective for the GPI anchor (Ross et al, 2007), most likely in the X-linked Pig A gene. It is important to understand the role of hypoxia in tumor development and progression, as well as its role in treatment resistance and importance of its prognostic aspect. This would be beneficial for the possible development of novel therapeutic strategies that, by targeting tumor hypoxia, may influence genomic stability and result in a better prognosis for patients with hypoxic tumors.

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CHAPTER 5

CONCLUSIONS

The two sections of this dissertation are concerned with a common feature of the tumor microenvironment: tumor hypoxia. Even though extensively investigated in various experimental settings and tumor models for over 50 years, many unanswered questions remain. The causes and consequences of tumor hypoxia are significant because of its impact on cancer progression and resistance to therapy.

The term tumor hypoxia is still not precisely defined. From the radiation biology perspective, importance is given to the level of oxygen in the tumor that causes tumor cells to become resistant to killing by radiation. This is referred to as radiobiological hypoxia. The level of hypoxia that causes radioresistance is lower than the level necessary to cause other hypoxia-related biological phenomena (such as cell growth, cell survival, and angiogenesis). Tumor cells start developing radioresistance at a pO_2 of 10 mmHg, and are completely resistant at oxygen levels less than 1 mmHg (Steen, 1991). This 10 mmHg benchmark has been used by many authors as the threshold of tumor hypoxia. More recent studies are advocating measurements of tumor oxygen levels less than 5 mmHg as hypoxic, or even below 2.5 mmHg as a more meaningful clinical predictor. This has been applied to clinical studies in human and veterinary medicine.

Furthermore, some authors are defining radiobiological hypoxia at even lower oxygen levels like those of the maximally radioresistant fraction of tumor cells found at $pO_2 < 1$ mm Hg or <0.5 mm Hg (Gulledge and Dewhirst, 1996; Wouters and Brown, 1997, respectively). The confusion about tumor hypoxia thus begins with the understanding of what we consider hypoxic region in tumor: value of pO_2 less than 10, 5, 2.5 mm Hg or less than 1, or 0.5 mm Hg; the oxygen level where cell radioresistance starts to develop, progress through that development or when cells are fully resistant to radiation.

Part 1 is an *in vivo* study of changes of oxygen level in tumors after a single dose of radiation treatment. Measuring oxygen partial pressures and other biological parameters in spontaneously developed canine tumors revealed that their microenvironment is very much comparable to the human tumors. We evaluated changes after radiation, but also gained insight in unperturbed tumor microenvironment. Tumor microenvironment is shown to be very complex and tumor hypoxia has to be regarded in that complexity. The classification to perfusion-limited and diffusion-limited oxygen delivery is really oversimplified. Many other parameters are playing a role in the development of tumor hypoxia, and it is important to examine this problem in the complex three-dimensional view as a part of tumor microenvironment. Even more, doing my research with CHO A_L assay and creating the survival curves to determine what the exposure of the cells to hypoxic conditions should be, I demonstrated a role for time. The consequences of different levels of hypoxia were greatly influenced by the time of the exposure, adding the new dimension to the mosaic of hypoxic conditions.

Part 2 is concerned with the role of hypoxia in the induction of mutagenesis and subsequently in genomic instability, which is a hallmark of malignancies. This *in vitro*

study gave us insight in the possible and probable development of the chain of the events that could lead to a more aggressive tumor behavior.

The results of the second study showed that extreme hypoxia may lead to mutagenesis. The results of the first study proved that this level of hypoxia is present in most of the hypoxic regions existing in naturally occurring tumors.

Both of my studies have an implication in the present understanding of tumor treatment failure. The main factors determining disease control after radiation therapy are tumor radioresistance and incidence of tumor metastasis (West et al, 1997; Lyng et al, 2000). Hypoxia may induce genetic instability of tumors leading to increased metastatic potential (Young et al, 1988; Reynolds et al, 1996). The hypoxia-induced radioresistance is dependant on oxygenation at the time of irradiation, relying on changes in biological parameters responsible for the oxygen supply and consumption in the tumor. As stated by Overgaard (2007), among the several thousands of publications about hypoxia and radiation therapy, only about 3% address hypoxia in the therapeutic clinical setting. Therefore, studies of the changes in these parameters after a fraction of radiation during scheduled radiation treatment are needed, and studies performed in a clinical setting must incorporate concepts related to tumor hypoxia into routine clinical use, which is still very limited.

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